

## **Diploma Thesis**

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# Modeling of the Hardening Process of Micro-Particles

Modellierung des Aushärtungsprozesses von Mikropartikeln

Hannes Pucher

Advised by:

Dipl.-Ing. Dr.-Ing. Daniele Suzzi Dipl.-Ing. Dr.techn. Stefan Radl

Univ.-Prof. Dipl.-Ing. Dr.techn. Johannes G. Khinast



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#### Abstract

Considering the increasing complexity of drugs, process understanding in the pharmaceutical industry becomes more and more important. Often the method by which a drug is delivered has a significant influence on the therapeutic effectiveness. Biodegradable-controlled-release-systems, as investigated in this work, introduce new concepts in drug administration, can replace other dosage forms and provide new treatment options for doctors and patients in their fight against diseases.

Due the poorly reported process-engineering approaches the objective of this work was to investigate the extraction step of a micro-particle process on the basis of emulsification solvent extraction method. The gained insights should on the one hand provide a better understanding and on the other hand help to predict different characteristics of microparticles.

Therefore a numerical model was developed and different experimental investigations were performed. The developed numerical model is capable to describe the mass transfer from the disperse phase into the continuous phase respectively the hardening/extraction process. At the first step the obtained numerical results were compared with an analytical solution, found by John Crank [7] which showed a good agreement. Furthermore a custom build shrinking model respectively a method to numerically compute the diameter reduction of the micro-particles was implemented.

Next the discretization uncertainty was investigated and in addition a parameter study was performed to find realistic ranges for the values of the unknown variables.

For the validation of the numerical model, the estimated results were compared with the experimentally determined diameter of the micro-particles. It showed, that the predictions of our numerical model fit experimental data reasonably well.

For the experimentally research of the process an experimental set up was build in the labs of the Research Center Pharmaceutical Engineering (RCPE GmbH) in Graz. The performed investigations were able to quantify the micro-particle size during the extraction process and determine the influences of different parameters on the final micro-particle quality.

II

#### Kurzfassung

In Anbetracht der zunehmenden Komplexität von Medikamenten, gewinnt das Prozessverständnis in der pharmazeutischen Industrie immer mehr an Bedeutung. Oft hat die Methode, mit der ein Medikament zugeführt wird, einen entscheidenden Einfluss auf die therapeutische Effektivität. Biologisch abbaubare-kontrollierte-Freisetzungsysteme, die Arbeit untersucht wurden. könnten dieser neue Konzepte in der in Medikamentenverabreichung ermöglichen, andere Darreichungsformen ersetzen und neue Behandlungsmöglichkeiten für Ärzte und Patienten in ihrem Kampf gegen Krankheiten anbieten.

Aufgrund der kaum verfügbaren verfahrenstechnischen Konzepte, war das Ziel dieser Arbeit den Extraktionprozess eines Mikro-Partikel-Prozesses auf der Grundlage der "Solvent Extraction Method" zu untersuchen. Die gewonnenen Erkenntnisse sollten einerseits das Prozessverständnis fördern und andererseits dazu dienen verschiedene Eigenschaften der Mikropartikel vorherzusagen.

Aus diesem Grund wurde ein numerisches Modell entwickelt und verschiedene experimentelle Untersuchungen durchgeführt. Das entwickelte numerische Modell ist in der Lage, den Stoffübergang von der dispersen Phase in die kontinuierliche Phase beziehungsweise den Aushärtungs- bzw. Extraktionsvorgang zu beschreiben. Im ersten Schritt wurden die erhaltenen numerischen Ergebnisse mit einer analytischen Lösung von John Crank [7] verglichen, welche eine gute Übereinstimmung zeigten. Darüber hinaus wurde ein selbst entwickeltes Schrumpfungs-Modell bzw. eine Methode zur numerischen Berechnung der Durchmesserreduktion der Mikro-Partikel implementiert.

Des Weiteren wurde der auftretende Diskretisierungsfehler untersucht und eine Parameter-Studie durchgeführt, um realistische Wertebereiche für die unbekannten Variablen zu finden. Zur Validierung des numerischen Modells wurden die errechneten Ergebnisse mit den experimentell bestimmten Durchmessern der Mikropartikel verglichen. Dies, zeigte dass Vorhersagen unseres numerischen Modells gut mit experimentell erhobenen Daten übereinstimmen.

Für die experimentelle Untersuchung des Prozesses wurde ein experimenteller Aufbau in den Labors der Research Center Pharmaceutical Engineering (RCPE GmbH) in Graz errichtet. Mithilfe der durchgeführten Untersuchungen konnte die Mikro-Partikelgröße während der Extraktion quantifiziert und die Einflüsse verschiedener Parameter auf die endgültige Mikro-Partikel Qualität ermittelt werden.

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### Abbreviations

SMD	Sauter mean diameter
CFL-number	Courant-Friedrichs-Lewy-number
EA	Ethyl acetate
BA	Benzyl alcohol
PVA	Polyvinyl alcohol
W	Water

#### Nomenclature

#### Latin symbols:

- $A_P$  Surface area of the micro-particle  $[m^2]$
- Bi Biot number
- $\Delta c$  Concentration difference
- C<sub>i</sub> Initial concentration [kmol/m<sup>3</sup>]
- $C_0$  Equilibrium concentration [kmol/m<sup>3</sup>]
- C<sub>S</sub> Actual concentration [kmol/m<sup>3</sup>]
- $D_i$  Diffusion coefficient of the component i  $[m^2/s]$
- $D_{i,CP}$  Diffusion coefficient in the continuous phase [m<sup>2</sup>/s]
- $D_{i,DP}$  Diffusion coefficient in the disperse phase [m<sup>2</sup>/s]
  - d<sub>P</sub> Diameter of the micro-particle [m]
  - d<sub>P,t</sub> Characteristic length/dimension/diameter at time t [m]
  - d<sub>R</sub> Diameter of the stirrer blade [m]
  - Fo Fourier number
  - $J_i$  Volume flux relative to polymer velocity  $[m^3/(m^2 s)]$
  - K Equilibrium Constant
  - M Molecular weight [kg/kmol]
- $\dot{M}_{t=0}$  Mass transfer rate at the beginning [kg/s]
- m<sub>i,m,t</sub> Mean Mass of component i [kg]
- m<sub>Shell,m,t</sub> Mass of a spherical shell at time t [kg]
- $\Delta m_{\text{Shell,m,t}}$  Mass difference [kg]
  - N<sub>i</sub> Number of drops

- n Revolution rate of the stirrer [rpm]
- $\dot{n}_i$  Molar flow [mol/s]
- n<sub>Radial</sub> Number of radial sections
  - R Gas constant [J/(mol K)]
  - Re Reynolds number
    - r Radius of the micro-particle [m]
  - $r_{max}$  Radius of the micro-particle [m]
    - r<sub>n</sub> Normalized radius of the micro-particle
- $r_{1,i}$ ,  $r_{2,i}$ ,  $r_{3,i}$  System dependent constants for the component i
  - Sc Schmidt number
  - Sh Sherwood number
    - T Temperature [K]
    - t Time [s]
  - t<sub>total</sub> Total extraction time [s]
    - $\Delta t$  Time step [s]
    - V Molar volume of the dissolved substance at its boiling point  $[cm^3/mol]$
    - V<sub>i</sub> Volume of component i [m<sup>3</sup>]
  - V<sub>i,m,t</sub> Volume of a spherical shell [m<sup>3</sup>]
  - $V_{\text{Shell},r,t}$  Volume of spherical shell at r and time t [m<sup>3</sup>]
  - $V_{\text{Sphere,m,t}}$  Volume of sphere at the time t [m<sup>3</sup>]
    - V<sub>Total</sub> Total volume [m<sup>3</sup>]
      - $\Delta V$  Volume difference [m<sup>3</sup>]
        - v Mean fluid velocity [m/s]
      - $\overline{v}_i$  Molar volumes of the component i [m<sup>3</sup>/mol]

- v<sub>3</sub> Velocity of the polymer [m/s]
- $w_i \quad \text{Mass fraction of the component } i$
- $w_{i,m,t} \quad \text{Mean mass fraction of the component } i$ 
  - x Association parameter
  - $\Delta x$  Length of a radial section [µm]

### Greek symbols:

α, β, γ	Ratios of the molar volumes	
$\beta_i$	Mass transport coefficient of the component i [m/s]	
$\beta_{i,CP}$	Mass transport coefficient in the continuous phase [m/s]	
$\beta_{i,DP}$	Mass transport coefficient in the disperse phase [m/s]	
$\delta_i$	Interface thickness [m]	
η	Dynamic viscosity of the solvent $[1 \text{ cp} = 10^{-3} \text{ Pas}]$	
μ <sub>i</sub>	Chemical potential of the component i [J/mol]	
$\gamma_{Cp}$ Kinematic viscosity of the continuous phase [n		
$\rho_{DP}$	Density of the disperse phase [kg/m <sup>3</sup> ]	
$ ho_i$	Density of the component i [kg/m <sup>3</sup> ]	
$\rho_{Shell,m,t}$	Density of the spherical shell [kg/m <sup>3</sup> ]	
φAnalytical,i,r,t	Analytically found volume fraction of the component i	
$\phi_i$	Volume fraction of the component i	
$\phi_i{}^0$	Initial composition of component i	
$\phi_{i,CP,\infty}$	Volume fraction in the continuous phase	
$\phi_{i,DP,\infty}$ Volume fraction in the disperse phase		
$\phi^*_{i,CP,I}$ Equilibrium volume fraction at the interface of the		
$\phi^{*}_{i,DP,I}$	Equilibrium volume fraction at the interface of the CP	

 $\phi_{i,m,t}$  Mean volume fraction of component i

- $\phi_{Numerical,i,r,t}$  Numerically found volume fraction of the component i
- $\phi_{i,n,t}, \phi_{i,n+1,t}$  Volume fraction of component i at two specific radial positions
  - $\phi_P$  Volume fraction of the polymer

- $\Delta \phi$  Volume fraction difference
- $\chi_{ij}$  Binary interaction parameters

### 1. Introduction

### 1.1. Motivation

Micro-particles are widely used in the pharmaceutical industry as delivery forms for many kinds of drugs [16]. Microencapsulated drugs and vaccines have often a therapeutic benefit and that's why they forth the need to prepare such particles in larger quantities and in sufficient quality suitable for clinical trials and commercialization [9]. Generally, these so-called controlled-release systems refer to materials, or devices, which control the release time of a chemical, the release rate, or both [27].

In Figure 1-1 the concentration of the drug over the time is shown for a conventional and a controlled drug delivery system. In the conventional profile, at the beginning of the dissolution process the concentration of the drug increases very fast to a peak above the optimum therapeutic range. This peak could even lead to potentially fatal toxicity, for example in case of sleeping pills. After that, the concentration decreases rapidly under the optimum therapeutic range, leading no therapeutic effect.

As a consequence of these facts, it is evident that by using a conventional drug delivery system the time spent in the optimum concentration range is very short. The ideal concentration profile should be therefore nearly time independent and the optimal amount of drug should be release continuously. This "controlled" profile, also known as sustained release, is shown as well in Figure 1-1.



Figure 1-1: Exemplary concentration c vs time t profile for conventional and controlled-release drug delivery devices [27]

The influence of the method by which a drug is delivered on the therapeutic effectiveness becomes more and more important [3]. Without a continuous drug supply, the optimum therapeutic range of concentration of some drugs is attained only during very short time periods and concentration variations can be toxic or have no therapeutic benefit. Also in cases where a treatment over a longer time period is necessary, controlled-release systems are highly desirable. These systems could as well replace common dosages forms like multiple injections in order to ensure a certain drug level for a defined period of time [16].

Practically, the controlled profile could for example be achieved by incorporating the drug in a biodegradable polymeric carrier that controls the drug delivery and the release rate of the drug. These biodegradable-controlled-release-systems introduced new concepts in drug administration and usually provide high stability and easy handling. The desired release profile can be controlled by the choice and the production method of the polymer carrier. Common problems like short in vivo half-lives, physical and chemical instability, as well as low oral bioavailability of proteins, can be overcome by adopting sustained release concepts.

Historically, since the first appearance in the 1960s and 1970s, the number and variety of the controlled-released systems for drug delivery have increased dramatically. Nowadays these approaches have many different fields of application and are common in food, pesticides and cosmetic industry. Typical implementations are for example the release of flavors and vitamins in food, fragrances in perfumes, as well as inks in carbonless copy paper [27]. The largest application area for controlled release products is nevertheless the field of drug delivery in the pharmaceutical industry.

Despite the versatile use and the many advantages of the biodegradable-controlled-release systems, process-engineering aspects and numerical models of the different preparation techniques remain poorly reported [19]. A concrete numerical model concerning the solidification of microspheres is to our knowledge only build by Li et al. [18]. Actually, the numerical results of this model are only experimentally validated concerning the residual of solvent in the micro-particle. The resulting micro-particle size or other parameters were not compared.

To sum up, the ultimately idea behind a biodegradable-controlled-release system is to achieve more effective therapies with optimal dosage of the drug and provide new treatment options for the doctors and patients in their fight against diseases [24] [27].

Therefore, a deep understanding of each step of the production process is of great significance.

### 1.2. Goals

The final goal of the project, which this thesis is part of, is to develop a robust and scalable micro-particle process on the basis of solvent extraction method. This method is a very popular and often used technique for the preparation of micro-particles and is described in detail in Chapter 2. The final process should produce micro-particles with a defined (and close) size distribution and every micro-particle should consist of the same components.

The objective of this study is to systematically analyze the extraction step and to develop a numerical model for the description of the process. The final outcome is to predict different product characteristics, like the size of the final micro-particle, in dependence to the process parameters and the initial conditions of the extraction stage. The results and the knowledge gained in this work should provide on the one hand a better understanding of preparation process and, on the other hand, determine the influences of the most important process parameters on the final micro-particles. For this purpose, experimental analysis as well as computational mathematically modeling had been used.

For the detailed experimentally investigation of the process an experimental set up was built up in the labs of the Research Center Pharmaceutical Engineering (RCPE GmbH) in Graz. The mathematically model of the diffusion/extraction process was based on the MATLAB software from MathWorks Inc. Here, the most important phenomena simultaneously occurring inside the microparticle have been described in the numerical code.

Finally, the results obtained from the experimentally study were used to validate the mathematical model and a parameter study for different process parameters was carried out as well.

### 1.3. Thesis Outline

First, the state of the art for micro-particle preparation/microencapsulation processes used in the pharmaceutical industry are presented and described in Chapter 2. This background chapter should provide a general overview of the different preparation techniques and the common used chemicals.

The most important units of the experimental set up are then described in the Basic Engineering Chapter (Chapter 3).

The different conducted experiments and the different used measurement systems (HELOS and QICPIC) are accurately described in Chapter 4. Finally, the results of the performed experiments are also summarized in here.

Chapter 5 deals with the mathematical model for the description of the extraction/diffusion process. In this chapter the mass transport model, the shrinking model, the analytic verification, the used PDEPE solver and all the important parameters are described in detail.

In the following Discussion and Interpretation Chapter (Chapter 6) different parameters studies are performed. The objective is to get on the on hand a deeper understanding of the model and, on the other hand, to identify the ranges of some unknown parameters.

### 2. Background

### 2.1. Fabrication Techniques of biodegradable Micro-Particles for Drug Delivery Applications

According to Birnbaum et al. [5] there are innumerable methods to produce microparticles, but the serviceability of a particular method is often determined by the solubility of the polymer and the drug. Furthermore, shear forces and temperature have often a damaging impact on the micro-particles when for example peptides and proteins have to be encapsulated [13].

Scheler [9] and Freitas et al. [28] defined that the production processes of polymer microparticle are often modifications of three basic techniques, namely:

- 1. solvent extraction/evaporation,
- 2. phase separation (coacervation),
- 3. and spray drying.

According to Luan [20], the general requirements for micro-particle preparation are:

- Keep the stability of the encapsulated active ingredient.
- Achieve optimal drug loading, high encapsulation efficiency and yield.
- Obtain the desired drug release profile.
- Produce micro-particles with free flow ability.
- Establish a simple and reproducible process.

Concerning the structure of this chapter first of all the three different basic techniques are described in detail. Afterwards the main influences on the properties of the micro-particle are presented. Therefore the commonly used compounds for the two phases, namely the disperse and continuous phase are summarized.

### 2.2. Solvent Evaporation and Extraction based Processes

According to Herrmann et al. [13] the most popular methods for the preparation of microparticles from hydrophobic polymers are organic phase separation and solvent removal techniques. This method neither requires high temperatures nor phase separation-inducing agents. Nevertheless it is possible to achieve controlled particle sizes in the nano to micrometer range [9].

Freitas et al. [9] defined the four major steps of the micro-particle preparation by solvent extraction/evaporation as listed below.

- Dispersion or dissolution of the API (Active Pharmaceutical Ingredient), in an organic solvent which contains the matrix forming material (for example PLGA polymer).
- 2. This organic phase in then emulsified in a second continuous (frequently aqueous) phase immiscible with the first one.
- 3. The solvent is extracted from the dispersed phase into the continuous phase, which is optionally accompanied by the evaporation of the solvent. As a consequence of that the droplets are transformed into solid micro-particles.
- 4. In this step the micro-particles are harvested and dried.

A schematic overview over these four major steps is shown in Figure 2-1Figure 1-1.



Figure 2-1: Schematic overview over the four principal process steps in the micro-particle preparation by solvent extraction/evaporation [9].

Classically, the drug-containing organic polymer solution is emulsified into an aqueous phase which normally contains a suitable stabilizer. The solubility properties of the drug determine if it is dissolved, dispersed or emulsified as an aqueous solution into the organic polymer solution [13].

### 2.3. Phase Separation (Coacervation)

According to IUPAC (International Union of Pure and Applied Chemistry), coacervation is defined as the separation of colloidal systems into two liquid phases [21]. This long established and widely used method for micro-encapsulation of biological materials relies upon a decrease of the polymer solubility by addition of a non-solvent [23] [11].

According to Nihant et al. [23], the point has to be reached where the two liquid phases are formed: a polymer-rich coacervate where the dissolved drug is entrapped and a supernatant liquid phase depleted in polymer.

In Figure 2-2 a schematic representation of the coacervation process is shown. As defined by Jyothi et al. [17], the major steps of a micro-encapsulation by coacervation process are:

- 1. Dispersion of the core material in a solution of shell polymer.
- 2. Separation of coacervate from solution.
- 3. Coating of the core material by the produced micro-droplets of coacervate.
- 4. Formation of a continuous shell around core particles trough the coalescence of coacervate.



Figure 2-2: Schematic representation of the coacervation process [17].

According to Luan [20] the major disadvantages of coacervation method are the difficulties in scaling-up, the use of large amount of organic solvent and the high residual of solvent and coacervating agents in the micro-spheres. Also the production of micro-particles in the low micrometer size range is difficult [9].

### 2.4. Spray Drying

Spray drying has been used for many years as micro-encapsulation technique because of its simplicity, the high throughput and the low-costs [17] [33] [9]. In comparison to the previous mentioned methods, spray drying, is easily to be scaled up [20].

As shown in Figure 2-3, the core particles which contain the drug are dispersed in a polymer solution and atomized/sprayed into a hot chamber [17] [20]. This leads to an instantaneously evaporation of the solvent whereby relatively rapid solidification of the shell material onto the core particles is effected [33] [20].



Figure 2-3: Schematic illustrating the process of micro-encapsulation by spray-drying [17].

The greatest disadvantages of this method are that it must not be used for highly temperature sensitive-compounds and that there are large amount of product loss during process, which result in a low yield [9]. Furthermore, spray drying is also prone to produce agglomeration. Hence the control of the particle size is difficult [20].

### **2.5.** Choice of Material

According to Izumikawaa et al. [15] the properties of the used compounds and the operating parameters have a big impact on the physical properties of the obtained micro-particles. These main factors are summarized in Figure 2-4.

In these section an overview over the different common used compounds for the two phases, namely the disperse and continuous phase are presented. The detail description of the compounds used in our process can be found in section 3.2.



Figure 2-4: Schema of the factors influencing the properties of micro-particles [19].

### 2.5.1. Dispersed Phase

#### Polymer

An essential characteristic of the polymers used in the pharmaceutical industry are their biodegradability or biocompatibility. That means that the components should on the one hand degrade into harmless components which are either metabolized or excreted. On the other hand they should be physiologically acceptable and should not cause a negative local or systemic reaction after the administration.

Polymers and copolymer copolymers of lactic and glycolic acids are often used as the biomaterials for the microencapsulation of therapeutics because they provide the requested properties and the applications in humans are approved by the FDA (Food and Drug Administration) [19].

The desired drug release rate is determined by the physical properties of the polymer. So if one polymer cannot offer the wanted release characteristics a single polymer, called copolymer can be synthesized from two different ones.

The main properties of the usually used polymers and copolymers for microencapsulation by solvent evaporation method are presented in Table 2-1.

Abbreviation	Complete name	Properties	
PLGA, PLG	Poly(lactic-co-glycolic acid) or Poly(lactide-co-glycolide)	Good biodegradability and biocompatibility	
PLA	Poly(lactic acid) or polylactide	Good biodegradability and biocompatibility, slow degradation rate compared to PLGA	
PEG (used in co-polymer)	Poly(ethylene glycol)	Often synthesized with PLGA or with PLA to form a co-polymer with fast degradation rate	
PHB	Poly-3-hydroxybutyrate	Bacterial storage polyester; slower degradation rate than polylactic polymers	
PHB-HV	Poly-3-hydroxybutyrate with hydroxyvalerate	Bacterial storage polyester; slower degradation rate than polylactic polymers	
EC	Ethyl cellulose	Degradable, biocompatible, approved by FDA for pharmaceutical application; low cost	
PMMA	Polymethyl methacrylate	Non-degradable but biocompatible, approved by FDA; bone cement material; low cost; alternative polymer for scale-up investigation	

## Table 2-1: Polymers commonly used for microencapsulation using solvent evaporation techniques [19].

#### Solvent

According to Li et al. [19] the solvent for the technique of microencapsulation by solvent evaporation, should fulfill the following criteria:

- being able to dissolve the chosen polymer;
- being poorly soluble in the continuous phase;
- having a high volatility and a low boiling point;
- having low toxicity.

The main solvents used in the literature and their properties are presented in Table 2-2.

Name	Advantages/Disadvantages
Chloroform	Low solubility in water; higher toxicity than dichloromethane
Dichloromethane (methylene chloride)	Dissolvation of most of the polymers; almost immiscible in water; high volatility and quite low boiling temperature; high toxicity
Ethyl acetate	Low toxicity/partially soluble in water; very low vapour pressure
Ethyl formate	Low toxicity; partially soluble in water

# Table 2-2: List of solvents commonly used for microencapsulation by solvent evaporation [19]. Name Advantages/Disadvantages

#### **Alternative Components**

In some cases a co-solvent and a porosity generator could be added to the disperse phase [19]. A co-solvent could be improve/enhance the dissolution of the drug and a porosity generator could increase the number of pores inside the micro-particle.

### **2.5.2.** Continuous Phase

#### Surfactant

To reduce the surface tension of the continuous phase, avoid coalescence and agglomeration of the drops and, as well as to stabilize the emulsion frequently a surfactant, also called tensioactive agent, is employed. The most important criteria in selecting the surfactant are the desired size and the demand on the sphericity of micro-particles.

The amphiphilic behavior of the surfactants, that means one part of the molecule is hydrophilic and the other one is hydrophobic, causes the stabilizing effect by covering the surface of the drops.

According to Li et al. [19] there are four different surfactants classified by the nature of the hydrophilic part of the molecule:

- anionic,
- cationic,
- amphoteric
- and non-ionic

#### **Alternative Components**

In certain cases antifoam is added into the aqueous phase because the foaming problem disturbs the formation of the micro-particle [19].

### 3. Basic Engineering

### 3.1. Process Overview

The production of micro-particles represents an important unit operation in the pharmaceutical industry. The typical methods to manufacture solid particles from liquid solutions are described in detail in Chapter 2.

As illustrated in Figure 3-1, the investigated micro-particle formation process based on solvent extraction method can be separated into 5 stages:

- 1. Mixing Step (Droplet Formation)
- 2. First Extraction Stage (First Solvent Removal/Solidification Stage)
- 3. Intermediate Drying Stage
- 4. Second Extraction Stage (Second Solvent Removal/Solidification Stage)
- 5. Final Drying Stage

Concerning the structure of this chapter first of all the different used chemicals are presented. Then the different preparation steps of the three needed solution respectively the organic, the liquid and the continuous phase and the stages of the micro-particle process are describe in detail. After that an overview over the experimental set up is given and the most important details of the different units, namely the mixer, reactor and the cooling unit are shown.



Figure 3-1: Overview of the process.
# **3.2.** List of the Chemicals

The material parameters of the most important components are summarized in Table 6-3. The compounds used in our process are here described in detail.

### 3.2.1. Ethyl acetate

The often used solvent ethyl acetate respectively ethyl Ethanoate and commonly abbreviated EtOAc or EA is an organic compound with the formula CH<sub>3</sub>COOCH<sub>2</sub>CH<sub>3</sub>. It shows promising potential as the solvent of the polymer (PLGA) in the micro-particle production based on solvent extraction method because its less toxic than the often used methylene chloride [19]. In comparison to methylene chloride, ethyl acetate is highly soluble. Hence, the micro-particles cannot form properly if the disperse phase is directly introduced in the continuous one. Due the sudden extraction of ethyl acetate the polymer precipitated into fibre-like agglomerates [10]. According to Li et al. [19] three methods can be used to resolve this problem:

- 1. The aqueous solution could be pre-saturated with solvent to slow down the extraction and prevent agglomerates.
- 2. The dispersed phase could be first emulsified in a little amount of continuous phase for the formation of the drops. After that this solution could be led into larger amount of continuous phase where the main part of the ethyl acetate is extracted.
- 3. The dispersed phase could again be emulsified in a little amount of continuous phase. This solution is then agitated and trough the evaporation of the solvent the solidification of the micro-particle occurs.

# **3.2.2. Benzyl alcohol**

In the investigated process benzyl alcohol was used as the solvent of the API. It is an organic compound with the formula  $C_6H_5CH_2OH$ , a low toxicity, good solubility characteristics and a low vapor pressure.

# **3.2.3.** Polyvinyl alcohol (PVA)

The polyvinyl alcohol is a protective colloid and was used to stabilize the emulsion droplets after the emulsification. It is a non-ionic surfactant which has excellent film forming, emulsifying, and adhesive properties [19].

### 3.2.4. Polymer (PLGA)

PLGA or poly (lactic-co-glycolic acid) is a copolymer and is most frequently used as the biomaterials for the microencapsulation of therapeutics [9]. It provides an excellent biocompatibility and biodegradability and the applications in humans are approved by the FDA (Food and Drug Administration) [19].

# **3.3.** Preparation of the Solutions

The different required solutions respectively phases, as described in Chapter 2, had to be prepared separately.

The ingredients and the weighted sample of the three needed phases (the organic, the liquid and the continuous phase) are listed in Table 3-1 and Table 3-2. The different used chemicals are described in section 3.2.

The organic phase was prepared in two parts to prevent mutual interference between the different ingredients during the dissolution process of the PLGA and the API.

One consisted of the polymer (PLGA) and its solvent ethyl acetate, while the other one consisted of the API and its solvent benzyl alcohol. The first solution was stirred magnetically at 1200 rpm and the other one at 600 rpm for 15 minutes, respectively. After that they were combined and stirred together at 600 rpm for 2 minutes. To decompose the weight of the polymer to 80000 Dalton the organic phase was tempered for 3 hours in a water bath at 20 °C.

The liquid and the continuous phases were produced by mixing the different ingredients together. The liquid phase consisted of ethyl acetate and polyvinyl alcohol (PVA) and the ingredients of the continuous phase were water and ethyl acetate.

Ethyl acetate	Water		
[g]	[g]		
83,03	3440,00		

Table 3-1: Ingredients of the first continuous phase.

#### Table 3-2: Ingredients of the disperse phase.

Organic Phase			Liqu	iid Phase	
Polymer	API	Ethyl acetate	Benzyl alcohol	PVA	Ethyl acetate
[g]	[g]	[g]	[g]	[ml]	[g]
8,80	6,13	44,76	18,90	635,00	45,00

### 3.3.1. Mixing Step

At the beginning the reactor was filled with the continuous phase and was cooled down to  $5 \,^{\circ}$ C. For the whole process the stirrer rate was set to 260 rpm.

In the mixing step the organic phase was emulsified into the liquid phase generating the initial stage of micro-particle shaping. Therefore, the two phases were pumped through a static mixer unit with two gear pumps. The different influences like speed and volume flow on the resulting emulsion droplet size and their distribution are presented in a publication from Kiss et al. [22].

### **3.3.2.** First Extraction Stage

The produced emulsion was then led trough a custom build glass device in the reactor unit. There the two solvents (ethyl acetate and benzyl alcohol) were extracted into the surrounding aqueous continuous phase. As a consequence of the decrease of ethyl acetate concentration inside the micro-particles, which is the solvent of the polymer (PLGA), the emulsion droplets transformed into semi-solid micro-particles.

#### **3.3.3. Intermediate Drying Stage**

The first extraction step was assessed to be finished after 20 hours. In the intermediate drying stage the semi-solid particles were separated from the slurry. Afterwards the whole solution of the reactor was filled in a custom build vacuum-sieve-drying unit and the most of the aqueous phase was removed. The remaining micro-particles were dried with air for 24 hours at -5  $^{\circ}$ C.

#### **3.3.4. Second Extraction Stage**

After the intermediate drying stage the dried micro-particles were suspended again and a second extraction step with a different continuous phase was conducted. The temperature and the stirrer rate were held constant. The ingredients and weighted sample of the second continuous phase are listed in Table 3-3.

Ethanol	hanol Water		
[ml]	[ml]		
1000,00	3000,00		

.f 41 **T 11 22 T** ٦. nta . . : . .

# **3.3.5. Final Drying Stage**

At the end the micro-particles were dried again in the custom build vacuum-sieve-drying unit for about 5 days at -5 °C. When the water content and the residual solvent content of the micro-particles was under 0.2 mass percent this final drying process was over.

# **3.4.** Overview over the Experimental Set up

For the detailed investigation of the process an experimental installation was build up in the laboratories of the Research Center Pharmaceutical Engineering (RCPE GmbH) in Graz. A picture of the final experimental installation is shown in Figure 3-2, while P&ID-Flow Diagram of the process is shown in Figure 3-3. The most important units are described in the following sub-sections.



Figure 3-2: Experimental installation.



### 3.4.1. Mixer Unit

The emulsification of the organic and liquid phase is a very important step for the whole process. In fact, the final size of the micro-particles could be directly related to the size of the emulsion droplets. In our case the emulsions were produced by pumping the liquid and the organic phase with two Ismatec MCP-Z IP 65 gear pumps trough a custom build static mixer unit. After this static mixer unit the produced emulsion droplets were led into the reactor unit. In Figure 3-4 the mixer unit is shown. The most important facts about the gear pumps and there pump heads are summarized in Table 3-4, Table 3-5 and Table 3-6.



Figure 3-4: Mixer unit.

<b>Flow rates</b> <sup><math>1</math></sup>	1 - 7020	[ml/min]	
Motor speed	60 - 6000	[rpm]	
Speed setting	digital speed setting	(resolution 1 rpm)	
Calibrating functions	<ul><li> for flow rate [ml/min]</li><li> for dispensing volume [ml]</li></ul>		
Power consumption	150	[W]	
Weigth	6,9	[kg]	

# Table 3-4: Data sheet of the gear pumps (MCP-Z IP 65). **ISMATEC MCP-Z IP 65**

## Table 3-5: Data sheet of the gear pump head (Z-120).

ISMATEC	Magnetically	coupled (	<b>Cavity Style</b>	numn h	nead Z-120
DUNILL	magnetically	coupieu c	Javily Digit	pump n	

38 - 3840	[ml/min]
3,5 / 50,8	[bar/psi]
21 / 304,6	[bar/psi]
-46 +54	[°C]
	PTFE
	PTFE
	SS316
	38 - 3840 3,5 / 50,8 21 / 304,6 -46 +54

<sup>&</sup>lt;sup>1</sup> depending on mounted pump-head <sup>2</sup> Flow rates without differential pressure <sup>3</sup> With other seals up to 99°C possible

ISMATEC Magnetically coupled Suction shoe style pump head Z-186			
Flow rates	1 - 102	[ml/min]	
Differential pressure	1,4 / 20,3	[bar/psi]	
System pressure, max	21 / 305	[bar/psi]	
<b>Operating temperature</b> <sup>4</sup>	-46 +177°C	[°C]	
Gear Material	Grap	bhite	
Seals	PT	FE	
Stainless steel housing	SS3	316	

Table 3-6: Data sheet of the gear pump head (Z-186). SMATEC Magnetically coupled Suction shoe style pump head Z-180

The custom build static mixer unit consisted of ten mixer elements (SMX elements) build from Sulzer Chemtech AG and a custom build housing from Bamberger & CO. The mixer elements were cast of stellite and were placed into a camber in the housing. The different parts of the housing were then locked together with four TRI-Clamps.

The custom build housing was made of austenitic stainless steel 1.4404. In Figure 3-5 one SMX element is shown.



Figure 3-5: Mixer elements.

 $<sup>^4</sup>$  With other seals up to 99°C possible

#### 3.4.2. Reactor Unit

As described before, the produced emulsion droplets were led into the 5 liter double jacket lab reactor trough a custom build glass device. In Figure 3-6 the complete set up of the reactor unit is shown.



Figure 3-6: Reactor unit.

This lab reactor was made out of glass by Ruprechter Glasbläserei-Laborbedarf e.U. and its engineering drawing can be found in the Appendix.

The reactor was stirred by an impeller build by Schmizo AG. The shaft of the stirrer was made out of glass and the blade consisted of PTFE. The engineering drawing of the stirrer unit can be found in the Appendix as well.

#### 3.4.3. Cooling Unit

During the extraction process the liquids in the reactor unit had to be tempered constantly under 5 °C in order not to excess the glass transition temperature of the polymer. This was achieved by a refrigerated/heating circulator (F 25 ME), shown in Figure 3-7, build by Julabo Labortechnik GmbH. This circulator was connected with silicon tubes to the double jacket lab reactor. To provide the needed temperature, Glycol was used as cooling liquid. In Table 3-7 the most important parameters about the circulator are summarized.



Figure 3-7: Cooling unit.

Table 3-7: Data sheet of the circulator.

#### Julabo F 25 ME

Working temperature range	-28	+200	[°	[°C]	
Temperature stability	0,01		[°C]		
Heater capacity	2000		[W]		
Filling volume	4,5		[liters]		
Ambient temperature	5 +40		[°C]		
Cooling capacity	20	0	-20	[°C]	
	350	250	60	[W]	

# 4. Experimental Work

# 4.1. Introduction

The main target of the experimental work was to monitor the micro-particle size during the extraction process. Therefore, two measurements systems from Sympatec GmbH, namely HELOS, a laser diffraction system, and QICPIC, an image analysis system, were used. These two systems are described in section 4.2.

Basically, experimental data were produced, in cooperation with M. Sc. Nikolett Kiss, in order to validate the numerical model developed in Chapter 5. This validation is presented in sub section 6.5.

# 4.2. Particle Size Analysis

# 4.2.1. HELOS

The HELOS (Helium-Neon Laser Optical System), shown in Figure 4-1, is a laser diffraction sensor from Sympatec GmbH. This system uses one measuring principle (laser diffraction in the parallel laser beam) for the its whole measuring range from 0.1  $\mu$ m to 8750  $\mu$ m.



Figure 4-1: HELOS/BR and wet disperser CUVETTE 50ML/US for small sample quantities [37].

The supplied software, WINDOX, offers two different evaluation modes, which allows the analysis of extremely wide size distributions at highest precision:

- FREE: a parameter free solution basing on Fraunhofer diffraction
- MIEE: basing on precision Mie theory extended to the full size range

The classical field of application is the particle size analysis of dry and wet samples, i.e. of powders, suspensions, emulsions or sprays and the absolute accuracy is typically within  $\pm 1\%$  with respect to the standard metre.

The HELOS analysis system combines high resolution and guaranteed reproducibility with high speed data acquisition.

### 4.2.2. QICPIC

The QICPIC, shown in Figure 4-2, is an image analysis system from Sympatec GmbH which combines particle size with shape analysis for particles with a speed of up to 100 m/s. For dry particles, a dispersion unit guarantees proper dispersion of agglomerated fine and cohesive powders. In addition it is also possible to apply wet disperser as LIXELL and SUCELL for the analysis of emulsions and suspensions.



Figure 4-2: Particle size analysis of suspensions and emulsion with the wet disperser LIXELL inserted in the measuring zone of a QICPIC [38].

The QICPIC analysis system is able to measure particles between 1  $\mu$ m and 20 mm and the high performance data compression allows grabbing up to 500 images per second. These leads to a high statistical security of measurement results in short analysis time

Besides that the supplied software, WINDOX, is capable of simultaneous calculate different size and shape features.

In addition QICPIC fulfills the security requirements of the FDA and is compliant to 21 CFR Rule 11.

# 4.3. Micro-Particle Sizing during the Extraction Process

The size distribution of the micro-particles, during the extraction process, was determined using the HELOS laser diffraction instrument. At different instants of time, samples were taken out of the extraction reactor and the micro-particle size was determined right away to avoid aging influences. Therefore the samples were filled into a cuvette provided by Sympatec GmbH and measured in triplicate. The Fourier optic R5, which has a drop size measuring range from 0,5/4,5 to 875 µm, was here used. The evaluations of the different diffraction patterns were evaluated with the FREE (Fraunhofer Enhanced Evaluation) mode which is provided from the evaluation software.

#### Median value x<sub>50</sub>:

The median value is defined as the particle diameter that corresponds to a cumulative distribution  $Q_3$  of 50 %. This value divides the density distribution  $q_3$  into two equal halves.

#### Sauter mean diameter SMD/d<sub>32</sub>:

The Sauter mean diameter SMD is defined as the diameter of that spherical particle which has exactly the same volume/surface area ratio as a particle of interest. It's commonly in literature defined as:

$$d_{32} = \frac{\sum_{i} N_{i} d_{i}^{3}}{\sum_{i} N_{i} d_{i}^{2}}$$
(4-1)

Here,  $N_i$  is the number and  $d_i$  is the diameter of the particles of interest.

# 5. Modeling

# 5.1. Introduction and MATLAB Overview

The final quality of the considered micro-particles can be predicted and controlled only by a deep understanding of each step of the production process, namely mixing, hardening/extraction and drying.

As described in this section, the modeling of the diffusion process was one of the main challenges of this work. The developed numerical method was based on the MATLAB software from MathWorks Inc. The MATLAB environment and its solvers are commonly used for technical computing and data visualization in many engineering fields.

Concerning the structure of this chapter first of all the developed mass transport model is described in detail. Then the estimation procedure of the mass transport coefficient and the diffusion coefficient are declared. Afterwards an overview over the MATLAB-PDEPE solver is given. Then the analytical verification of the model without shrinking is presented. Finally the method to numerically compute the diameter reduction respectively the shrinking model is presented.

All the different code parts concerning the numeric model can be found in the appendix.

# 5.2. Diffusion Model

### 5.2.1. Mass Transport Model

As described in chapter 3, the extraction process is a process with four different components:

- 1. Solvent (Ethylacetate)
- 2. Co-Solvent (Benzylalcohol)
- 3. Polymer
- 4. API

Basically, the mass transfer in the micro-particle can be assumed to be a multicomponent diffusional process. The chosen approach to resolve this physical problem is based on the work of Li et al. [18].

Here, the continuity equation for multiple component diffusion for an infinitesimal volume can be written as follows:

$$\frac{\partial \phi_i}{\partial t} = -\nabla \cdot (J_i + \phi_i v_3) \tag{5-2}$$

where i represent the four different components in the disperse phase,  $\phi_i$  is the volume fraction,  $J_i$  is the volume flux relative to the polymer velocity and  $v_3$  is the velocity of the polymer.

For a first analysis of the problem the term  $v_3$  was assumed to be equal to zero, meaning that the shrinking of the particle was considered negligible. For the development of the mathematical model the following assumptions have been made:

- The particles were assumed to be spherical and uniformly distributed in  $\varphi$  and  $\theta$ .
- The porosity of the micro-particles was neglected.
- It was assumed that there were no interactions between the different components which mean that the different components can diffuse independently from each other.

The volume flux is defined as follows:

$$J_{i} = \frac{1}{r} \frac{D_{i}}{RT} \nabla_{r_{n}} \mu_{i}$$
(5-3)

where  $D_i$  is the concentration-dependent binary diffusion coefficient, R is the gas constant, T is the temperature and  $\mu_i$  is the chemical potential for each component i.

The normalized position variable of the micro-particle r<sub>n</sub> is defined as follows:

$$r_n = \frac{r}{r_{max}}$$
(5-4)

Here r is the position vector and  $r_{max}$  is the radius of the micro-particle.

With the presented assumptions and the equation found by Bird et al. [4], the equation can be transformed in:

$$\frac{\partial \varphi_{i}}{\partial t} = \frac{1}{r^{2}} \cdot \frac{\partial}{\partial r} \cdot \left( \frac{r^{2}}{R \cdot T} \cdot D_{i} \cdot \frac{\partial \mu_{i}}{\partial r} \right)$$
(5-5)

The chemical potential for this system can be expressed as a function of different interaction parameters and of the volume fraction of the different components. As described before a four component system was assumed. Since the API loading was generally low the polymer and API were considered as one component. According to Tompa et al. [31] and Flory et al. [8], the chemical potential for the solvent i is defined as:

$$\frac{\Delta \mu_{i}}{RT} = \ln(\varphi_{1}) - \alpha \varphi_{2} - \beta \varphi_{3} - \gamma \varphi_{4} + (1 + \chi_{12}\varphi_{2} + \chi_{13}\varphi_{3} + \chi_{14}\varphi_{4})(1 - \varphi_{1}) - \alpha \chi_{23}\varphi_{2}\varphi_{3} - \gamma \chi_{34}\varphi_{3}\varphi_{4} - \beta \chi_{24}\varphi_{2}\varphi_{3}$$
(5-6)

where  $\alpha$ ,  $\beta$ ,  $\gamma$  are the ratios of the molar volumes  $\overline{v}_i$  which can obtain from the Eqn. (5-7) and  $\chi_{ij}$  represent the binary interaction parameter.

$$\alpha = \frac{\overline{v}_1}{\overline{v}_2}, \beta = \frac{\overline{v}_1}{\overline{v}_3}, \gamma = \frac{\overline{v}_1}{\overline{v}_4}$$
(5-7)

The molar volume for the component i is defined as follows:

$$\overline{v}_{i} = \frac{M_{i}}{\rho_{i}}$$
(5-8)

where  $M_i$  is the molar mass and  $\rho_i$  is the mass density.

The presented Eqn. (5-6) represents the chemical potential for a quaternary system and can be simplified during the formation stage into a ternary system which can be rewritten as:

$$\frac{\Delta\mu_{i}}{RT} = \ln(\varphi_{1}) - \alpha\varphi_{2} - \beta\varphi_{3} + (1 + \chi_{12}\varphi_{2} + \chi_{13}\varphi_{3}) - \alpha\chi_{23}\varphi_{2}\varphi_{3}$$
(5-9)

And for the solvent removal stage the chemical potential is defined as:

$$\frac{\Delta \mu_{i}}{RT} = \ln(\varphi_{1}) - \beta \varphi_{3} - \gamma \varphi_{4} + (1 + \chi_{13}\varphi_{3} + \chi_{14}\varphi_{4})(1 - \varphi_{1})$$

$$- \gamma \chi_{34}\varphi_{3}\varphi_{4}$$
(5-10)

The Eqn. (5-9) and Eqn. (5-10) are the final expressions of the chemical potential for a ternary system as described in literature (see e.g. Li et al. [18]).

The binary interaction parameter  $\chi_{ij}$ , the gas constant R, the process temperature T and also the ratios of the molar volumes  $\alpha$ ,  $\beta$ ,  $\gamma$  remain constant throughout the entire process. These constants may also be neglected for the modeling.

The final differential equation for the mass transfer in the micro-particle is shown in (5-11):

$$\frac{\partial \phi_{i}}{\partial t} = \frac{1}{r^{2}} \cdot \frac{\partial}{\partial r} \cdot \left( r^{2} \cdot D_{i} \cdot \frac{\partial \phi_{i}}{\partial r} \right)$$
(5-11)

The terms on the left hand side are they so-called accumulation terms, while the terms on the right hand side are the so-called diffusion terms.

#### 5.2.2. Initial and Boundary Conditions

In order to solve the above-presented differential equation, the MATLAB PDEPE solver was used (please see section 5.3 for more details about this module).

The initial condition for the volume fraction  $\phi_i$  of the component i is defined as:

$$\varphi_{i(r,t=0)} = \varphi_i^0 \quad i = 1,2,4$$
 (5-12)

At the beginning (t=0) all components were equally distributed and the volume fraction was determined by the initial composition of the different components.

The first boundary condition for the volume flux of the component i is:

$$J_{i(0,t)} = 0 (5-13)$$

This boundary applied no volume flow at the center of the micro-particle and is also called regularity condition.

The second boundary condition describes the mass flow from the interface of the microparticle into the continuous phase:

$$-D_{i} \cdot \frac{\partial \varphi_{i,r=R}}{\partial r} = \beta_{i,t} \cdot \Delta \varphi$$
(5-14)

Here,  $D_i$  is the binary diffusion coefficient,  $\beta_{i,t}$  is the mass transport coefficient and  $\Delta \phi$  is the volume fraction difference between the disperse and the continuous phase.

According to the formulation of the film theory [2], the mass transfer between particle (disperse phase) and extraction medium (continuous phase) depends on the mass transfer coefficient and the volume fraction difference between the interface and the continuous phase, namely  $\phi_{DP,i,\infty}$  and  $\phi_{CP,i,\infty}$ .

Generally, the transport process can be divided into three components:

- Transport of component i from the disperse phase to the interface;
- Transport of component i through the interface;
- Transport of component i from the interface into the continuous phase.

A schematic representation of the volume fraction profiles of component i at the interface between disperse and continuous phases is shown in Figure 5-1.



Figure 5-1: Schematic representation of the volume fraction profiles of component  $\phi_i$  at the interface.

$$\begin{array}{ll} \phi_{i,DP,\infty} & \mbox{Volume fraction in the DP} \\ \phi_{i,CP,\infty} & \mbox{Volume fraction in the CP} \\ \phi^{*}{}_{i,DP,I;} \phi^{*}{}_{i,CP,I} & \mbox{Equilibrium volume fraction at the interface} \\ & \beta_{i} & \mbox{Mass transfer coefficient} \\ & \mbox{D}_{i,DP}; \mbox{D}_{i,CP} & \mbox{Diffusion coefficient in the DP and CP} \\ & \mbox{\delta}_{CP} & \mbox{Interface thickness} \end{array}$$

The transport through the interface is usually assumed to be unresisting. Therefore, the thickness of the interface is regarded to be infinitely thin. Another assumption is that phase equilibrium is present at the interface.

Generally, the mass transport for a liquid-liquid system can be defined by Eqn. (5-15) to Eqn. (5-18).

$$\dot{\mathbf{n}}_{i,\text{DP}} = \beta_{i,\text{DP}} \cdot (\varphi_{i,\text{DP},\infty} - \varphi^*_{i,\text{DP},\text{I}})$$
(5-15)

$$\dot{n}_{i,CP} = \beta_{i,CP} \cdot (\varphi_{i,CP,I}^* - \varphi_{i,CP,\infty})$$
(5-16)

$$\dot{\mathbf{n}}_{\mathbf{i}} = \dot{\mathbf{n}}_{\mathbf{i},\mathsf{CP}} = \dot{\mathbf{n}}_{\mathbf{i},\mathsf{DP}} \tag{5-17}$$

$$\dot{n}_{i} = \frac{1}{\frac{1}{\beta_{i,DP}} + \frac{1}{K \cdot \beta_{i,CP}}} \cdot \left(\varphi_{i,DP,\infty} - \frac{1}{K} \cdot \varphi_{i,CP,\infty}\right)$$
(5-18)

Here,  $\dot{n}_i$  is the molar flow,  $\beta_{i,j}$  and  $\phi_{i,j,\infty}$  are the mass transport coefficient and the volume fraction of the component i in the phase j, respectively, while K is the equilibrium constant, also known as Nernst distribution coefficient.

In our approach, the mass transport in the disperse phase was modeled through a multicomponent diffusion model. The exact algorithm to determine the value of the mass transport coefficient  $\beta_{i,CP}$  for the continuous phase is presented in section 5.2.3. Furthermore, this coefficient depends on the diameter of the micro-particle and is a time-dependent value.

The equilibrium constant K is defined as follows:

$$K = \frac{\varphi^*_{CP,i,I}}{\varphi^*_{DP,i,I}} \gg 1$$
(5-19)

The value of K becomes strongly greater than 1 concerning the big volume difference between the continuous and disperse phase on the one hand and the fact that the saturation concentration for the solvents in the continuous phase is definitely higher than for the disperse phase on the other hand.

This means that the concentration of the two solvents in the continuous phase could be negligible and set equal to zero for the entire process. As a consequence of that assumption the extracted components diffuse very fast from the interface into the continuous phase.

#### 5.2.3. Estimation of the Mass Transport Coefficient

The mass transport rate from the interface of the micro-particles into the continuous phase basically depends on the mass transport coefficient  $\beta_i$  and the ambient concentration  $\phi_{i,CP,\infty}$ . Moreover, the value of  $\beta_i$  is highly dependent on the surrounding flow regime, on the diameter of the micro-particle  $d_{P,t}$  and on the binary diffusion coefficient  $D_i$  of the solvent i in the continuous phase. The mass transfer coefficient is usually expressed as a function of the Sherwood number Sh, the binary diffusion coefficient  $D_i$  and the diameter of the micro-particle  $d_{p,t}$  as follows:

$$Sh = \frac{\text{convective mass transfer coefficent}}{\text{diffusive mass transfer coefficent}} = \frac{\beta_i \cdot d_{P,t}}{D_i}$$
(5-20)  
$$\beta_i = \frac{D_i \cdot Sh}{d_{P,t}}$$

The dimensionless Sherwood number represents the ratio of convective to diffusive mass transport and can be expressed as function of Reynolds and Schmidt numbers.

$$Sh = f(Re, Sc) \tag{5-21}$$

The dimensionless Reynolds number represents the ratio of inertial forces to viscous forces and is used to determine whether a flow will be laminar or turbulent.

$$Re = \frac{\text{inertial forces}}{\text{viscous forces}} = \frac{v \cdot d_{P,t}}{\gamma_{CP}}$$
(5-22)

Here, v is mean velocity of the object relative to the fluid and  $\gamma_{CP}$  is the kinematic viscosity of the continuous phase.

As presented above, the mass transport coefficient depends on the diameter of the microparticle. This means that in a shrinking process its value changes over time. For our case, the mean fluid velocity in the extraction tank was estimated with a correlation found by Kolmogoroff for isotropic turbulence:

$$\mathbf{v} = \mathbf{v}_0 \cdot \left(\frac{\mathbf{d}_{\mathrm{P,t}}}{\mathbf{d}_{\mathrm{R}}}\right)^{\frac{1}{3}} = \pi \cdot \mathbf{n} \cdot \mathbf{d}_{\mathrm{R}} \cdot \left(\frac{\mathbf{d}_{\mathrm{P,t}}}{\mathbf{d}_{\mathrm{R}}}\right)^{\frac{1}{3}}$$
(5-23)

where n is the revolution rate of the stirrer and  $d_R$  is the diameter of the stirrer blade.

The dimensionless Schmidt number Sc is the ratio of momentum diffusivity (viscosity) and mass diffusivity, expressed in terms of kinematic viscosity  $\gamma_{CP}$  and binary diffusion coefficient D<sub>i</sub>.

$$Sc = \frac{viscous \text{ diffusion rate}}{mass \text{ diffusion rate}} = \frac{\gamma_{CP}}{D_i}$$
(5-24)

The Schmidt number is used to characterize fluid flows in which momentum and mass diffusion-convection processes happen simultaneously.

There are many empirical and semi-empirical correlations to express the dimensionless Sherwood number as a function of the Reynolds and Schmidt numbers shown in equations Eqn. (5-22) and Eqn. (5-24). The correlations listed in Table 5-1 were found by different researchers and are described in a book from Tosun [32]. All these correlations are only valid for a certain range of Reynolds and the Schmidt number.

	Reynolds number	Schmidt number	Sherwood number
	Re	Sc	Sh
Garner/Suckling	100 ÷ 700	1100 ÷ 2200	$2 + 0.95 \cdot \sqrt{\text{Re}} \cdot \text{Sc}^{\frac{1}{3}}$
Frössling	> 100	$\leq 1000$	$2 + 0.552 \cdot \sqrt{\text{Re}} \cdot \text{Sc}^{\frac{1}{3}}$
Steinberger/Treybal	10 ÷ 17000	$1 \div 70000$	$2 + 0.347 \cdot \text{Re}^{0.62} \cdot \text{Sc}^{0.31}$
Rowe et al.	25 ÷ 1150	1220	$0.79 \cdot \sqrt{\text{Re}} \cdot \text{Sc}^{\frac{1}{3}}$

As shown in Table 5-2, the values from Reynolds and Schmidt numbers at the beginning fit the correlation found by Steinberger and Treybal exactly, namely Reynolds number from 10 to 17000 and a Schmidt number from 1 to 70000. Therefore, this correlation was used for further calculations.

Table 5-2: Values of Reynolds and Schmidt number.					
	Reynolds number Schmidt number		Sherwood number		
	Re	Sc	Sh		
Ethylacetate		8,680	6,160		
Benzylalcohol	18,628	8,980	6,200		

#### **5.2.4. Diffusion Coefficient**

As mentioned in section 5.1, the differential equations were solved with MATLAB. The different code parts concerning the calculation of the value of the binary diffusion coefficient can be found in the appendix. At the beginning of the extraction process, the binary diffusion coefficient could be estimated with an equation from Hayduk and Minhas [30]:

$$D_{i} = 1,25 \cdot 10^{-8} \cdot (V^{-0,19} - 0,292) \cdot T^{1,52} \cdot \eta^{\epsilon_{b}}$$
(5-25)

where V is the molar volume of solute of solute at normal boiling point, T is the temperature and  $\eta$  is the dynamic viscosity. The term  $\epsilon_b$  is defined as:

$$\epsilon_{\rm b} = \frac{9,58}{\rm V} - 1,12$$
 (5-26)

This equation is valid for liquid-liquid system and represents a good approach to find initial values for the binary diffusions coefficient for each solvent.

Another correlation for the binary diffusion coefficient was found by Wilke and Chang [36]. This equation is also valid for diffusion in water and in non-associated solvents.

$$D_{i} = 7,4 \cdot 10^{-8} \cdot \frac{(x \cdot M)^{\frac{1}{2}} \cdot T}{\eta \cdot V^{0,6}}$$
(5-27)

Here, M is the molecular weight of solvent and x is an association parameter.

The following paragraph is cited from their paper [36].

"The correlation represented by equation 19 is satisfactory for estimation of diffusion coefficient in dilute solution with sufficient precision for most engineering purposes, i.e., about 10% average error<sup>5</sup>. It must be emphasized that the diffusion process is extremely complex and that any rigorous treatment must consider solute-solvent interaction in a more detailed manner that the present

<sup>&</sup>lt;sup>5</sup> For 285 points among 251 solute-solvent systems of this study

relation could possibly imply<sup>6</sup>. Although the present functional relationship of diffusion coefficient to solute molar volume rests upon some qualitative theoretical foundation, the relationship to solvent molecular weight is strictly empirical."

Both above described correlations provide different starting values for the binary diffusion coefficient. The correlation found by Wilke and Chang [36] is typically used in literature (see e.g. Wang et al. [35]), so it was also used in our work.

As described before, the extraction of the solvents leads to the hardening of the microparticle. Furthermore, with the increase of the volume fraction of the polymer the value of the diffusion coefficient decreases. This means that the diffusion coefficient is highly depending on the polymer volume fraction in the micro-particle. The correlation between the diffusion coefficient and the volume fraction of the solvent was found by Reuvers et al. [25] and used in the work by Li et al [18] and can be written as:

$$D_{i} = r_{1,i} \cdot 10^{-(r_{2,i} + r_{3,i} \cdot \varphi_{P})}$$
(5-28)

Where the parameters  $r_{1,i}$ ,  $r_{2,i}$  and  $r_{3,i}$  are system dependent constants and  $\varphi_P$  is the volume fraction of the polymer.

<sup>&</sup>lt;sup>6</sup> Diffusion of iodine in aromatic hydrocarbons, for example, has been excluded from the present correlation because of known complex formation.

# **5.3. PDEPE Solver Description**

In order to solve the one-dimensional parabolic-elliptic partial differential equations (PDE) described in the previous sections, the MATLAB-PDEPE solver was used and the system of equations was implemented in MATLAB 7.9.0 R2009b. All the different code parts can be found in the appendix.

In the following chapter an overview of the numerical solution method is given. The following description is a summary/abstract of several instructions which can be found in the books "MATLAB kompakt" by Schweizer [29] and "MATLAB guide" by Desmond et al. [14], as well as in the MATLAB product help [1].

Basically, the MATLAB's PDEPE solves a class of parabolic/elliptic PDE systems. "These systems involve a vector-valued unknown function u that depends on a scalar space variable, x, and a scalar time variable, t." [14]

The PDEPE algorithm is based on the discretization of the space variable, xmesh, and uses a second-order spatial discretization method based on the xmesh values. This means that the choice of xmesh has a strong influence on cost and accuracy of the numerical solution.

The generated system of ordinary differential equations is then solved by the routine "ode15s". This routine is a variable order solver based on the numerical differentiation formulas (NDFs), which is capable of solving stiff DAE systems.

Generally, the PDEPE module in MATLAB solves PDEs of the form:

$$\mathbf{c} \cdot \left(\mathbf{x}, \mathbf{t}, \mathbf{u}, \frac{\partial \mathbf{u}}{\partial \mathbf{x}}\right) \cdot \frac{\partial \mathbf{u}}{\partial \mathbf{t}} = \mathbf{x}^{-\mathbf{m}} \cdot \frac{\partial}{\partial \mathbf{x}} \cdot \left(\mathbf{x}^{\mathbf{m}} \cdot \mathbf{f}\left(\mathbf{x}, \mathbf{t}, \mathbf{u}, \frac{\partial \mathbf{u}}{\partial \mathbf{x}}\right)\right) + \mathbf{s} \cdot \left(\mathbf{x}, \mathbf{t}, \mathbf{u}, \frac{\partial \mathbf{u}}{\partial \mathbf{x}}\right)$$
(5-29)

The solution function  $u_{(x,t)}$  is limited to the finite space interval  $a \le x \le b$  and the time interval  $t_0 \le t \le t_f$ . The exponent m can be 0, 1, or 2, corresponding to slab, cylindrical, or spherical symmetry, respectively. The function c is a diagonal matrix and the flux and source function f and s are vector valued.

For  $a \le x \le b$ , thus all positions x of the discretized domain, and  $t = t_0$  the solution components satisfy initial conditions of the form:

$$u_{(x,t_0)} = u_{0(x)} \tag{5-30}$$

For x=a and all times t ( $t_0 \le t \le t_f$ ) the solution must satisfy Eqn. (3-31) for particular functions  $p_a$  and  $q_a$ :

$$p_{a(x,t,u)} + q_{a(x,t)} \cdot f\left(x, t, u, \frac{\partial u}{\partial x}\right) = 0$$
(5-31)

Similarly, for x=b and all times t ( $t_0 \le t \le t_f$ ),

$$p_{b(x,t,u)} + q_{b(x,t)} \cdot f\left(x, t, u, \frac{\partial u}{\partial x}\right) = 0$$
(5-32)

must hold for particular functions  $p_b$  and  $q_b$ . Elements of  $q_a$  and  $q_b$  are either identically zero or never zero.

A call to PDEPE has the general form

The input parameter m corresponds to the above-discussed symmetry parameter and can take the values 0, 1 and 2. The vector xmesh defines the x values at which the numerical solution is computed. The vector tspan specifies the time points where the solution is to be returned.

"The time integration in pdepe is performed by "ode15s" and the actual timestep values are chosen dynamically-the tspan points simply determine where the solution is returned and have a little impact on computational cost or accuracy. The default properties of the "ode15s" can be overridden via the optional input argument options.

The output argument sol is a three-dimensional array such that sol(j,k,i) is the approximation to the i-th component of u at the point t=tspan(j) and x=xmesh(k)." [14]

The function pdefun has the form:

function [c, f, s] = pdefun(x, t, u, DuDx)

and accepts the space and time variables together with the vectors u and DuDx, which approximate the solution u and the partial derivate  $\partial u \partial x$ . "The function returns vectors containing the diagonal of the matrix c, as well as the flux and source functions f and s. Initial conditions are encoded in the function pdeic, which takes the form:

function 
$$u0 = pdeic(x)$$

Finally, the function pdebc, defined as

function [pa, qa, pb, qb] = pdebc(xa, ua, xb, ub, t, p1, p2, ....)

evaluates  $p_a$ ,  $q_a$ ,  $p_b$  and  $q_b$  for the boundary conditions at xa=a and xb=b.

The remaining input arguments p1, p2, ... are optional problem parameters that are passed to the functions pdefun, pdeic and pdebc." [14]

# 5.4. Analytical Verification without Shrinking

To prove the solution of Eqn. (5-11) with the boundary conditions in Eqn. (5-13) and Eqn. (5-14), the numerical results were compared with an analytical solution of a similar system. Precisely, the solution for surface evaporation found by John Crank [7] was used as an analytical benchmark for the discretized method used in this work. To compare the above presented numerical algorithm with the analytic one, the same parameters must be used. The assumption and most important parameters are listed below. The whole MATLAB code for the solution for surface evaporation was provided by Dipl.-Ing. Radl. The analytic verification without shrinking is attached in the appendix.

To compare the concentration used in the equations by Crank [7] and the volume fraction used in our algorithm, the molar density of every component was set to one. This assumption enables a direct comparison between analytical and numerical solution. The equations showed below are all found in the book "Mathematics of Diffusion" by Crank [7]. At the beginning the sphere is initially at a uniform concentration  $C_i$  and there is a surface condition:

$$-D_{i}\frac{\partial C}{\partial r} = \beta_{i} \cdot (C_{S} - C_{0})$$
(5-33)

Where  $D_i$  is the binary diffusion coefficient,  $\beta_i$  is the mass transport coefficient, r is the radial position,  $C_s$  is the actual concentration just within the sphere, and  $C_0$  is the concentration required to maintain equilibrium with the surrounding atmosphere. According to Crank [7], the analytical solution for this problem can be written as:

$$\frac{C_{\rm S} - C_0}{C_{\rm i} - C_0} = \frac{2 \cdot \text{Bi}}{r_{\rm n}} \cdot \sum_{n=1}^{\infty} \frac{\exp \left(-\text{Fo} \cdot \alpha_n^2\right)}{\{\alpha_n^2 + \text{Bi}(\text{Bi} - 1)\}} \cdot \frac{\sin(\alpha_n \cdot r_n)}{\sin(\alpha_n)}$$
(5-34)

Here,  $r_n$  is the normalized radius, which is correlated to the maximum radius of the sphere  $r_{max}$  as:

$$r_n = \frac{r}{r_{max}}$$
(5-35)

The dimensionless mass Fourier number is used in the analysis of unsteady transfer processes [12] and can be expressed as:

$$Fo = \frac{t \cdot D_i}{r_{max}^2}$$
(5-36)

The terms  $\alpha_n s$  are the roots of

$$\alpha_{n}\cot(\alpha_{n}) + Bi - 1 = 0 \tag{5-37}$$

Some of the roots can be found in the book "Mathematics of Diffusion" by Crank [7]. The Biot number is defined as:

$$Bi = \frac{r_{max} \cdot \beta_i}{D_i}$$
(5-38)

The dimensionless mass transfer Biot number is used to characterize non-steady-state (or transient) mass diffusion processes.

These equations were also solved with MATLAB, and the results were compared with the numerical ones. The comparison of these calculations is presented in Figure 5-2. The deviation between the numeric and analytic results at the inner  $r_{min}$  and the outer radius  $r_{max}$  is shown in Figure 5-3 and can be obtained from Eqn. (5-39). Here,  $\phi_{Analytical,i,r,t}$  is the analytic and  $\phi_{Numerical,i,r,t}$  is the numerical found value for the volume fraction.

Deviation = 
$$\left(\frac{\varphi_{\text{Analytical,i,r,t}}}{\varphi_{\text{Numerical,i,r,t}}} - 1\right) \cdot 100$$
 (5-39)



Figure 5-2: Comparison of analytical solution of Crank [7] and numerical results.



Figure 5-3: Deviation between the numerical and analytical results at r<sub>min</sub> and r<sub>max</sub>.

Figure 5-2 clearly shows that the numerical solution and the analytical algorithm provide nearly the same results. To verify this observation, the deviation between the two algorithms was compared at the inner  $r_{min}$  and the outer radius  $r_{max}$ . In Figure 5-3 the deviation between the analytic and numerical results is shown in percent over time. The occurring deviation of +/- 1 % was assumed to be negligible for the engineering objectives of this work.

# 5.5. Particle Shrinking

For the first calculations, the shrinking of the particles during the hardening process was not taken into account. This assumption is reasonable if the extraction on the surface of the micro-particle is so fast, e.g. under a few seconds, that a hull is formed immediately and, consequently, the diameter of the particles do not significantly change over time. This hull would be then considered the limiting step for the mass transfer.

To prove this assumption a series of experiments were conducted. During the extraction process samples were taken and the micro particle diameter was determined. The two particle size analysis systems used are from Sympatec, namely HELOS, a well proven laser diffraction system, and QICPIC, an image analysis system. In the experimental section of this work a short overview of these two measurement systems is presented.

### 5.5.1. Experimental Results

Figure 5-4 shows experimental results of the micro-particle diameter over time. At the beginning of the experiment (t=0) the diameter of the micro-particle was measured to be equal to 163,49  $\mu$ m. During the extraction process the diameter of the particle decreased to around 100  $\mu$ m because the two solvents diffused in the continuous phase. As a consequence of these occurrences, the assumption that the micro-particle size will not change significantly over time has been disproved. Thus, the description of the shrinking process appeared necessary to obtain correct results.


Figure 5-4: Experimental results for the diameter of the micro-particle over time during the extraction process (Revolutions 260 rpm).

#### 5.5.2. Shrinking Model

As presented above, the shrinking of the particle cannot be considered to be negligible. Therefore, a method to numerically compute the diameter reduction of the micro-particles was developed, which is described in the following sections. The different MATLAB code parts can be found in the appendix.

Basically, the following procedure was used:

1. The differential equation presented in chapter 5.1, for convenience written here again as Eqn. (5-40), was solved for a defined time interval assuming that the shrinking was insignificant during the considered time step.

$$\frac{\partial \varphi_{\text{DP,EA}}}{\partial t} = \frac{1}{r^2} \cdot \frac{\partial}{\partial r} \cdot \left( r^2 \cdot D_{\text{DP,EA}} \cdot \frac{\partial \varphi_{\text{DP,EA}}}{\partial r} \right)$$
(5-40)

The solution of the equation is a three dimensional array which determines the volume fraction  $\varphi_i$  of the two solvents at any given radial position  $x_n$  respectively  $r_n$  and at any time t. As mentioned in section 5.3, the strictly monotonic increasing row vector  $x_{mesh}$  defines the x values  $x_n$  at which the numerical solution is

computed, while the strictly monotonic increasing row vector  $t_{span}$  specifies the time points t where the solution has to be returned.

2. For calculation purposes, the micro-particle was discretized into n different spherical shells. The number of spherical shells is determined by the number of radial sections  $n_{Radial}$ , which also determines the number of elements of the row vector  $x_{mesh}$ . This value has an enormous influence on the accuracy of the results and has been investigated in Chapter 6.

The volume fraction of every spherical shell was determined with the mean volume fractions  $\varphi_{i,m,n,t}$  of the two adjacent radial positions  $x_{n,t}$  and  $x_{n+1,t}$ . The equation to calculate the mean volume fraction of a spherical shell at time t is defined as:

$$\varphi_{i,m,n,t} = \frac{\left(\varphi_{i,n,t} + \varphi_{i,n+1,t}\right)}{2}$$
(5-41)

Here,  $\phi_{i,n,t}$  and  $\phi_{i,n+1,t}$  are the volume fractions of a component i, determined by the solution matrix of the differential equation at two specific radial positions  $x_{n,t}$  respectively  $r_n$  and  $x_{n+1,t}$  respectively  $r_{n+1,t}$ , as well as a certain time t.

In Figure 5-5 a scheme of a spherical shell at the time t is shown. The continuous line represents one boundary of the exemplary discussed spherical shell with the volume fractions  $\varphi_{i,n+1,t}$  at  $x_{n+1,t}$  and the radius  $r_{n+1,t}$ . The dashed line represent the other boundary surface with the volume fractions  $\varphi_{i,n,t}$  at  $x_{n,t}$  and the radius  $r_{n,t}$ .  $\varphi_{i,m,n,t}$  is the mean volume fraction of the considered spherical shell n+1 obtained from Eqn. (5-41).



Figure 5-5: Scheme of a singular spherical shell where the shrinking process is calculated.

In order to determine the mass loss  $m_i$  of a singular particle in a time interval t, the mean volume fractions  $\phi_{i,m,t}$  of the solvents is first transformed into the mass fraction  $w_{i,m,t}$  by using Eqn. (5-42) to Eqn. (5-46).

$$\varphi_{i,m,t} = \frac{V_{i,m,t}}{\sum_{1}^{i} V_{i,m,t}}$$
(5-42)

$$m_{i,m,t} = \rho_i \cdot V_{i,m,t} \tag{5-43}$$

$$w_{i,m,t} = \frac{m_{i,m,t}}{\sum_{1}^{i} m_{i,m,t}}$$
(5-44)

$$w_{i,m,t} = \frac{\rho_{i} \cdot \varphi_{i,m,t} \cdot \sum_{1}^{i} V_{i,m,t}}{\sum_{1}^{i} m_{i,m,t}}$$
(5-45)

$$\frac{\sum_{i}^{i} V_{i,m,t}}{\sum_{1}^{i} m_{i,m,t}} = \frac{1}{\rho_{\text{shell},m,t}}$$
$$w_{i} = \frac{\rho_{i} \cdot \varphi_{i}}{\rho_{\text{shell},m,t}}$$
(5-46)

Here,  $\rho_i$  is the density of the component i and  $\rho_{Shell,m,t}$  is the density of a spherical shell,  $V_{i,m,t}$  is the volume and  $m_{i,m,t}$  is the mass of a spherical shell at the time t.

3. Basically, the density of every spherical shell  $\rho_{Shell,m,t}$  is not constant and is a function of the volume fractions of the different components. The value of the density thus changes with the extraction of the solvents and is a time-dependent value.

$$\rho_{\text{Shell,m,t}} = \varphi_{\text{EA,m,t}} \cdot \rho_{\text{EA}} + \varphi_{\text{BA,m,t}} \cdot \rho_{\text{BA}} + \varphi_{\text{PVA,m,t}} \cdot \rho_{\text{PVA}} + \varphi_{\text{PLGA,m,t}} \cdot \rho_{\text{PLGA}} + \varphi_{\text{API,m,t}} \cdot \rho_{\text{API}}$$
(5-47)

The volume of every spherical shell  $V_{Shell,m,t=0}$  can be determined by just subtracting the volumes of two neighboring spheres  $V_{Sphere,r_{n+1},t=0}$  and  $V_{Sphere,r_n,t=0}$  at the time (t=0).

$$V_{\text{Shell},m,t=0} = V_{\text{Sphere},r_{n+1},t=0} - V_{\text{Sphere},r_n,t=0}$$
(5-48)

$$V_{\text{Shell},m,t=0} = \frac{4}{3} \cdot \pi \cdot \left( r_{n+1,t=0}^3 - r_{n,t=0}^3 \right)$$
(5-49)

The mass of the spherical shell  $m_{Shell,m,t=0}$  can be then determined by multiplying the volume of the spherical shell  $V_{Shell,m,t=0}$  with its current density  $\rho_{Shell,m,t=0}$ .

$$m_{\text{Shell},m,t=0} = V_{\text{Shell},m,t=0} \cdot \rho_{\text{Shell},m,t=0}$$
(5-50)

4. The presented steps enable the calculation of the mass difference  $\Delta m_{Shell,m,t}$  from one time step to another.

$$\Delta m_{\text{Shell},m,t} = m_{\text{Shell},m,t=0} \cdot \left( w_{i,m,t=0} - w_{i,m,t} \right)$$
(5-51)

Consequently, the new mass m<sub>Shell,m,t</sub> of every spherical shell can be updated as:

$$m_{\text{Shell,m,t}} = m_{\text{Shell,m,t}=0} - \Delta m_{\text{Shell,m,t}}$$
(5-52)

The volume of each shell  $V_{Shell,m,t}$  is then obtained by dividing its mass for its current density.

$$V_{\text{Shell,m,t}} = \frac{m_{\text{Shell,m,t}}}{\rho_{\text{Shell,m,t}}}$$
(5-53)

Afterwards, the volume of the new micro-particle  $V_{Sphere,t}$  can be obtained from Eqn. (5-54) and the whole volume difference  $\Delta V_{Sphere}$  from one time step to another is calculated from Eqn. (5-55).

$$V_{\text{Sphere,t}} = \sum_{m=1}^{i} V_{\text{Shell,m,t}}$$
(5-54)

$$\Delta V_{\text{Sphere}} = V_{\text{Sphere},t=0} - V_{\text{Sphere},t}$$
(5-55)

5. The new radius of the micro-particle  $r_t$  at the time t can now be determined by solving the Eqn. (5-56) to Eqn. (5-58).

$$\Delta V_{\text{Sphere}} = V_{\text{Sphere},t=0} - V_{\text{Sphere},t}$$
(5-56)

$$\Delta V_{\text{Sphere}} = \frac{4}{3} \cdot \pi \cdot r_{t=0}^3 - \frac{4}{3} \cdot \pi \cdot r_t^3$$
(5-57)

$$r_{t} = \sqrt[3]{r_{t=0}^{3} - \sum_{n=1}^{n} \frac{3}{4 \cdot \pi} \cdot \Delta V_{\text{Sphere}}}$$
(5-58)

Here,  $r_{t=0}$  is the radius of the micro-particle at the time (t=0).

6. Finally, the numerical grid is rearranged to the updated radius. This algorithm is solved after each time step of the PDEPE solver from MATLAB. The method seemed not to relevantly affect the computational costs of the simulation.

# 6. Parameter Studies

In this section the effects of different parameters on the extraction/shrinking process are presented in detail. Precisely, the influence of variables like the time step size ( $\Delta t$ ), the length of a radial section ( $\Delta x$ ) or the system dependent constant ( $r_{2i}$  and  $r_{3i}$ ), in the correlation of the diffusion coefficient are presented and discussed in terms of final micro-particle diameter and distribution of the polymer inside the micro-particle.

Concerning the structure of this chapter, the studied parameters are first defined. Afterwards, the influence of the length of a radial section ( $\Delta x$ ) and the time step size ( $\Delta t$ ) on the results are determined. Then a sensitivity analysis of the correlation of the diffusion coefficient is presented. Finally, a experimental validation of the numerical results was conducted.

#### **6.1. Material Properties**

The most important material properties of the four different components used in the process are summarized in the following tables. The volume fraction of the different components  $\phi_i$  can be calculated from Eqn. (6-59)

$$\varphi_{i} = \frac{V_{i}}{V_{\text{Total}}}$$
(6-59)

where  $V_i$  is the volume of one component and  $V_{Total}$  is the total volume of the system which is defined as follows:

$$V_{\text{Total}} = \sum_{i=1}^{m} V_i \tag{6-60}$$

The volume fractions at the beginning of the process (t=0) are shown in Table 6-1.

Table 6-1: Volume fractions of the different components at the beginning of the extraction
process.

<b>Φ</b> EA, t=0	<b>ФВА, t=0</b>	<b>Φ</b> Polymer, t=0	ФАРІ, t=0
[m <sup>3</sup> EA/m <sup>3</sup> DP]	[m <sup>3</sup> BA/m <sup>3</sup> DP]	[m <sup>3</sup> Polymer/m <sup>3</sup> DP]	[m <sup>3</sup> API/m <sup>3</sup> DP]
0,618	0,2294	0,1114	0,0412

#### Volume fractions of the different components

The mass fraction of the different components  $w_i$  can be calculated from Eqn. (6-61).

$$w_{i} = \frac{\phi_{i} \cdot \rho_{i,}}{\rho_{DP}} \tag{6-61}$$

Here,  $\rho_i$  is the density of one component and  $\rho_{DP}$  is the density of the disperse phase. The mass fractions at the beginning (t=0) are shown in Table 6-2.

# Table 6-2: Mass fractions of the different components at the beginning of the extraction process.Mass fractions of the different components

$W_{EA, t=0}$	$W_{BA, t=0}$	WPolymer, t=0	WAPI, t=0
[kg EA/kg DP]	[kg BA/kg DP]	[kg Polymer/kg DP]	[kg API/kg DP]
0,5695	0,2405	0,1120	0,0780

All the material parameters needed for the simulations refer to Perry's Chemical Engineers' Handbook [26], the VDI Wärmeatlas [34] or the sticker on the chemicals and are summarized in Table 6-3.

**Table 6-3: Material Parameters.** 

			Ethyl acetate	Benzyl alcohol	Water
Molecular weight	Μ	[g/mol]	88,10	108,14	18,02
Melting point	$\mathbf{T}_{\mathbf{m}}$	[°C]	-82,4	-15,3	0,01
<b>Boiling Point</b>	T <sub>B</sub>	[°C]	77,1	204,7	99,97
Density	ρ	[g/cm <sup>3</sup> ]	0,901	1,046	1,00
Dynamic Viscosity	η	[mPa s]			1,518

# The densities and viscosities of disperse and continuous phase are shown in Table 6-4 and were determined experimentally using a shear rheometer (Physica MCR 301) and a digital densitymeter (DMA 38) from the Anton Paar GmbH.

	Density	Dynamic Viscosity
	ρ	η
	[g/cm3]	[mPa s]
<b>Disperse Phase</b>	0.9948	174,01
<b>Continuous Phase</b>	0.9993	1,419

## Table 6-4: Densities and viscosities of the disperse and continuous phase.

# 6.2. Sensitivity Study for the Time Step Size and the Number of Radial Sections

As described beforehand the differential equation was solved for a determined time interval assuming that the shrinking was insignificant during the considered time step. Hence, the influences of the time step size and the length of one radial section on the accuracy of the results were first investigated.

The length of one radial section  $(\Delta x)$  can be calculated from equation (4-4).

$$\Delta \mathbf{x} = \frac{\mathbf{d}_{\mathrm{t}}}{\mathbf{n}_{\mathrm{Radial}}} \tag{6-62}$$

Here,  $d_t$  is the diameter of the micro-particle at the time (t) and  $n_{Radial}$  is the number of radial sections.

The most important simulation parameters for the sensitivity study are shown in Table 6-5.

Diameter	Time	<b>Revolution</b> rate	Diffusion	coefficient
$\mathbf{d}_{t=0}$	t <sub>total</sub>	n	D <sub>EA,t=0</sub>	D <sub>BA,t=0</sub>
[µm]	[s]	[rpm]	[m <sup>2</sup> /s]	[m <sup>2</sup> /s]
163,49	50	260	1,750.10-7	1,692.10-7

Table 6-5: Simulation parameters for the sensitivity study.

The values of the system-dependent constants  $r_1$ ,  $r_2$  and  $r_3$ , which are needed to calculate the concentration-depending diffusion coefficient, are assumed to be equal to the values used by Reuvers et al. [25], (see Table 6-6). A detailed analysis of the influence of these coefficients is presented in section 1.4.

 Table 6-6: System-dependent constants for the calculation of the diffusion coefficient.

 System-dependent constants

r <sub>EA,1</sub>	r <sub>EA,2</sub>	r <sub>EA,3</sub>	r <sub>BA,1</sub>	r <sub>BA,2</sub>	r <sub>BA,3</sub>
1,750	5,75	11.25	1,692	5,75	11,25

The investigated ranges of the various parameters are shown in Table 6-7 and Table 6-8.

	$\Delta t$
_	[sec]
	0,05
	0,1
	0,5
	1

# Table 6-7: Investigated range of time step sizes ( $\Delta t$ ). Time step

# Table 6-8: Investigated range of radial sections lengths ( $\Delta x$ ).Number of Radial sectionsLength of a radial section

<b>n</b> <sub>Radial</sub>	$\Delta \mathbf{x}$
	[µm]
20	8,175
50	3,269
100	1,635
200	0,817
400	0,409





The influence of the number of radial sections ( $n_{Radial}$ ) on the SMD after 50 s of extraction is illustrated in Figure 6-1. With the increase of the number of radial sections the SMD decreases. As also shown in Figure 6-1, the influence of the time step size ( $\Delta t$ ) on the SMD appears insignificant in the investigated range. Notice, that if the number of radial sections is doubled from 200 to 400 the results change by only one percent. The calculation time instead has to be increased by a factor of 5. Thus, the enhancement due to finer grid was considered to be insignificant for the engineering objectives of this work. As a consequence, all further simulations were conducted with 200 radial sections, which correspond to a length of a singular section of 0,817 µm.

In Figure 6-2 the SMD after 50 s of extraction over the different time step sizes ( $\Delta t$ ) is shown. This figure clearly shows that the influence of the time step size on the final micro-particle diameter is insignificant in the investigated range.



Figure 6-2: Dependency of the SMD on the time step size ( $\Delta t$ ).

# 6.3. CFL-Analysis

In this section the combined effect of the time step size and the grid refinement on the accuracy of the results was further investigated.

The CFL-number or Courant-number is used in the numerical flow simulation for the discretization of time dependent partial differential equations. This parameter is named after Richard Courant, Kurt Friedrichs, and Hans Lewy [6]. It arises when explicit time-marching schemes are used for the numerical solution. To avoid incorrect results, the time step must be less than a certain time in many explicit time-marching computer simulations.

In our case we simply use this parameter to connect the sizes of time step and radial sections with a well-known parameter. Nevertheless, it has not to be confused with the stability analysis for the CFD simulations.

The value of the CFL-number (6-63) is written as follows:

$$CFL < \frac{v \cdot \Delta t}{\Delta x}$$
 (6-63)

where v is the velocity at the beginning of the extraction process, which can be obtained from Eqn. (6-64).

$$\mathbf{v} = \frac{\dot{\mathbf{M}}_{t=0}}{\mathbf{A}_{\mathrm{P}} \cdot \boldsymbol{\rho}_{\mathrm{DP}}} \tag{6-64}$$

Here,  $\dot{M}_{t=0}$  is the mass transfer rate at (t=0),  $A_P$  is the surface of the micro-particle and  $\rho_{DP}$  is the density of the disperse phase.

The mass transfer rate at the beginning can be defined as:

$$\dot{M}_{t=0} = \beta_i \cdot A_p \cdot \Delta c \tag{6-65}$$

where  $\beta_i$  is the mass transport coefficient of the different diffusing solvents and  $\Delta c$  is the concentration difference between the continuous and disperse phase.

The concentrations of the different solvents at the interface can be expressed trough their volume fractions  $\phi_i$  and their densities  $\rho_i$  and the concentration in the continuous phase at

the beginning can be assumed to be equal to zero. Finally, the mass transfer rate is calculated by using Eqn. (6-66) to Eqn. (6-67):

$$\dot{M}_{t=0} = \dot{M}_{EA,t=0} + \dot{M}_{BA,t=0}$$

$$\dot{M}_{t=0} = \beta_{EA} \cdot A_{P} \cdot \left(\phi_{EA}^{*} \cdot \rho_{EA} + c_{CP,EA}\right) + \beta_{BA} \cdot A_{P}$$

$$\cdot \left(\phi_{BA}^{*} \cdot \rho_{BA} + c_{CP,BA}\right)$$

$$v = \frac{\beta_{EA} \cdot \left(\phi_{EA}^{*} \cdot \rho_{EA}\right) + \beta_{BA} \cdot \left(\phi_{BA}^{*} \cdot \rho_{BA}\right)}{\rho_{DP}}$$

$$(6-67)$$

Here,  $\phi_i^*$  is the volume fraction of the component i at the interface.

The calculated values for the velocity and the corresponding CFL-numbers are shown in Table 6-9.

CFL-Number	Velocity	Length of a radial section	Time step size
	v	Δx	Δt
	[m/s]	[μm]	[ <b>s</b> ]
3,24			0,0005
6,48	0.0053	$\frac{D}{200} = 0,817$	0,001
647,74	0,0055	200	0,1
6477,45			1

Table 6-9: CFL-numbers for the different calculated cases.

To ensure the comparability of the two analyses, the same simulation parameters and system-dependent constants used in the previous paragraph were used for the CFL-analysis. Hence, the most important simulation parameters are shown in Table 6-5 and the values of the system-dependent constants are presented in Table 6-6.



Figure 6-3: SMD over time for different CFL-numbers.

In Figure 6-3 the time evolution of the Sauter mean diameter (SMD) for different CFLnumbers is shown. According to these results, it appears evident that the decrease of the CFL-number has no significant influence on the results. To verify this observation, the deviation between the different calculated diameters after one second of extraction process was compared. In Figure 6-4 the deviation in percent is shown over the different CFLnumbers. The occurring deviation of about  $\pm$  1,2% was assumed to be negligible for the engineering objectives of this work.



**Figure 6-4: Deviation between the different diameters after one second of the extraction process.** The influence of the CFL-number on the calculation time is illustrated in Figure 6-5. As shown in the figure, the computational effort for the simulation of one second of the extraction process increased from about 40 seconds at a CFL-number of 6477,4 to about 35 minutes at a CFL-number of 3,24.

As a consequence of the presented facts, all further simulations were conducted with a time step size of one second.



Figure 6-5: Calculation period for one second of the extraction process for different CFLnumbers.

In Table 6-10 the most important results of the CFL-analysis are summarized again.

CFL-number	SMD <sub>after 1</sub> second	Calculation period
CFL	d <sub>t=1</sub>	
	[µm]	[min]
3,24	1,5645	33,37
6,48	1,5645	15,73
647,74	1,5661	0,66
6477,45	1,5836	0,07

 Table 6-10: Results of the CFL-analysis.

## 6.4. Sensitivity Analysis for the Diffusion Coefficient

As also mentioned in section 5.2.4, the diffusion coefficient for both solvents is highly depending on the polymer volume fraction in the micro-particle. The correlation from Reuvers et al. [25] in a paper by Li et al. [18] for convenience written here again as Eqn (6-68):

$$D_{i} = r_{1,i} \cdot 10^{-(r_{2,i} + r_{3,i} \cdot \phi_{P})}$$
(6-68)

where  $r_{1,i}$ ,  $r_{2,i}$  and  $r_{3,i}$  are the system-dependent constants and  $\phi_P$  is the volume fraction of the polymer.

The rule of thumb of specifying the  $r_i$  values is to adjust these constant to result in a reasonable diffusion coeffcient [18]. Thus, the influences of these system-dependent constants on the results are investigated in this section.

The two system-dependent constants  $r_{1,i}$  and  $r_{2,i}$  were determined by equating the correlation for the diffusion coefficient from Wilke and Chang [36] with the one from Reuvers et al. [25] at the beginning of the extraction process (t=0). The correlation from Wilke and Chang [36], which is valid for diffusion of various substances in water and in non-associated solvents, is for convenience written here again as Eqn. (6-69).

$$D_{i} = 7.4 \cdot 10^{-8} \cdot \frac{(x \cdot M)^{\frac{1}{2}} \cdot T}{\eta \cdot V^{0,6}}$$
(6-69)

Here, M is the molecular weight of the solvent, T the temperature,  $\eta$  is the viscosity of solution and V is the molar volume of solute at normal boiling point.

The obtained values for system-dependent constants  $r_{1,i}$  and  $r_{2,i}$  for the two solvents are shown in Table 6-11.

System-dependent constants

sensitiv	ity analysis.
Ethyl acetate	Benzyl alcoh
System-dep	endent constants
r <sub>1,EA</sub> r <sub>2,EA</sub>	$\mathbf{r}_{1,\mathrm{BA}}$ $\mathbf{r}_{2,\mathrm{BA}}$
1,750 7,0	1,692 7,

 Table 6-11: System-dependent constants for the correlation of diffusion coefficient for the sensitivity analysis.

For a first anlysis, the value of  $r_{3,EA}$  for ethyl acetate was set to be equal to the value of  $r_{3,BA}$  for benzyl alcohol. The corresponding diffusion coefficients of the two solvents at the beginning ( $\phi_{P,t=0}$ ) and at a theoretical maximal concentration of polymer ( $\phi_{P}=1$ ) are shown in Table 6-12.

 Table 6-12: System-dependent constants and corresponding diffusion coefficients for the two solvents.

**Diffusion coefficients** 

r <sub>3,EA</sub>	<b>r</b> <sub>3,BA</sub>	$D_{EA,\phi_{P,t=o}}$ $[m^2/s]$	$D_{EA,\phi_{P}=1}$ $[m^2/s]$	$\mathbf{D}_{\mathrm{BA},\phi_{\mathrm{P},t=o}}$ $[\mathbf{m}^2/\mathbf{s}]$	$D_{BA,\phi_{P}=1}$ $[m^2/s]$
0		$1,75 \cdot 10^{-7}$	$1,75 \cdot 10^{-7}$	$1,69 \cdot 10^{-7}$	$1,69 \cdot 10^{-7}$
2		$1,05 \cdot 10^{-7}$	$1,75 \cdot 10^{-9}$	$1,01 \cdot 10^{-7}$	1,69 · 10 <sup>-9</sup>
4	ļ	$6,27 \cdot 10^{-8}$	$1,75 \cdot 10^{-11}$	6,06 · 10 <sup>-8</sup>	$1,69 \cdot 10^{-11}$
6	, )	$3,76 \cdot 10^{-8}$	$1,75 \cdot 10^{-13}$	3,63 · 10 <sup>-8</sup>	$1,69 \cdot 10^{-13}$
8	}	$2,25 \cdot 10^{-8}$	$1,75 \cdot 10^{-15}$	$2,17 \cdot 10^{-8}$	1,69 · 10 <sup>-15</sup>
1	0	$1,35 \cdot 10^{-8}$	$1,75 \cdot 10^{-17}$	$1,30 \cdot 10^{-8}$	$1,69 \cdot 10^{-17}$
1	2	$8,06 \cdot 10^{-9}$	$1,75 \cdot 10^{-19}$	$7,79 \cdot 10^{-9}$	$1,69 \cdot 10^{-19}$

The most important simulation parameters for the sensitivity analyses are shown in Table 6-13. These data come again from experimental analysis of the process and are the so called standard parameters.

Table 6-13: Simulation parameters for the sensitivity analysis.				
Diameter	Time	<b>Revolution rate</b>	Time step	Length of a radial section
$\mathbf{d}_{t=0}$	t <sub>total</sub>	n	Δt	Δx
[µm]	[s]	[rpm]	[sec]	[µm]
163,49	10	260	1	0,817

In Figure 6-6 the influences of the values of the system-dependent constants  $r_{3,EA}$  and  $r_{3,BA}$  on the SMD are shown. It appears evident that the values of these constants have an enourmous influence on the final diameter of the micro-particle. In fact, if the constants  $r_{3,EA}$  and  $r_{3,BA}$  are for example set to be equal to zero, represented by the black colored line, the diffusion coefficients remain constant to a very high value. As a consequence of that the solvents diffuse immediatly in the continuous phase and the diameter of the micro-particle decreases fastly to its final value.

On the other hand, if the constants  $r_{3,EA}$  and  $r_{3,BA}$  are set to be equal to twelve, represented by the magenta colored line, the diffusion coefficients change with the variation of the polymer volume fraction inside the micro-particle. As a consequence of that, the diameter of the micro-particle does not decrease so quickly and the extraction is limited by the mass transport rate to the interface inside the micro-particle.



Figure 6-6: Particle SMD over time for different values of r<sub>3</sub>.

In Figure 6-7 the volume fraction of the remaining components (API, Polymer) after a extraction time of ten seconds is shown over the normalized radius. As mentioned above, the solvents diffuse immediatley when the constants  $r_{3,EA}$  and  $r_{3,BA}$  are set to be equal to zero. This is also evident by the black colored line in Figure 6-7, where the volume fraction of the remaining components increases immediatley and converges to one.

A complete different behaviour is observed when the constants  $r_{3,EA}$  and  $r_{3,BA}$  are set to be equal to twelve. In this case the diffusion coefficient decreases to a very low value with the increase of the volume fraction of polymer. Hence the hardening process respectivley the extraction of the solvents is limited by the mass transport, inside the micro-particle to the interface. As shown in the figure and represented by the magenta colored line, the volume fraction inside the micro-particles remain almost constant after 10 seconds of extraction. Only at the surface the two solvents are extracted immediatley and the diffusion coefficients decrease to a small values.

This can suggest the formation of a shell and indicates that the first seconds of the extraction process determine the final characteristics of the micro-particle. This assumption is reasonable because this behavior was also observed experimentally. It was supposed that the first seconds that means the first contact from the emulsion droplets with the continuous phase have a great influence on the final characteristics of the micro-particles.

However, further experimentally analysis is required to prove these assumptions.



Figure 6-7: Volume fraction of the remaining components  $\phi_{RP}$  over the normalized radius for different values of  $r_3$  after a extraction time of 10 s.

# 6.5. Experimental Validation

In the previous sections a numerical model has been presented, which is able to simulate the diffusion process of two solvents during the hardening/extraction step, as well as the consequent shrinking of the particles in a stirred reactor. Now, the validation of the method is performed by comparing the numerical results with the data obtained by different experiments performed in laboratory scale.

The prediction of the final micro-particle size was considered to be one of the most important quality attribute. Therefore, the Sauter mean diameters of the micro-particles were determined at different instants of time by two different particle size analyzers, namely HELOS and QICPIC from the Sympatec GmbH. A detailed description of the experimental work and of these two measurement systems can be found in Chapter 6. The experimental set up is shown and described in Chapter 3.

For comparability purposes, the main request was that all the important parameters in the simulation, namely revolution rate of the stirrer, diameter of the micro-particle at the beginning (t=0), as well as material properties, had to be the same as the one used in the experiment. In Table 6-14 the most important simulation parameters for the experimental validation are shown.

	Table 6-14: Simulation parameters for the experimental validation.			
Diameter	Time	<b>Revolution rate</b>	Time step	Length of radial sections
$\mathbf{d}_{t=0}$	t <sub>total</sub>	n	Δt	Δx
[µm]	[ <b>s</b> ]	[rpm]	[sec]	[µm]
163,49	50	260	1	0,817

mulation noromators for the o Table 6 14. 6%

As discussed in section 5.2.4, the rule of thumb is to fit the system-dependent constants ( $r_{1,i}$  $r_{2,i}$  and  $r_{3,i}$ ) to the experimental data. These values were determined on the one hand by equating the correlation for the diffusion coefficient from Wilke and Chang [36] with the one from Reuver et al. [25] and on the other hand by setting reasonable final values for the diffusion coefficient in the hardened micro-particle. These values and their corresponding diffusion coefficients at the beginning ( $\varphi_{P,t=0}$ ) and at a theoretical maximal concentration of polymer ( $\phi_P=1$ ) are shown in Table 6-15 and Table 6-16.

System-dependent constants			Diffusion of	<b>Diffusion coefficients</b>		
r <sub>1,EA</sub>	r <sub>2,EA</sub>	r <sub>3,EA</sub>	$D_{EA,\phi_P,t=o}$	$D_{EA,\phi_{P=1}}$		
			[m <sup>2</sup> /s]	[m <sup>2</sup> /s]		
1,75	6,25	6,75	$1,75 \cdot 10^{-7}$	$1.75 \cdot 10^{-13}$		
1,75	6,00	9,00	$1,75 \cdot 10^{-7}$	$1,75 \cdot 10^{-15}$		
1,75	5,75	11,25	$1,75 \cdot 10^{-7}$	$1,75 \cdot 10^{-17}$		

 Table 6-15: System-dependent constants and corresponding diffusion coefficients for ethyl acetate.

 Table 6-16: System-dependent constants and corresponding diffusion coefficients for the benzyl alcohol.

Syster	n-dependent con	stants	Diffusion of	coefficients
r <sub>1,BA</sub>	r <sub>2,BA</sub>	r <sub>3,BA</sub>	$D_{BA,\phi P,t=0}$	$D_{BA,\phi P^{=1}}$
			[m <sup>2</sup> /s]	$[m^2/s]$
1,70	6,25	6,75	$1,69 \cdot 10^{-7}$	$1,70 \cdot 10^{-13}$
1,70	6,00	9,00	$1,69 \cdot 10^{-7}$	$1,70 \cdot 10^{-15}$
1,70	5,75	11,25	$1,69 \cdot 10^{-7}$	$1,70 \cdot 10^{-17}$

The comparison between the numeric and experimental results are illustrated for different extraction times in Figure 6-8 (1 hour of extraction), Figure 6-10 (5 hours of extraction) and Figure 6-9 (20 hours of extraction). In these figures the Sauter mean diameter (SMD) is shown over the time. The colored markers represent the experimental data and the different colored lines the numeric results.



Figure 6-8: Comparison between the numerical and experimental data over an extraction time of 1 hour.



Figure 6-9: Comparison between the numerical and experimental data over an extraction time of 5 hours.



Figure 6-10: Comparison between the numerical and experimental data over an extraction time of 20 hours.

As shown in the three figures it is evident that the best match between numerical and experimental data is achieved when the system-dependent constants  $r_{3,EA}$  and  $r_{3,BA}$  of the two solvents are set to be equal to nine and the  $r_{2,EA}$  and  $r_{2,BA}$  are set to be equal to six. Thus, we used these values for further analysis of the hardening/extraction step for the material system we considered.

The influences of the system-dependent constants ( $r_{2,EA}$ ,  $r_{2,BA}$ ,  $r_{3,EA}$  and  $r_{3,BA}$ ) on the distribution of the volume fractions of the two solvents (ethyl acetate and benzyl alcohol) and the remaining components (API, Polymer) are shown in Figure 6-11, Figure 6-12 and Figure 6-13. The volume fractions are shown for four different instants of time:

- The black colored lines represent the distribution of the different volume fractions at the beginning (t = 0 hour).
- The blue colored lines show the distribution of the different volume fractions after one hour of extraction.
- The red colored lines show the distribution of the different volume fractions after five hours of extraction.

- The magenta colored lines show the distribution of the different volume fractions after twenty hours of extraction.

These three figures clearly show the same behavior as observed by the sensitivity analyses presented in subsection 5.4. For readability reason only the system-dependent constant  $r_{3,i}$  is shown in the legend of these figures. The corresponding values of  $r_{2,i}$  can be found in Table 6-15 and Table 6-16.

With the increase of the value of the system-dependent constants, the mass transport inside the micro-particle to the interface becomes more and more the limiting step. Hence, the solvents cannot diffuse that quickly and remain inside. In this case the volume fraction is represented by the line with the upward-pointing triangle. In short the volume fractions of the solvents only converge at the interface against zero.

A complete different behavior is observed for the other two cases. Here the solvents diffuse very quickly out of the micro-particle in the continuous phase. As a consequence of that the residual solvent content is very low after 20 hours of extraction.



Figure 6-11: Volume fraction of ethyl acetate over the normalized radius for different values of r<sub>3</sub> at different instants of time.



Figure 6-12: Volume fraction of benzyl alcohol over the normalized radius for different values of r<sub>3</sub> at different instants of time.



Figure 6-13: Volume fraction of remaining components over the normalized radius for different values of r<sub>3</sub> at different instants of time.

In Figure 6-14, Figure 6-15 and Figure 6-16 the diffusion coefficients of the two solvents with respect to the normalized radius for different values of  $r_3$  at different instants of time are shown. The diffusion coefficients of the solvents change with the change of the volume fraction of polymer. Precisely:

- In Figure 6-14  $r_{2,EA}$  and  $r_{2,BA}$  are set to be equal to 6,25 and  $r_{3,EA}$  and  $r_{3,BA}$  are set to be equal to 6,75.
- In Figure 6-16 r<sub>2,EA</sub> and r<sub>2,BA</sub> are set to be equal to 6,00 and r<sub>3,EA</sub> and r<sub>3,BA</sub> are set to be equal to 9,00.
- In Figure 6-15 r<sub>2,EA</sub> and r<sub>2,BA</sub> are set to be equal to 5,75 and r<sub>3,EA</sub> and r<sub>3,BA</sub> are set to be equal to 11,25.

As shown in the figures the trend of the diffusion coefficients of the two solvents are equal. This is reasonable considering that the system-dependent constants of these two solvents were set to the same values. To validate this behavior further experimental analysis is required.



Figure 6-14: Diffusion coefficients of the two solvents over the normalized radius for different extraction times.



Figure 6-16: Diffusion coefficients of the two solvents over the normalized radius for different extraction times.



extraction times.

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Finally a surface plot for the volume fraction of each component as a function of time and radius are shown in Figure 6-17, Figure 6-18 and Figure 6-19. These diagrams relate to the best match between numerical and experimental data, namely with  $r_{3,EA}$  and  $r_{3,BA}$  of the two solvents equal to 9, as well as  $r_{2,EA}$  and  $r_{2,BA}$  equal to 6.



Figure 6-17: Volume fraction of ethyl acetate as a function of the time and radius.



Figure 6-18: Volume fraction of benzyl alcohol as a function of the time and radius.



Figure 6-19: Volume fraction of the remaining components (API, Polymer) as a function of the time and radius.

It is evident that the volume fraction of the ethyl acetate and benzyl alcohol decrease fast, at the beginning, until the outer shells are almost completely free from solvent. The low diffusion coefficient inside the polymer leads then to a slow mass transport from the middle to the outer part of the micro-particle, thus to a slower extraction.

#### 6.6. Diameter Variation Analysis

As described in Chapter 3 the emulsion was produced by a static mixer unit and was then led into the extraction reactor. It was determined that the emulsion drop size distribution depended on different parameters like volume flow and number of SMX static mixer elements. Consequently, the developed model had to be able to deal with different initial values for the emulsion drop size.

The investigated range of the initial diameter (t=0) variations are shown in Table 6-17. The same simulation parameters described in the previous sections, were used. Furthermore, the investigation was performed with the empirical parameters  $r_i$  that provide the best agreement between experimental and numerical data. Hence, the most important simulation parameters are shown in Table 6-14 and the system values of the system dependent constants are presented in Table 6-15 and Table 6-16.

	$\mathbf{d}_{t=0}$	
	[µm]	
1	50	
2	100	
3	163,49	
4	200	

# Table 6-17: Investigated range of initial diameters.CaseDiameter at the beginning

The SMD over the extraction time for the different initial diameters are illustrated in Figure 6-20. It is apparent that the shrinkage depends on the initial size of the emulsion drops. To verify this observation, the ratio between the current diameter and the initial one was calculated as well. This percentage of shrinkage is shown over the extraction time in Figure 6-21.

This behavior could be easily explained as by decreasing micro-particle diameter the surface to volume ratio increases, leading to a stronger mass transfer from the surface to the extraction medium and, consequently, to an increase in the percentage of shrinkage. This ratio can be calculated by using Eqn. (6-70) to Eqn. (6-72).

$$V_{\rm P} = \frac{d_{\rm P}^3 \cdot \pi}{6} \tag{6-70}$$

$$A_{\rm P} = d_{\rm P}^2 \cdot \pi \tag{6-71}$$

$$\frac{A_{\rm P}}{V_{\rm P}} = \frac{6}{d_{\rm p}} \tag{6-72}$$

Here  $V_p$  is the volume,  $d_p$  is the diameter and  $A_p$  is the surface of the micro-particle.



Figure 6-20: SMD over time for different initial diameters.



Figure 6-21: Ratio of difference between the current and the initial diameter.



Figure 6-22: Shrinkage over the different initial diameters.

In Figure 6-22 the Shrinkage in percent over the initial diameter is illustrated. In the investigated range of the micro-particle size from 50 to 200  $\mu$ m and with a revolution rate
of the stirrer of 260 rpm, the shrinkage ratio is almost linearly correlated to the initial diameter as the  $2^{nd}$  and  $3^{rd}$  exponent of the series are very low.

In Table 6-18 the most important results of the diameter variation analysis are summarized again.

Case	Diameter at the beginning	Diameter after 1 hour	Shrinkage after 1 hour		
	$\mathbf{d}_{t=0}$	$\mathbf{d}_{t=1\mathbf{h}}$			
	[µm]	[µm]	[%]		
1	50	29,61	40,78		
2	100	62,49	37,51		
3	163,49	106,75	34,71		
4	200	132,95	33,53		

#### Table 6-18: Results of the diameter variation analysis.

### **6.7.** Overview over the Experiments

The presented mass transfer model takes only the mean value for the relative velocity between particles and flow into account. To determine the influence of other parameters, like the local flow field, on the final micro-particle size, different experiments were conducted. For this purpose the revolution rate n and the position of the inlet point were varied. According to this, in Figure 6-23 a sketch of the reactor unit is shown where the position-determining variables  $h_e$  and  $x_e$  are defined. The engineering drawing of the reactor and stirrer unit can be found in the appendix. The different variations are summarized in Table 6-19.

 Table 6-19: Revolution rate n and distance between the inlet position and stirrer blade for the different experimental cases.

Cases	<b>Revolution rate</b>	Distance between inlet position and stirrer blade						
n		h <sub>e</sub>						
	[rpm]	[mm]						
1	100	30						
2	260	100						
3	260	30						



Figure 6-23: Sketch of the extraction reactor to define the inlet position.

# 6.8. Experimental Results

In Figure 6-24 the Sauter mean diameter (SMD) is shown over the extraction time for the three investigated cases.



Figure 6-24: Experimental results for the diameter of the micro-particle over time during extraction process for the three variations.

As shown in the figure the revolution rate and the position of the inlet point have an influence on the final micro-particle size.

In case 1 where the revolution rate was set to 100 rpm and the distance between the inlet point and the stirrer blade was about 30 mm, represented by the blue line, the micro-particle diameter after twenty hours of extraction reduced from 163,49  $\mu$ m to about 130  $\mu$ m. This low revolution rate led to a lower local Reynolds number (see Equation (5.22)) respectively to a lower local velocity at the inlet point.

A complete different behaviour was observed when the revolution rate was set to 260 rpm and the distance between the inlet point and the stirrer blade was about 30 mm. In this so called standard case, represented by the red line, the local Reynolds number and the local velocity at the inlet point were much higher than in case 1. The micro-particle shrunk much more during the 20 hours of extraction to a final diameter of about 107  $\mu$ m.

As a consequence of these facts it was assumed that the final micro-particle diameter can be related to the value of the local Reynolds number and the local velocity at the inlet point.

To determine the influence of the position of the inlet point the revolution rate was set to 260 rpm and only the distance between the inlet point and the stirrer blade was increased to about 100 mm. This larger pitch had the effect that the emulsion was inserted in an area with lower local velocity. After 20 hours of extraction the micro-particle diameter was around 130  $\mu$ m. On the whole the observed trend was very similar to the case 1 where the revolution rate was much lower.

This additional insight suggests that the prevailing flow regime respectively the local velocity at the point of inlet is of extraordinary significance for the entire process.

The volume-based size and density distributions of the three cases after 20 hours of extraction are shown in Figure 6-25, Figure 6-26 and Figure 6-27.

In the cases where the emulsion was inserted in an area of low local velocity, case 1 and 2, the median value  $x_{50}$  was around 200  $\mu$ m. Furthermore the density distribution was a little bit narrower than in case 3, where the local velocity at the point of inlet was much higher.

To sum up, the following considerations can be derived from experimental results:

- The position of the inlet point is very important because the prevailing flow regimes at this point have a great influence on the size distribution of the microparticles.
- If the emulsion is inserted in an area of low local velocity the resulting microparticles are larger than the one produced at higher stirrer speed.
- The emulsions size distribution appears tighter for emulsions injected in regions of lower local Reynolds numbers.

Further research is nevertheless required to ensure the observations.



Figure 6-25: Experimental results for case 1 after 20 hours of extraction (n = 100 [rpm] and  $h_e = 30$ [mm]).

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Figure 6-26: Experimental results for case 2 after 20 hours of extraction (n = 260 [rpm] and  $h_e = 100$ [mm]).

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Figure 6-27: Experimental results for case 3 after 20 hours of extraction (n = 260 [rpm] and  $h_e = 30$ [mm]).

# 7. Conclusions and Outlook

### 7.1. Conclusions

The objective of this work was to investigate the extraction step of a micro-particle process on the basis of solvent extraction method to predict different characteristics and to determine the most important process parameters. The final quality of the considered micro-particles can be controlled only by a deep understanding of each step of the production process. Therefore on the one hand a numerical model was developed and on the other hand different experimental investigations were performed.

The developed numerical model is capable to describe the mass transfer from the disperse phase into the continuous phase respectively the hardening/extraction process. First a mass transport model based on the work of Li et al. [18] was established using mass diffusion theory and thermodynamic principles. Therefore the different phenomena and variables, like the mass transport coefficient and the concentration dependent diffusion coefficient, were described and modeled mathematically. Also the comparison of the obtained numerical results by this model with an analytical solution, found by John Crank [7] showed a good agreement. Furthermore a custom build shrinking model respectively a method to numerically compute the diameter reduction of the micro-particles was implemented. Unfortunately, assumptions had to be made in order to perform the simulation due the fact that different data on chemical media are not exactly known and occurring phenomena are not fully researched.

However predictions of our numerical model fit the experimental data reasonably well. Therefore the experimental obtained results of the micro-particle size were compared with the numerical ones. Besides that to determine the discretization uncertainty the influence of the time step size and the grid size on the accuracy of the results were also investigated. In order to find realistic ranges for the values of the unknown variables a parameter study was performed. The results of the sensitivity analyses indentified the correlation of the concentration depending diffusion coefficient respectably the system-dependent constants as the most influential parameters. Consequently these parameters are well suited to adjust the results of the simulation.

The numerical model clearly showed that the mass transport inside the micro-particle is the determining step in the extraction process. It is much slower than the mass transport from the interface to the continuous phase. As a result the limiting step of the extraction process is given by the diffusion in the polymer.

Concerning the experimental investigations first of all an experimental set up was build up in the laboratories of the Research Center Pharmaceutical Engineering (RCPE GmbH) in Graz. The performed investigations were able to quantify the micro-particle size during the extraction process. Therefore two particle size analysis systems from Sympatec GmbH., namely HELOS and QICPIC were used. Also the influences of different parameters, like the revolution rate of the stirrer and the position of the inlet point, on the final microparticle size distribution were investigated.

These investigations suggested that the first seconds of the process have the greatest influence on the final "quality" of the micro-particles. It was assumed that the prevailing flow regimes, at the beginning this means at the first contact of disperse and continuous phase in the extraction tank determine the final properties of the micro-particles.

On the whole I have to mention that most of the goals set in this work were reached. The developed numerical model is a first approach to get a better understanding of the extraction stage. It also helps to determine the most important process parameters and which influence they have on the final micro-particle quality.

To sum up the gained knowledge provides a very useful guideline for the process technology development. This helps on the one hand to reduce the tedious trial and error experiments and on the other hand to cut development costs.

Finally I have to mention that a better process understanding is the key to superior and more cost efficient pharmaceuticals.

# 7.2. Future Work

Further investigations, both experimental and numerical, of the observed processes are of utmost importance. For example, numerical CFD (Computational Fluid Dynamics) simulations of the flow field inside the reactor may be useful to understand the local effects on the hardening process. These computations can provide information about the prevailing flow regimes in the reactor and can lead to a better insight here. In addition to this, the developed numerical MATLAB model should be linked with the CFD simulations. The gained information should then be approved experimentally.

Moreover, microscopy measurements of the micro-particle during the extraction process could provide a deeper understanding on the structure of the hardening polymer.

Another future task is the further improvement and testing of the numerical model. Here, the different unknown parameters have to be determined whether by experimental investigations or by further literature research. These new information should then be implemented in the existing model. Besides all that, a variation the revolution rate of the stirrer should be investigated.

Further experimental validations of the numerical results should be also carried out to verify the model in terms of mass transfer. To achieve this, the volume fraction of the solvents in the continuous phase during the extraction process should be determined. The entire required chemical analysis (GC method) was already established and tested during this work.

Another future task can be the evaluation of different measurement systems for the inline/online/real-time monitoring of the process. The potential of these techniques should be assessed in terms of accuracy and measuring speed. A previous analysis of measurement systems, performed during this work, showed that spectroscopic systems (e.g. Raman-, Near-infrared- and Mid-infrared-Spectroscopy) fulfill most of the requirements and are therefore the best possibilities to measure the volume fractions of the solvents (ethyl acetate and benzyl alcohol) in the continuous phase.

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# I. Code (MATLAB R2009b)

#### Calc.m

```
% Numerical Model
% (c) by Hannes Pucher
8-----
8-----
% Clear, Close and delete all
clc
clear all
close all
§_____
8-----
% Stopwatch start
tStart=tic
8-----
§_____
% Load the different parameter files
cd
DiffusionCoefficient
Parameters
§_____
§_____
% Define the memory variables
memRadius end = [];
memTime = [];
memVolumefraction EA = [];
memVolumefraction BA = [];
memRadius = [];
memMass = [];
memAmbient EA = [];
memAmbient BA = [];
membetafl EA = [];
membetafl BA = [];
memDiffusion = [];
             _____
8_____
8-----
\% Solve the differential equation for every delta t as long as t total <
% t total max
while t_total < t_total_max</pre>
   % Call the PDEPE solver
   sol
   pdepe(m,@calcpde,@calcic 2,@calcbc,radius,t);
```

```
% Extract the solutions as volume fraction EA/BA/W
volume fraction EA
                        = sol(:,:,1);
volume fraction BA
                         = sol(:,:,2);
volume fraction W
                        = sol(:,:,3);
% Call the numerical model for shrinking
Shrinking
% Extract the different solutions
volume f current EA
                        = volume_fraction_EA(t_span,:); % Extract
the last volumefraction profile of ethylacetate
volume f current BA = volume fraction BA(t span,:); % Extract
the last volumefraction profile of benzylalcohol
delta m EA temp
                         = sum delta m EA;
delta m BA temp
                         = sum delta m BA;
radius
                         = radius new cell; % [m] Define the new
radius of the sphere
radialPositions
                        = radius; % [m] Define the new radial
position of every volumefraction
Surface particle
                        = Surface particle new; % [m^2] Define the
new surface of the sphere
mass ethylacetate q temp = mass ethylacetate q new;
mass benzylalcohol q temp= mass benzylalcohol q new;
                         = t total + delta t % [s] Define the new
t total
time (t total)
memRadius end
                        = [memRadius end radius(r intervall)]; %
[m] Save the actual radius of the sphere
memTime
                        = [memTime t_total]; % [s] Save the actual
time
memVolumefraction EA
                       = [memVolumefraction EA
volume_f_current_EA'];
\ensuremath{\$} Save the actual volume fraction vector of ethylacetate
memVolumefraction BA = [memVolumefraction BA
volume f current BA'];
% Save the actual volume fraction vector of benzylalcohol
memRadius
                        = [memRadius radius']; % [m] Save the
actual
radial vector
memMass
                         = [memMass sum mass']; % [kg] Save the
actual
mass of the sphere
                         = [memAmbient EA ambientconc EA']; % Save
memAmbient EA
the
actual ambient volume fraction of ethylacetate
                       = [memAmbient BA ambientconc BA']; % Save
memAmbient BA
the
actual ambient volume fraction of benzylalcohol
                         = [membetafl EA betafl EA]; % [m/s] Save
membetafl EA
the
actual mass transport coefficient of ethylacetate
                         = [membetafl BA betafl BA]; % [m/s] Save
membetafl BA
the
```

actual mass transport coefficient of benzylalcohol end 8-----8-----% Plot file for the radius Plot Radius % Plot file for the diffusion coefficients Plot Diffusion EA Plot Diffusion BA % Plot file for the result for ethylacetate, benzylalcohol and water Plot EA Plot\_BA %Plot W % 3D Plot of the volume fraction SurfPlot % Stopwatch stop tElapsed = toc(tStart)8-----

#### Parameters.m

```
% Numerical Model Parameterfile
% (c) by Hannes Pucher
% Sources : Perry's handbook of chemical engineering, VDI, infosticker on
% the bottle of the chemicals
%------
```

% Definition of the global parameters

global m global volume f initial EA global volume f initial BA global volume f initial W global volume f initial API global betafl EA global betafl BA global betafl W global ambientconc EA global ambientconc BA global ambientconc W global diffusion\_coefficent\_EA global diffusion coefficent BA global diffusion coefficent W global radius global t global diffusion c EA begin global diffusion c EA end global r\_EA\_1 global r\_EA\_2 global r\_EA\_3 global diffusion c BA begin global diffusion c BA end global r BA 1 global r BA 2 global r\_BA\_3 global radialPositions global volume\_f\_current\_EA global volume\_f\_current\_BA global Surface\_particle global memRadius plot global memVolumefraction EA plot global memVolumefraction BA plot global number of particles m §\_\_\_\_\_ \_\_\_\_\_ 8-----% Variables for the solver % Radius d measured = 163.49\*10^-6; % [m] Diameter of the emulsion measured by Msc. Nikolett Kiss = 0; % [m] Initial value for the radial r min vector = d measured/2; % [m] Final value for the r\_max radial vector r intervall = 100; % Radial steps

radius = linspace(r min,r max,r intervall); % [m] Radial vector % Time = 10; % [s] End time t total max t total = 0; % [s] Total time delta t = 1; % [s] Time steps in wich the PDE will be solved = 0; % [s] Initial value for the time t min vector = delta t; % [s] Final value for the time t max vector = r intervall; % Time steps t span = linspace(t min,t max,t span); % [s] Time t vector §\_\_\_\_\_ % Define the key parameters to get the radius, the volume fraction and % every other parameter for the plot function at tau = 0.1 t plot intervall = 0.1\*t total max; % [s] Plot intervall for tau = 0.1t intervall = t\_total\_max/t\_plot\_intervall; % [s] Intervall for the plot function; get value every .. [s] value get = t\_plot\_intervall/delta\_t; % Defines at wich row the data for the plot will be stand in the matrix §\_\_\_\_\_ 8-----% Parameters of the different components and solutions density\_quench = 0.9993; % [g/cm^3] Density of the quench Solution measured by Msc. Nicolett Kiss density\_disp = 0.9948; % [g/cm^3] Density of the organic phase measured by Msc. Nicolett Kiss density disp vector linspace(density disp,density disp,r intervall-1); % [g/cm^3] Density vector at the beginning (t=0) % Water = 1.000; % [g/cm^3] Density of water at 5 density water 5 [°C] = 0.997; % [g/cm^3] Density of water at 25 density water 25 [°C] = (density water 5 + density water 25)/2; % density water [g/ml] Average density of ethylacetate % Ethylacetate = 0.9168; % [g/cm^3] Density of density\_ea\_5 ethylacetate at 5 [°C] = 0.89362; % [g/cm^3] Density of density\_ea\_25 ethylacetate at 25 [°C] = (density ea 5 + density ea 25)/2; % density ea [g/ml] Average density of ethylacetate

```
% Benzylalcohol
density_ba_20
                          = 1.043; % [g/cm^3] Density of
benzylalcohol at 20 [°C]
density ba
                           = density ba 20;% [g/cm^3] Average density
of benzylalcohol
% Polyvinylalcohol
                          = 1.250; % [g/cm^3] Density of the
density pva
polyvinylalcohol (NOT REAL VALUE)
% Polymer
                  = 1; % [g/cm^3] Density of the polymer (NOT
density polymer
REAL VALUE)
% API
%density api
                           = ?; % [g/cm^3] Density of the api,
definition follows (NOT REAL VALUE)
§_____
§_____
% Parameters for the different phases
% Organic phase
mass polymer o
                          = 8.8; % [g] PLGA
                         = 44.76; % [g] Ethylacetate
mass ethylacetate o
mass_api_o
                          = 6.13; % [g] API
                         = 18.9; % [g] Benzylalcohol
mass_benzylalcohol_o
mass o
mass_polymer_o+mass_ethylacetate_o+mass_api_o+mass_benzylalcohol_o; % [g]
Mass of the organic phase
% Liquid phase
                          = 635; % [ml] Polyvinylalcohol [ONLY ON THE
volume pva l
OUTSIDE]
mass_pva_l
                          = volume_pva_l/density_pva; %
Polyvinylalcohol
mass_ethylacetate_l
                           = 45; % [g] Ethylacetate
                           = mass pva l+mass ethylacetate l; % [g]
mass l
Mass of the liquid phase
% Quench solution
                          = 3440; % [ml] Water
volume water q
                          = volume_water_q/density_water_5; % [g]
mass water q
Water
mass ethylacetate q
                         = 83.03; % [g] Ethylacetate
۶_____
               _____
                       _____
§_____
% Dimensions and operating parameter of the experimental vessel
                          = 1000 % [1/min] Revolutions per minute
n revolutions
                          = 112*10^(-3); % [m] Diameter of the
d stirrer
stirrer
d particle
                          = 2*r max; % [m] Diameter of the sphere
```

v relative \_ pi\*(n revolutions/60)\*d stirrer\*(d particle/d stirrer)^(1/3); % [m/s] Relative velocity % Reynolds, Schmidt and Sherwood number for the ethylacetate Re (v relative\*d particle)/Viscosity water kin; % Reynolds number Sc EA = Viscosity water kin/D EA WC; % Schmidt number = 2 + 0.347\*(Re)^(0.62)\*(Sc EA)^(0.31); % Sh EA Sherwood number by Steinberger/Treybal et al. % Reynolds, Schmidt and Sherwood number for the benzylalcohol Sc BA = Viscosity water kin/D BA WC; % Schmidt number Sh BA = 2 + 0.347\*(Re)^(0.62)\*(Sc BA)^(0.31); % Sherwood number by Steinberger/Treybal et al. % Mass transfer coefficent betafl EA = (Sh EA\*D EA WC)/d particle; % [m/s] Mass transfer coefficient of ethylacetate betafl BA = (Sh BA\*D BA WC)/d particle; % [m/s] Masstransport coefficent of benzylalcohol betafl W = 1 \* 10<sup>(-2)</sup>; % [m/s] Masstransport coefficent of water Surface particle = radius(1,r intervall)^2\*4\*pi; % [m^2] Initial surface of the sphere &\_\_\_\_\_ §\_\_\_\_\_ % Parameters for the shrinking function = (mass o); % [g] Initial mass of the whole mass disp initial disperse phase = r max^3\*pi\*4/3; % [m^3] Volume of the volume particle intial sphere at the beginning (t=0) mass particle initial = density disp\*volume particle initial; % [kg] Mass of one sphere at the beginning (t=0) volume disp inital = mass disp initial\*10^-3/density disp; % [m^3] Initial volume of the whole disperse phase number of particles m = mass disp initial\*10^-3/mass\_particle\_initial; % Number of spheres number of particles v volume disp inital/volume particle intial; % Number of spheres mass ethylacetate q temp = 0:mass benzylalcohol q temp = 0; ٥<u>,</u> <u>۶</u>\_\_\_\_\_ % Volumefraction in the quench solution = ((mass\_water\_q/density\_water\_5 + ambient volume ((mass ethylacetate q + mass ethylacetate l) / density ea 5) + mass pva l/density pva));

ambientconc EA = ((mass ethylacetate q + mass ethylacetate 1) / density ea 5)/ambient volume; % [m^3 EA/m^3 Quench Solution] Volumefraction of Ethylacetate in the quench solution = 0; % [m^3 BA/m^3 Quench Solution] ambientconc BA Volumefraction of Benzylalcohol in the quench solution ambientconc W = (mass water q / density water 5)/ambient volume; % [m^3 W/m^3 Quench Solution] Volumefraction of Water in the quench solution ambientconc PVA = (mass pva l/density pva)/ambient volume; % [m^3 PVA/m^3 Quench Solution] Volumefraction of PVA in the quench solution Sum ambient ambientconc BA+ambientconc EA+ambientconc PVA+ambientconc W % Sum ambient concentrations must be 1 §\_\_\_\_\_ 8-----% PDEPE parameter = 2; % PDEPE parameter m <u>ي</u>\_\_\_\_\_ 8-----% Initial volumefraction and massfraction in the sphere at the beginning (t=0) volume f initial EA = ((mass ethylacetate o \* 10<sup>-3</sup>) / density\_ea\_5)/volume\_disp\_inital; % [m^3 EA/m^3 DP]Volumefraction of ethylacetate in the sphere at the beginning (t=0) mass\_f\_initial\_EA = mass\_ethylacetate\_o /mass\_o; % [kg EA/kg DP] Massfraction of ethylacetate in the sphere at the beginning (t=0) volume f initial BA =  $((mass benzylalcohol o * 10^-3) /$ density ba)/volume disp inital; % [m^3 BA/m^3 DP] Volumefraction of benzylalcohol in the sphere at the beginning (t=0) mass f initial BA = mass benzylalcohol o / mass o; % [kg BA/kg DP] Massfraction of benzylalcohol in the sphere at the beginning (t=0) volume f initial PLGA = ((mass polymer o \* 10^-3) / density polymer)/volume disp inital; % [m^3 Polymer/m^3 DP] Volumefraction of Polymer (PLGA) mass f initial PLGA = mass polymer o / mass o; % [kg Polymer/kg DP] Massfraction of Polymer (PLGA) volume f initial W = 0; % [m^3 W/m^3 DP]Volumefraction of water in the sphere at the beginning (t=0)= 0; % [kg W/kg DP] Massfraction of water mass f initial W in the sphere at the beginning (t=0)= mass api o / mass o; % [kg API/kg DP] mass f initial API Massfraction of API volume\_f\_initial API = 1 - (volume f initial EA + volume\_f\_initial\_BA + volume\_f\_initial\_PLGA + volume\_f\_initial\_W); % [m^3 API/m<sup>3</sup> DP] Volumefraction of API

% API

```
density api
                             = (density disp -
density_ea_5*volume_f_initial_EA - density_ba*volume f initial BA -
density_polymer*volume_f_initial_PLGA)/volume_f_initial_API % [g/cm^3]
Density of the api (NOT REAL VALUE)
%display(density api);
if density api < 0</pre>
    display('Density Polymer wrong');
    stop;
end
volume f initial_API_c
                            = volume f initial API -
mass f initial API*density disp/density api;
% Density of the disperse phase without the ethylaceate and benzylalcohol
                             = volume f initial API +
volume_f_po_api
volume_f_initial_PLGA;
volume f API
                            = volume_f_initial_API/volume_f_po_api;
volume_f_PLGA
                            = volume f initial PLGA/volume f po api;
sum volume f
                            = volume f API + volume f PLGA;
if sum volume f ~= 1
    display('Volume fraction wrong !!');
    stop;
end
                            = volume f API * density api +
density po api
volume_f_PLGA * density_polymer; % [g/cm^3] Density of the
benzylalcohol, api and polymer solution
%display(density po api );
density disp controll
volume f initial API*density api+volume f initial BA*density ba+volume f
initial EA*density ea 5+volume f initial PLGA*density polymer; % [g/cm^3]
Controll the calculated values
if density_disp_controll ~= density_disp
    display('Mass fraction wrong !!');
    stop;
end
% Sum of all volumefractions at the beginning must be 1
                            = mass_f_initial_EA + mass_f_initial BA +
sum_mass_f_initial
mass_f_initial_PLGA + mass_f_initial_API + mass_f_initial_W;
+ volume_f_initial_API + volume_f_initial_PLGA + volume_f_initial_W;
if sum mass f initial ~= 1
```

```
display('Mass fraction wrong !!');
   stop;
end
if sum_volume_f_initial ~= 1
   display('Volume fraction wrong !!');
   stop;
end
% Mass distribution of the shells at the beginning t=0
for n=1:r intervall-1
    volume areas(1,n)
                                  = 4/3*pi*(radius(1,(n+1))^3-
    radius(1,n)^3); % [m^3] Volume of the spherical shells
    mass_volume_areas_init(1,n)
                                  =
    volume_areas(1,n).*density_disp_vector(1,n); % [kg] Mass of every
    spherical cell at the beginning
end
% Controll weight function
Sum mass
                              = sum(mass volume areas init); % [kg]
Sum the mass of the shells at the beginning t=0
                             = (mass o*10^-3)/number of particles m;
Sum mass controll
% [kg] Define the initial mass of every sphere
Error sum mass
                              = Sum mass/Sum mass controll; % Error of
the calculation
%display(Error sum mass);
                              = 0;
delta_m_EA_temp
                              = 0;
delta m BA temp
۶_____
8-----
% Shrinking parameters
                           = radius; % [m] Define the radial positions
radialPositions
volume f current EA
linspace(volume_f_initial_EA,volume_f_initial_EA,r_intervall); % Initial
volume fraction current vector for ethylacetate
volume f current BA
linspace(volume f initial BA,volume f initial BA,r intervall); % Initial
volume fraction current vector for benzylalcohol
<u>ي</u>_____
§_____
% Define Memory matrixes and variables
memVolumefraction EA plot = zeros(r intervall,t intervall+1);
```

```
memVolumefraction BA plot
                           = zeros(r intervall,t intervall+1);
memRadius plot
                            = zeros(r intervall,t intervall+1);
memMass plot
                           = zeros(1,t intervall+1);
memTime plot
                           = zeros(1,t intervall+1);
memAmbient EA plot
                           = zeros(1,t intervall+1);
memAmbient BA plot
                           = zeros(1,t intervall+1);
membetafl EA plot
                           = zeros(1,t intervall+1);
membetafl BA_plot
                           = zeros(1,t intervall+1);
                            = zeros(1,t intervall+1);
memDiffusion plot
memVolumefraction_EA_plot(:,1) = volume_f_current_EA'; % Define the first
row of the new volumefraction matrix
memVolumefraction BA plot(:,1) = volume f current BA'; % Define the first
row of the new volumefraction matrix
memRadius plot(:,1)
                            = radius'; % [m] Define the first row of
the radius matrix
memMass plot(1,1)
                          = r max^3*4/3*pi*density disp; % [kg]
Define the mass of the sphere at the beginning (t=0)
memTime plot(1,t intervall+1) = t total max; % [s] Define the start time
memAmbient EA plot(1,1) = ambientconc EA; % Define the
volume fraction distribution of the quench solution at the beginning (t=0)
memAmbient_BA_plot(1,1) = ambientconc_BA; % Define the
volume fraction distribution of the quench solution at the beginning (t=0)
membetafl_EA_plot(1,1) = betafl_EA; % [m/s] Define the mass
transport coefficient at the beginning (t=0)
membetafl BA plot(1,1) = betafl BA; % [m/s] Define the mass
transport coefficient at the beginning (t=0)
memDiffusion plot(1,1) = D EA WC; \[m^2/s]\] Define the diffusion
coefficient at the beginning (t=0)
<u>۶_____</u>
8-----
% Diffusioncoefficents of the different components and there constants
diffusion coefficent EA = D EA WC; % [m^2/s] Diffusion coefficient
of ethylacetate
                            = -7;
diffusion c EA begin
diffusion c EA_end
                            = -15;
r EA 1
                            = 1.7496; % Constant depending on the
system
r EA 3
                            = -((diffusion c EA begin)-
(diffusion c EA end))/(volume f initial PLGA-1) % Constant depending on
the system
r EA 2
                            = -(diffusion c EA end)-r EA 3 % Constant
depending on the system
diffusion coefficent BA
                          = D BA WC; % [m^2/s] Diffusion coefficient
of benzylalcohol
                            = -7;
diffusion c BA begin
                            = -15;
diffusion c BA end
r BA_1
                            = 1.6916; % Constant depending on the
system
r BA 3
                            = -((diffusion c BA begin)-
(diffusion c BA end))/(volume f initial PLGA-1) % Constant depending on
the system
                            = -(diffusion c BA end)-r BA 3 % Constant
r BA 2
depending on the system
```

diffusion\_coefficent\_W = 10^-10; % [m^2/s] Diffusion coefficient
of water
%-----%-----% CFL\_Number
velocity = (betafl\_EA\*density\_ea\_5\*volume\_f\_initial\_EA +
betafl\_BA\*density\_ba\*volume\_f\_initial\_BA)/density\_disp;
CFL = velocity\*delta t/(d measured/(r intervall\*2));

display(CFL);

°

#### **DiffusionCoefficient.m**

```
% Diffusion Coefficent
% Empirical correlation from HAYDUK and MINHAS and WILKE and Chang
% (c) by Hannes Pucher
% Sources : Perry's handbook of chemical engineering, VDI, infosticker on
% the bottle of the chemicals
۶_____
% Reaction Parameters
                       = 278.15; % Temperatur of the solutions [K]
temp
% Parameters of Ethylacetate
             = 88.1; % Molar mass of ethylacetate [g/mol]
M ethyl
T_melt_ethyl = -82.4; % Melting point of ethylacetate [°C]
T_boiling_ethyl = 77.1; % Boiling Point of ethylacetate [°C]
density_ethyl = 0.901; % Density of ethylacetate [g/cm^3]
molar volume ethyl = M ethyl/density ethyl; % Molar Volume of
ethylacetate [cm^3/mol]
% Parameters of Benzylalcohol
M_benzyl= 108.14; % Molar mass of benzylalcohol [g/mol]T_melt_benzyl= -15.3; % Melting point of benzylalcohol [°C]T_boiling_benzyl= 204.7; % Boiling Point of benzylalcohol [°C]density_benzyl= 1.0455; % Density of benzylalcohol [g/cm^3]
molar_volume_benzyl = M_benzyl/density benzyl; % Molar Volume of
benzylalcohol [cm^3/mol]
% Parameters of Water
M_water = 18.0153; % Molar mass of water [g/mol]
T_melt_water = 0.01; % Melting point of water [°C]
T_boiling_water = 99.974; % Boiling Point of water [°C]
Viscosity_water = 1518.1 * 10^-6; % [Pa*s] or [kg/(m*s)] VDI 5 Dba 4;
Dynamic viscosity of water at 5 [°C]
Viscosity_water_calc= Viscosity_water*10^3; % Dynamic viscosity of water
[cp]
Viscosity water kin = 1.518 * 10^(-6); % [m^2/s] VDI 5 Dba 4; Kinematic
Viscosity of water at 5 [°C]
               = 2.26; % Association factor of solvent water that
ass factor
accounts for hydrogen bonding
% Correlation for the diffusion coefficent by WILKE - CHANG, Perry's
% handbook of chemical engineering 5-51
D EA WC
                        = (7.4*10^(-8)*(ass factor*M water/1000)^(1/2)*temp)/
(Viscosity water calc*(molar volume ethyl)^(0.6))
                        = (7.4*10^(-8)*(ass factor*M water/1000)^(1/2)*temp)/
D BA WC
(Viscosity water calc*(molar volume benzyl)^(0.6))
```

% Correlation for the diffusion coefficent by HAYDUK and MINHAS; % Multicomponent Mass Transfer 1993 by Ross Taylor, R. Krishna %epsilon\_b\_EA = 9.58/molar\_volume\_ethyl-1.12; %D\_EA\_HM = 1.25\*10^(-8)\*(molar\_volume\_ethyl^(-0.19) -0.292)\*temp^(1.52)\*Viscosity\_water\_calc^(epsilon\_b\_EA) % Dissusion coefficent of ethylacetate [m^2/s]

%epsilon\_b\_BA = 9.58/molar\_volume\_benzyl-1.12; %D\_BA\_HM = 1.25\*10^(-8)\*(molar\_volume\_benzyl^(-0.19)-0.292)\*temp^(1.52)\*Viscosity\_water\_calc^(epsilon\_b\_BA) % Diffusion coefficent of benzylalcohol [m^2/s]

# Calcpde.m

```
% Numerical Solution Calcpde
% (c) by Hannes Pucher
§_____
                          _____
% Definition of the c,f,s parameter for the PDEPE Solver
function [c,f,s, diffusion coefficent EA] = calcpde(radius, t,
volume fraction, Dvolume fractionDradius)
    % Definition of the global parameters
    global diffusion coefficent BA
    global diffusion coefficent W
    global r EA 1
    global r EA 2
    global r EA 3
    global r BA 1
    global r BA 2
    global r BA 3
    global volume f initial API
    % Diffusion coefficients
    diffusion coefficent EA = r EA 1.*10.^(-(r EA 2+r EA 3*(1-
    volume fraction(1,1)-volume fraction(2,1)-volume f initial API)));%
    [m<sup>2</sup>/s] Diffusion Coefficient of ethylacetate
    diffusion_coefficent_BA = r_BA_1.*10.^(-(r_BA_2+r_BA_3*(1-
    volume fraction(1,1)-volume fraction(2,1)-volume f initial API)));%
    [m<sup>2</sup>/s] Diffusion Coefficient of benzylalcohol
    c = [1;1;1];
    f = [diffusion coefficent EA; diffusion coefficent BA;
    diffusion coefficent W].*Dvolume fractionDradius;
    s = [0;0;0];
```

```
end
```

## Calcic.m

```
% Numerical Solution Initial Condition for the PDEPE
% (c) by Hannes Pucher
8-----
function volume fraction 0 = calcic(radius)
    % Definition of the global parameters
    global volume f initial EA
    global volume_f_initial_BA
    global volume f initial W
    global radialPositions
    global volume f current EA
    global volume_f_current_BA
    \% Define the initial condition to solve the PDE
    volume f initial EA = interp1(radialPositions, volume f current EA,
    radius, 'spline');
    volume f initial BA = interp1(radialPositions, volume f current BA,
    radius, 'spline');
    volume f initial W = interp1(radialPositions, volume f current EA,
    radius, 'spline');
    volume fraction 0 = [volume f initial EA; volume f initial BA;
    volume f initial W];
```

end

## Calcbc.m

```
% Numerical Solution Boundary Condition for the PDEPE
% (c) by Hannes Pucher
8-----
function [pl,ql,pr,qr] = calcbc(radius l, volume fraction l, radius r,
volume fraction r,t)
    % Definition of the global parameters
    global betafl EA
    global betafl BA
    global betafl W
    global ambientconc W
    global Surface particle
    global number_of_particles_m
    % Center of the microparticle (r=0)
    pl=[0;0;0];
    ql=[1;1;1];
    % Surface of the microparticle (r=r max)
    %Surface particle = 1;
    ambientconc EA bc = 0;
    ambientconc BA bc = 0;
    %number of particles m=1;
    pr=[betafl_EA*(volume_fraction_r(1) -
    ambientconc EA bc); betafl BA* (volume fraction r(2) -
    ambientconc BA bc); betafl W* (volume fraction r(3)-ambientconc W)]; %-
    equilibrium conc;
    qr=[1;1;1];
```

end

#### Shrinking.m

```
% Numerical Model for Shrinking
% (c) by Hannes Pucher
§_____
                           _____
٥<u>,</u>
% Define the different matrixes used in the calculation
volume fraction area EA
                                      = zeros(t span,r intervall-1);
volume fraction area BA
                                      = zeros(t span, r intervall-1);
                                      = zeros(1,r_intervall-1);
= zeros(1,r_intervall-1);
volume areas
volume distribution
                                      = zeros(t_span-1,r_intervall-1);
= zeros(t_span-1,r_intervall-1);
volume matrix EA
volume matrix BA
Weigth new
                                      = zeros(1,t_span-1);
radius new cell
                                      = zeros(1,t_span);
radius new cell temp
                                      = zeros(1,t_span-1);
delta radius
                                      = zeros(1,t_span-1);
                                      = zeros(1,r_intervall-1);
mass volume areas
8----
    _____
§_____
% Define the volume and mass difference of the ethylacetate from one
% timestep to another
for n=1:r intervall-1
   for u=1:t span-1
    volume_fraction_area_EA(:,n) = (volume_fraction_EA(:,n) +
    volume_fraction_EA(:,n+1))./2; % Mean volumefraction of two adjacent
    cells
    volume_areas(1,n)
                                   = 4/3*pi*(radius(1,(n+1))^3-
    radius(1,n)^3); % [m^3] Volume of the spherical shells
    mass volume areas(1,n)
    volume_areas(1,n).*density_disp_vector(1,n); % [kg] Mass of every
    spherical cell at the beginning
    volume matrix EA(u,n) = ((volume fraction area <math>EA(u,n) -
    volume fraction area EA(u+1,n))); % Volume fraction difference
    between each timestep
    Sum Volume EA
                                  = sum(volume matrix EA); % Sum the
    volume matrix to get the whole difference from one timestep to
    another
   end
end
          ------
8_____
% Define the volume and mass difference of the benzylalcohol from one
% timestep to another
```

```
for n=1:r intervall-1
    for u=1:t span-1
    volume fraction area BA(:,n) = (volume fraction BA(:,n) +
    volume_fraction_BA(:,n+1))./2; % Mean volumefraction of two adjacent
    cells
                                    = ((volume fraction area BA(u,n) -
    volume matrix BA(u,n)
    volume fraction area BA(u+1,n))); % Volume fraction difference
    between each timestep
    Sum Volume BA
                                     = sum(volume matrix BA); % Sum the
    volume matrix to get the whole difference from one timestep to
    another
   end
end
<u>ç</u>_____
§_____
% Define the mass and volume loss in every shell and define the new
radius
% after delta t
%sum volumefraction
                                         = volume f current EA
density new
                                        = density ea 5 *
volume fraction area EA(t span,:) + density ba *
volume fraction area BA(t span,:) + density po api*(1-
volume fraction area EA(t span,:)-volume fraction area BA(t span,:));
%[kg/m<sup>-3</sup>] New density of the spherical cells
mass_fraction_initial_EA
(density_ea_5*volume_fraction_area_EA(1,:))./density_disp_vector(1,:); %
Inital mass fraction distribution of ethylacetate
mass fraction final EA
(density ea 5*volume fraction area EA(t span,:))./density new; % Final
mass fraction distribution of ethylacetate
delta mass fraction EA
                                        = mass fraction initial EA-
mass fraction final EA; % Difference of the mass fraction of ehtylacetate
delta m EA
mass volume areas init.*delta mass fraction EA; % [kg] Mass difference of
ethylacetate in every spherical shell
                                        = sum(delta m EA); % [kg] Mass
sum mass EA
loss of ethylacetate of one sphere
sum delta m EA
                                        = delta m EA + delta m EA temp;
mass fraction initial BA
(density ba*volume fraction area BA(1,:))./density disp vector(1,:); %
Inital mass fraction distribution of benzylalcohol
```

mass fraction final BA = (density ba\*volume fraction area BA(t span,:))./density new; % Final mass fraction distribution of benzylalcohol delta\_mass\_fraction\_BA = mass\_fraction\_initial\_BAmass fraction final BA; % Difference of the mass fraction of benzylalcohol delta m BA = mass volume areas init.\*delta mass fraction BA; % [kg] Mass difference of benzylalcohol in every spherical shell sum mass BA = sum(delta m BA); % [kg] Mass loss of benzylalcohol of one sphere = delta m BA + delta m BA temp; sum delta m BA mass\_volume\_areas\_new = mass\_volume\_areas\_init sum delta m EA - sum delta m BA ; % [kg] New mass of every sperical shell sum mass = sum(mass volume areas new); % [kg] Mass of the new sphere Volume areas new mass\_volume\_areas\_new./density\_disp\_controll; % [m^3] Define the new volume of every spherical cell delta\_volume = volume areas -Volume areas new; % [m^3] Delta volume [temp dim delta volume] = size(delta volume); sum Sum volume = zeros(size(delta volume)); for j = 1:dim\_delta\_volume for k = 1:jsum Sum volume(j) = sum Sum volume(j) + delta volume(k); % [m^3] Sum delta volume matrix to get the whole difference from one timestep to another end end clear temp; for  $x = 1:t_span-1$ radius new cell temp(1,x) = ((-3/(4\*pi)\*sum Sum volume(1,x)) +radius(1,x+1)^3)^(1/3); % [m] New Radius of every shell
```
radius new cell(1,1)
                                   = radius(1,1); % [m] Define the first
    element of the new radial vector
    radius new cell(1,x+1)
                                   = radius new cell temp(1,x); % [m]
    Define the new radius of ever sphere cell
end
               _____
8----
§_____
% Define the new parameters needed for further calculations
radius new
                                       = radius new cell(1,t span); %
[m] Radius of the new sphere
                                       = radius new^2*pi*4; % [m^2]
Surface particle new
Surface of the new sphere
density disp vector
                                       = density new; % [kg/m^3] Density
of the new sphere
% Define the mass loss and the new ambient concentration
mass volume areas
                                       = mass volume areas new; % [kg]
Mass of every spherical sphere
mass ethylacetate q new
                                       = mass ethylacetate q temp +
sum_mass_EA*number_of_particles_m * 10^3; % [g] Mass loss of ethylacetate
mass benzylalcohol q new
                                       = mass benzylalcohol q temp +
sum mass BA*number of particles m * 10^3; % [g] Mass loss of
benzylalcohol
% Controll the mass balance
mass ethylacetate sphere
sum(mass fraction final EA.*mass volume areas init)*number of particles m
*10^3; % [g] Ethylacetate in the sphere at the end
mass benzylalcohol sphere
sum(mass fraction final BA.*mass volume areas init)*number of particles m
*10^3; % [g] Benzylalcohol in the sphere at the end
error ethylacetate
                                       = (mass ethylacetate o-
mass ethylacetate q new-
mass_ethylacetate_sphere)/mass_ethylacetate_o*100; % Error of the mass
balance of EA must be 0
error benzylalcohol
                                       = (mass benzylalcohol o-
mass_benzylalcohol_q_new-
mass_benzylalcohol_sphere)/mass_benzylalcohol_o*100; % Error of the mass
balance of BA must be 0
%density quench
                                        = %[kg/m^3] New density of the
quench solution
ambientconc EA
                                       = ((mass ethylacetate 1 +
mass ethylacetate q + mass ethylacetate q new) /
density ea 5)/((mass water q + mass ethylacetate q +
mass_ethylacetate_q_new + mass_l + mass_benzylalcohol_q_new) /
density_quench); % [m^3 EA/m^3 Quench Solution] New ambient concentration
ambientconc BA
                                       = ((mass benzylalcohol q new) /
density_ba)/((mass_water_q + mass_ethylacetate_q +
mass_ethylacetate_q_new + mass_benzylalcohol_q_new + mass_l) /
density quench); % [m^3 BA/m^3 Quench Solution] New ambient concentration
% Dimensions and operating parameter of the experimental vessel
```

d particle = 2\*radius new; % [m] Diameter of the sphere v relative pi\*(n revolutions/60)\*d stirrer\*(d particle/d stirrer)^(1/3); % [m/s] Relative velocity = (v relative\*d particle)/Viscosity water kin; % Re Reynolds number % Reynolds, Schmidt and Sherwood number for the ethylacetate = Viscosity\_water\_kin/D\_EA\_WC; % Schmidt number = 2 + 0.347\*(Re)^(0.62)\*(Sc\_EA)^(0.31); % Sc EA Sh EA Sherwood number by Steinberger/Treybal et al. % Reynolds, Schmidt and Sherwood number for the benzylalcohol Sc BA = Viscosity water kin/D BA WC; % Schmidt number  $= 2 + 0.347 (\text{Re})^{(0.62)} (\text{Sc} BA)^{(0.31)};$ Sh BA Sherwood number by Steinberger/Treybal et al. % Mass transfer coefficent = (Sh\_EA\*D\_EA\_WC)/d\_particle; % [m/s] Mass betafl EA transfer coefficient of ethylacetate betafl BA = (Sh BA\*D BA WC)/d particle; % [m/s]

Masstransport coefficent of benzylalcohol

# **II. Plot Files**

#### Plot\_Radius.m

```
% Plot file for Radius for the Numerical Solution
% (c) by Hannes Pucher
§_____
% Creation of the different matrixes used in the calculation
[temp dim memTime]
                                = size(memTime); % Get the size of the
memTime vector
memTime temp
                                = zeros(1,dim memTime+1);
memRadius temp
                                 = zeros(1,dim memTime+1);
% Resize and rearange the time and radius vector
for p = 1:dim memTime
                                  = t(1,1); % [s] Starting time
    memTime temp(1,1)
    memTime_temp(1,p+1)
                                  = memTime(1,p); % [s] Rearange the
    time vector
                                  = r_max; % [m] Radius at the
    memRadius_temp(1,1)
    beginning
    memRadius_temp(1,p+1)
                           = memRadius_end(1,p); % [m] Rearange
    the radius vector
end
memTime
                                 = memTime temp; % Define the variables
used in the plot
memRadius_end
                                = memRadius_temp; % Define the
variables used in the plot
for o = 1:t intervall
    memVolumefraction EA plot(:,o+1) =
    memVolumefraction_EA(:,o*value_get); % Volume matrix fraction of the
    ethylacetate
    memVolumefraction BA plot(:,o+1) =
    memVolumefraction BA(:,o*value get); % Volume matrix fraction of the
    benzylalcohol
    volume fraction rest
                                    = 1 - memVolumefraction EA plot -
    memVolumefraction BA plot; % Volume fraction of the rest
    (Polymere, API, BA, Polyvinylalcohol)
    memRadius plot(:,o+1) = memRadius(:,o*value_get); %
    [m]Radius matrix of the new sphere
    memMass plot(1, 0+1)
                                    = memMass(1,o*value get); % [kg]
    Mass vector of the new sphere
```

```
memTime plot(1,0)
                                 = memTime(1,(o-1)*value get+1); %
    [s] Rearangend time vector
    memAmbient EA plot(1,o+1)
                                 = memAmbient EA(1,o*value get); %
    [m^3 EA/m^3 Quench Solution] New volumefraction vector of
    ethylacetate in the quench solution
    memAmbient BA plot(1,o+1) = memAmbient BA(1,o*value get); %
    [m^3 BA/m^3 Quench Solution] New volumefraction vector of
    benzylalcohol in the quench solution
    membetafl EA plot(1,o+1) = membetafl EA(1,o*value get); %
    [m/s] Mass transport coefficient of ethylacetate
    membetafl BA plot(1,o+1)
                                 = membetafl BA(1,o*value get); %
    [m/s] Mass transport coefficient of benzylalcohol
end
<u>ç</u>_____
8-----
% Defines the normalized radius
for q = 1:t intervall+1
    memRadius plot normalized(:,q) =
    memRadius plot(:,q)/memRadius plot(t span,1); % Normalized radius
    matrix
end
8-----
§_____
% Data from 12/16.08.2010
QICPIC_data_1 = [163.49 \ 115 \ 111.675 \ 105.03 \ 99.5 \ 105 \ 96.25 \ 99.985
92.596 100.165].*10^-6; % [m] SMD measured with QICPIC
QICPIC_time_1 = [0 12 50 85 145 205 265 270 315 1170]; % [min]
QICPIC time
QICPIC_time_1_plot = QICPIC_time_1 * 60; % [sec] QICPIC time
HELOS data 1 = [163.49 116 96 110 96.66 104 106.01 107].*10^-6; %
[m] SMD measured with HELOS
HELOS time 1 = [0 50 85 225 265 270 315 1170]; % [sec] HELOS time
HELOS time 1 plot = HELOS time 1 * 60; % [sec] HELOS time
% Data from 19.11.2010
HELOS data 2 = [163.49 135.36 121.29 118.43 123.99 123.55 128.15
106.68 114.01 118.61].*10^-6; % [m] SMD measured with HELOS
HELOS time 2
               = [0 3.66 9.66 30.5 45.33 60.08 72.76 90.08 300 1200];
% [min] HELOS time
HELOS_time_2_plot = HELOS_time_2 * 60; % [sec] HELOS time
          ------
8-----
% Save all variables
save All Parameters.mat
```

```
۶<u>_____</u>
% Plot Radius vs Time
figure(1)
plot(QICPIC_time_1_plot/3600,QICPIC_data_1*10^6,'bd','MarkerSize',17,'Mar
kerFaceColor', 'b')
hold on
plot(HELOS time 1 plot/3600, HELOS data 1*10^6, 'gs', 'MarkerSize', 17, 'Marke
rFaceColor', 'g')
%hold on
%plot(HELOS time 2 plot/3600, HELOS data 2*10^6, 'ro', 'MarkerSize', 17, 'Mark
erFaceColor','r')
hold on
plot(memTime/3600,memRadius end*2*10^6,'k','LineWidth',2)
% Label and Title of the plot
title('', 'FontSize',35)
xlabel('Time [h]', 'FontSize',20)
ylabel('SMD [\mum]', 'FontSize',20)
set(gca, 'FontSize', 20)
% Legend
legend('QICPIC', 'HELOS', 'Location', 'NorthEast')
% Define the intervall of the axis
axis([0 t total max/3600 0*10^2 1.8*10^2])
% Resize the plot to fullscreen
set(gcf, 'position', get(0, 'screensize'))
% Save Figure as SMD.tiff
saveas(gcf,'SMD.tiff', 'tiffn');
§_____
% Plot Radius vs Volumefraction of the Polymere
figure(2)
plot(memRadius_plot_normalized,volume fraction rest,'LineWidth',2)
% Label and Title of the plot
title('', 'FontSize',35)
% Real Radial Positions
%xlabel('Radius [m]', 'FontSize',30)
% Normalized Radial Positions
xlabel('Normalized Radius', 'FontSize',20)
ylabel('\phi {Remaining Components}', 'FontSize',20)
set(gca, 'FontSize', 20)
% Legend
legend('\tau = 0','\tau = 0.1','\tau = 0.2','\tau = 0.3','\tau =
0.4','\tau = 0.5','\tau = 0.6','\tau = 0.7','\tau = 0.8','\tau =
0.9', '\tau = 1.0', 'Location', 'EastOutside')
% Resize the plot to fullscreen
set(gcf, 'position', get(0, 'screensize'))
% Save Figure as Volumefraction Poly.tiff
saveas(gcf,'Volumefraction Poly.tiff', 'tiffn');
```

%\_\_\_\_\_

# Plot\_Diffusion\_EA.m

```
% Plot file for Diffusion Coefficient of Ethylacetate
% (c) by Hannes Pucher
§_____
% Definition of the Diffusion Coefficient Matrix
diffusion coefficent EA=zeros(r intervall,t intervall+1);
for u=1:r intervall
    for n=1:t_intervall+1
     diffusion coefficent EA(u,n) = r EA 1.*10.^(-
     (r_EA_2+r_EA_3*(volume_fraction_rest(u,n)-volume f initial API)));
    end
end
% Plot Radius vs Diffusion Coefficient
figure(11)
semilogy (memRadius plot normalized, diffusion coefficent EA, 'LineWidth', 2)
% Label and Title of the plot
title('', 'FontSize',30)
% Real Radial Positions
%xlabel('Radius [m]', 'FontSize',30)
% Normalized Radial Positions
xlabel('Normalized Radius', 'FontSize',20)
ylabel('D {EA} [m^2/s]', 'FontSize',20)
set(gca, 'FontSize', 20)
% Legend
legend('\tau = 0','\tau = 0.1','\tau = 0.2','\tau = 0.3','\tau =
0.4','\tau = 0.5','\tau = 0.6','\tau = 0.7','\tau = 0.8','\tau =
0.9', '\tau = 1.0', 'Location', 'EastOutside')
% Resize the plot to fullscreen
set(gcf, 'position', get(0, 'screensize'))
% Save Figure as diffusion coefficent EA.tiff
saveas(gcf,'diffusion coefficent EA.tiff', 'tiffn');
hold on
```

# Plot\_Diffusion\_BA.m

```
% Plot file for Diffusion Coefficient of Benzy alcohol
% (c) by Hannes Pucher
§_____
% Definition of the Diffusion Coefficient Matrix
diffusion coefficent BA=zeros(r intervall,t intervall+1);
for u=1:r intervall
    for n=1:t_intervall+1
     diffusion coefficent BA(u,n) = r BA 1.*10.^(-
     (r_BA_2+r_BA_3*(volume_fraction_rest(u,n)-volume f initial API)));
    end
end
% Plot Radius vs Diffusion Coefficient
figure(12)
semilogy (memRadius plot normalized, diffusion coefficent BA, 'LineWidth', 2)
% Label and Title of the plot
title('', 'FontSize',30)
% Real Radial Positions
%xlabel('Radius [m]', 'FontSize',30)
% Normalized Radial Positions
xlabel('Normalized Radius', 'FontSize',20)
ylabel('D {BA} [m^2/s]', 'FontSize',20)
set(gca, 'FontSize', 20)
% Legend
legend('\tau = 0','\tau = 0.1','\tau = 0.2','\tau = 0.3','\tau =
0.4','\tau = 0.5','\tau = 0.6','\tau = 0.7','\tau = 0.8','\tau =
0.9', '\tau = 1.0', 'Location', 'EastOutside')
% Resize the plot to fullscreen
set(gcf, 'position', get(0, 'screensize'))
% Save Figure as diffusion coefficent BA.tiff
saveas(gcf,'diffusion coefficent BA.tiff', 'tiffn');
hold on
```

#### Plot\_EA.m

```
% Plot file for Ethylacetate for the Numerical Solution
% (c) by Hannes Pucher
§_____
% Ethylacetate
۶_____
% Plot matrixs for the ambient concentration and mass transport
coefficient
memAmbient_EA_plot_fine = zeros(1,t_total+1);
memAmbient EA plot fine(1,1) = memAmbient EA plot(1,1);
membetafl EA plot fine = zeros(1,t total+1);
membetafl EA plot fine(1,1) = membetafl EA plot(1,1);
for z = 2:t total+1
    memAmbient EA plot fine(1,z) = memAmbient EA(1,z-1);
    membetafl \overline{EA} plot fine(1,z) = membetafl \overline{EA}(1,z-1);
end
<u>ç</u>_____
§_____
% Plot Volume fraction in the quench solution vs time
figure(31)
plot(memTime/3600,memAmbient EA plot fine, 'LineWidth',2)
% Label and Title of the plot
title('', 'FontSize',35)
xlabel('Time [h]', 'FontSize',20)
ylabel('\phi {Ethylacetate in Continuous Phase}', 'FontSize',20)
set(gca, 'FontSize', 20)
% Define the intervall of the axis
axis([0 t total/3600 0 6*10^-2])
% Resize the plot to fullscreen
set(gcf, 'position', get(0, 'screensize'))
% Save Figure as Volumefraction EA in the Quench.tiff
saveas(gcf,'Volumefraction EA in the Quench.tiff', 'tiffn');
ş_____
§_____
% Plot Radius vs Volume fraction
figure(32)
plot (memRadius plot normalized, memVolumefraction EA plot, 'LineWidth', 2)
% Label and Title of the plot
title('', 'FontSize',35)
% Normalized Radial Positions
```

```
xlabel('Normalized Radius', 'FontSize',20)
ylabel('\phi {Ethylacetate}', 'FontSize',20)
set(gca, 'FontSize', 20)
set(gca,'YTickLabel',{'0','0.10','0.20','0.30','0.40','0.50','0.60','0.70
',})
% Legend
legend('{\tau} = 0', '{\tau} = 0.1', '{\tau} = 0.2', '{\tau} = 0.3', '{\tau}
= 0.4', \{ \{ u \} = 0.5', \{ \{ u \} = 0.6', \{ \{ u \} = 0.7', \{ \{ u \} = 0.7' \}
0.8', '{\tau} = 0.9', '{\tau} = 1.0', 'Location', 'EastOutside')
% Define the intervall of the axis
%axis([0 1 0.0 0.8])
% Resize the plot to fullscreen
set(gcf, 'position',get(0, 'screensize'))
% Save Figure as Volumefraction EA.tiff
saveas(gcf, 'Volumefraction EA.tiff', 'tiffn');
_____
۶_____
<u>۶_____</u>
% Plot Time vs Delta Mass
figure(33)
plot(memTime plot/3600,memMass plot,'LineWidth',2)
% Label and Title of the plot
title('', 'FontSize',35)
xlabel('Time [h]', 'FontSize',20)
ylabel('m {S} [kg]', 'FontSize',20)
set(gca, 'FontSize', 20)
% Define the intervall of the axis
%axis([0 5 0 3*10^-12])
% Resize the plot to fullscreen
set(gcf, 'position',get(0, 'screensize'))
% Save Figure as Mass Sphere.tiff
saveas(gcf,'Mass Sphere.tiff', 'tiffn');
                 _____
§_____
% Plot Time vs Mass Transport Coefficient
figure(34)
plot(memTime/3600,membetafl_EA_plot fine,'LineWidth',2)
% Label and Title of the plot
title('', 'FontSize',35)
xlabel('Time [h]', 'FontSize',20)
ylabel('\beta {Ethylacetate} [m/s]', 'FontSize',20)
set(gca, 'FontSize', 20)
%set(gca, 'YTickLabel', {'0', '0.10', '0.20', '0.30', '0.40', '0.50', '0.60', '0.7
0', \})
% Define the intervall of the axis
```

### Plot\_BA.m

```
% Plot file for Benzylalcohol for the Numerical Solution
% (c) by Hannes Pucher
8-----
% Benzylalcohol
۶_____
% Plot matrixs for the ambient concentration and mass transport
coefficient
memAmbient_BA_plot_fine = zeros(1,t_total+1);
memAmbient_BA_plot_fine(1,1) = memAmbient_BA_plot(1,1);
membetafl BA plot fine = zeros(1,t total+1);
membetafl BA plot fine(1,1) = membetafl BA plot(1,1);
for z = 2:t total+1
    memAmbient BA plot fine(1,z) = memAmbient BA(1,z-1);
    membetafl BA plot fine(1,z) = membetafl BA(1,z-1);
end
§_____
8-----
% Plot Volume fraction in the quench solution vs time
figure(21)
plot(memTime/3600,memAmbient BA plot fine, 'LineWidth',2)
% Label and Title of the plot
title('', 'FontSize',35)
xlabel('Time [h]', 'FontSize',20)
ylabel('\phi_{Benzylalcohol in Continuous Phase}', 'FontSize',20)
set(gca, 'FontSize', 20)
% Define the intervall of the axis
axis([0 t total/3600 0 0.005])
% Resize the plot to fullscreen
set(gcf, 'position',get(0, 'screensize'))
% Save Figure as Volumefraction BA in the Quench.tiff
saveas(gcf, 'Volumefraction_BA_in_the_Quench.tiff', 'tiffn');
8-----
% Plot Radius vs Volume fraction
figure(22)
plot(memRadius plot normalized,memVolumefraction BA plot,'LineWidth',2)
% Label and Title of the plot
title('', 'FontSize',35)
```

```
% Normalized Radial Positions
xlabel('Normalized Radius', 'FontSize',20)
ylabel('\phi {Benzylalcohol}', 'FontSize',20)
set(gca, 'FontSize', 20)
set(gca, 'YTickLabel', {'0', '0.05', '0.10', '0.15', '0.20', '0.25'})
% Legend
legend('{\tau} = 0', '{\tau} = 0.1', '{\tau} = 0.2', '{\tau} = 0.3', '{\tau}
= 0.4', \{ \{ u \} = 0.5', \{ \{ u \} = 0.6', \{ \{ u \} = 0.7', \{ \{ u \} = 0.7' \}
0.8', '{\tau} = 0.9', '{\tau} = 1.0', 'Location', 'EastOutside')
% Define the intervall of the axis
%axis([0 1 0 0.3])
% Resize the plot to fullscreen
set(gcf, 'position',get(0, 'screensize'))
% Save Figure as Volumefraction BA.tiff
saveas(gcf, 'Volumefraction BA.tiff', 'tiffn');
_____
۶_____
§_____
% Plot Time vs Mass Transport Coefficient
figure(23)
plot(memTime/3600,membetafl BA plot fine, 'LineWidth',2)
% Label and Title of the plot
title('', 'FontSize',35)
xlabel('Time [h]', 'FontSize',20)
ylabel('\beta_{Benzylalcohol} [m/s]', 'FontSize',20)
set(gca, 'FontSize', 20)
% Define the intervall of the axis
axis([0 t_total/3600 5*10^-3 10*10^-3])
% Resize the plot to fullscreen
set(gcf, 'position',get(0, 'screensize'))
% Save Figure as MassTransportCoefficient BA.tiff
saveas(gcf, 'MassTransportCoefficient BA.tiff', 'tiffn');
§_____
```

# Surf\_Plot\_EA.m

```
% Surf plot file for EA
% (c) by Hannes Pucher
§_____
8-----
% Define the new time matirx for the 3D Plot
mem time surf = zeros(t span, 11);
for n = 1 : t span
    mem time surf(n,:)=memTime plot/3600';
end
§_____
8-----
% Surf Plot Time vs Radius vs Volume fraction
figure(200)
surf(mem_time_surf,memRadius_plot*10^6,memVolumefraction_EA_plot)
% Label and Title of the plot
title('', 'FontSize',35)
xlabel('Time [h]', 'FontSize',20)
ylabel('Radius', 'FontSize',20)
zlabel('\phi_{Ethyl acetate}', 'FontSize',20)
set(gca, 'FontSize', 20)
view([125 15]);
% Legend
%legend('QICPIC', 'HELOS 1', 'HELOS 2', 'Location', 'NorthEast')
% Define the intervall of the axis
%axis([0 t total max 0 85])
% Resize the plot to fullscreen
set(gcf, 'position',get(0, 'screensize'))
% Save Figure as 3DPlot.tiff
saveas(gcf,'3DPlot_EA.tiff', 'tiffn');
```

## Surf\_Plot\_BA.m

```
% Surf plot file for BA
% (c) by Hannes Pucher
§_____
8-----
% Define the new time matirx for the 3D Plot
mem time surf = zeros(t span, 11);
for n = 1 : t span
    mem time surf(n,:)=memTime plot/3600';
end
§_____
8-----
% Surf Plot Time vs Radius vs Volume fraction
figure(200)
surf(mem_time_surf,memRadius_plot*10^6,memVolumefraction_BA_plot)
% Label and Title of the plot
title('', 'FontSize',35)
xlabel('Time [h]', 'FontSize',20)
ylabel('Radius', 'FontSize',20)
zlabel('\phi_{Benzyl alcohol}', 'FontSize',20)
set(gca, 'FontSize', 20)
view([125 15]);
% Legend
%legend('QICPIC', 'HELOS 1', 'HELOS 2', 'Location', 'NorthEast')
% Define the intervall of the axis
%axis([0 t total max 0 85])
% Resize the plot to fullscreen
%set(gcf,'position',get(0,'screensize'))
% Save Figure as 3DPlot.tiff
saveas(gcf,'3DPlot_BA.tiff', 'tiffn');
```

# Surf\_Plot\_RC.m

```
% Surf plot file for RC
% (c) by Hannes Pucher
§_____
8-----
% Define the new time matirx for the 3D Plot
mem time surf = zeros(t span, 11);
for n = 1 : t_span
   mem time surf(n,:)=memTime plot/3600';
end
§_____
8-----
% Surf Plot Time vs Radius vs Volume fraction
figure(200)
surf(mem_time_surf,memRadius_plot*10^6,volume_fraction_rest)
% Label and Title of the plot
title('', 'FontSize',35)
xlabel('Time [h]', 'FontSize',20)
ylabel('Radius', 'FontSize',20)
zlabel('\phi {Remaining Components}', 'FontSize',20)
set(gca, 'FontSize', 20)
view([310 25]);
% Legend
%legend('QICPIC', 'HELOS 1', 'HELOS 2', 'Location', 'NorthEast')
% Define the intervall of the axis
%axis([0 t total max 0 85])
% Resize the plot to fullscreen
set(gcf, 'position',get(0, 'screensize'))
% Save Figure as 3DPlot.tiff
saveas(gcf,'3DPlot_RC.tiff', 'tiffn');
```

# **III.** Parameter Studies

#### Sensivity\_Study.m

```
% Sensivity Study for the Time Step Size and the Number of Radial
Sections
% (c) by Hannes Pucher
§_____
8-----
% Clear, Close and delete all
clc
clear all
close all
           _____
§____
% Load memTime_plot files in the workspace
load('memTime_plot_tspan=10')
memTime_plot_tspan_10 = memTime_plot;
load('memTime_plot_tspan=25')
memTime_plot_tspan_25 = memTime_plot;
load('memTime_plot_tspan=50')
memTime_plot_tspan_50 = memTime_plot;
% Load files for t_span=10
load('memRadius_plot_1_tspan=10.mat')
memRadius_plot_1_tspan_10 = memRadius_plot;
load('memRadius_plot_0.5_tspan=10.mat')
memRadius_plot_0_5_tspan_10 = memRadius_plot;
load('memRadius_plot_0.1_tspan=10.mat')
memRadius_plot_0_1_tspan_10 = memRadius_plot;
load('memRadius_plot_0.05_tspan=10.mat')
memRadius_plot_0_05_tspan_10 = memRadius_plot;
load('Volumefraction Poly 1 tspan=10.mat')
Volume fraction Polymere 1 tspan 10 = volume fraction Rest;
load('Volumefraction Poly 0.5 tspan=10.mat')
Volume_fraction_Polymere_0_5_tspan_10 = volume_fraction_Rest;
load('Volumefraction_Poly_0.1_tspan=10.mat')
Volume_fraction_Polymere_0_1_tspan_10 = volume_fraction_Rest;
load('Volumefraction_Poly_0.05_tspan=10.mat')
Volume fraction Polymere 0 05 tspan 10 = volume fraction Rest;
% Load files for t_span = 25
load('memRadius plot 1 tspan=25.mat')
memRadius_plot_1_tspan_25 = memRadius_plot;
load('memRadius_plot_0.5_tspan=25.mat')
memRadius_plot_0_5_tspan_25 = memRadius_plot;
load('memRadius plot 0.1 tspan=25.mat')
memRadius plot 0 1 tspan 25 = memRadius plot;
load('memRadius plot 0.05 tspan=25.mat')
```

```
memRadius_plot_0_05_tspan_25 = memRadius_plot;
```

```
load('Volumefraction_Poly_1_tspan=25.mat')
```

```
Volume fraction Polymere 1 tspan 25 = volume fraction Rest;
load('Volumefraction Poly 0.5 tspan=25.mat')
Volume_fraction_Polymere_0_5_tspan_25 = volume_fraction_Rest;
load('Volumefraction Poly 0.1 tspan=25.mat')
Volume fraction Polymere 0 1 tspan 25 = volume fraction Rest;
load('Volumefraction Poly 0.05 tspan=25.mat')
Volume fraction Polymere 0 05 tspan 25 = volume fraction Rest;
% Load files for t span = 50
load('memRadius plot 1 tspan=50.mat')
memRadius plot 1 tspan 50 = memRadius plot;
load('memRadius plot 0.5 tspan=50.mat')
memRadius plot 0 5 tspan 50 = memRadius plot;
load('memRadius plot 0.1 tspan=50.mat')
memRadius plot 0 1 tspan 50 = memRadius plot;
load('memRadius plot 0.05 tspan=50.mat')
memRadius plot 0 05 tspan 50 = memRadius plot;
load('Volumefraction_Poly_1_tspan=50.mat')
Volume_fraction_Polymere_1_tspan_50 = volume_fraction_Rest;
load('Volumefraction_Poly_0.5_tspan=50.mat')
Volume_fraction_Polymere_0_5_tspan_50 = volume_fraction_Rest;
load('Volumefraction_Poly_0.1_tspan=50.mat')
Volume_fraction_Polymere_0_1_tspan_50 = volume_fraction_Rest;
load('Volumefraction_Poly_0.05_tspan=50.mat')
Volume_fraction_Polymere_0_05_tspan_50 = volume_fraction_Rest;
% Load files for t span = 100
load('memRadius_plot_1_tspan=100.mat')
memRadius_plot_1_tspan_100 = memRadius_plot;
load('memRadius_plot_0.5_tspan=100.mat')
memRadius_plot_0_5_tspan_100 = memRadius_plot;
load('memRadius_plot_0.1_tspan=100.mat')
memRadius_plot_0_1_tspan_100 = memRadius_plot;
load('memRadius_plot_0.05_tspan=100.mat')
memRadius_plot_0_05_tspan_100 = memRadius_plot;
load('Volumefraction Poly 1 tspan=100.mat')
Volume fraction Polymere \overline{1} \overline{1} tspan 100 = volume fraction Rest;
load('Volumefraction Poly 0.5 tspan=100.mat')
Volume fraction Polymere \overline{0} 5 tspan 100 = volume fraction Rest;
load('Volumefraction Poly 0.1 tspan=100.mat')
Volume fraction Polymere \overline{0} 1 tspan 100 = volume fraction Rest;
load('Volumefraction Poly 0.05 tspan=100.mat')
Volume fraction Polymere \overline{0} 05 tspan 100 = volume fraction Rest;
```

```
% Load files for t_span = 200
load('memRadius_plot_1_tspan=200.mat')
memRadius_plot_1_tspan_200 = memRadius_plot;
load('memRadius_plot_0.5_tspan=200.mat')
memRadius_plot_0_5_tspan_200 = memRadius_plot;
load('memRadius_plot_0.1_tspan=200.mat')
memRadius_plot_0_1_tspan_200 = memRadius_plot;
load('memRadius_plot_0.05_tspan=200.mat')
memRadius_plot_0_05_tspan_200 = memRadius_plot;
```

```
load('Volumefraction_Poly_1_tspan=200.mat')
Volume_fraction_Polymere_1_tspan_200 = volume_fraction_Rest;
```

load('Volumefraction Poly 0.5 tspan=200.mat') Volume\_fraction\_Polymere\_0\_5\_tspan\_200 = volume\_fraction\_Rest; load('Volumefraction Poly 0.1 tspan=200.mat') Volume fraction Polymere 0 1 tspan 200 = volume fraction Rest; load('Volumefraction Poly 0.05 tspan=200.mat') Volume\_fraction\_Polymere\_0\_05\_tspan\_200 = volume\_fraction\_Rest; % Define the different t spans and matrixes for the plots  $t_span_{10} = 10;$ t\_span\_25 = 25;  $t_{span_{50} = 50;}$ t\_span\_100 = 100; t span 200 = 200;radius end dt 0 05 = [memRadius plot 0 05 tspan 10(t span 10,11)\*2,memRadius plot 0 05 tspan 2 5(t span 25,11)\*2,memRadius plot 0 05 tspan 50(t span 50,11)\*2,memRadius plot 0 05 tspan 100(t span 100,11)\*2,memRadius plot 0 05 tspan 200(t span  $200,11) \times \overline{2} \times 10^{\overline{6}};$ radius end dt 0 1 = [memRadius\_plot\_0\_1\_tspan\_10(t\_span\_10,11)\*2,memRadius\_plot\_0\_1\_tspan\_25( t\_span\_25,11)\*2,memRadius\_plot\_0\_1\_tspan\_50(t\_span\_50,11)\*2,memRadius\_plo t 0 1 tspan 100(t span 100,11)\*2,memRadius plot 0 1 tspan 200(t span 200, 11)\*2]\*10^6; radius end dt 0 5 = [memRadius plot 0 5 tspan 10(t span 10,11)\*2,memRadius plot 0 5 tspan 25( t\_span\_25,11)\*2,memRadius\_plot\_0\_5\_tspan\_50(t\_span\_50,11)\*2,memRadius\_plo t\_0\_5\_tspan\_100(t\_span\_100,11)\*2,memRadius\_plot\_0\_5\_tspan\_200(t\_span\_200, 11)\*2]\*10^6; radius end dt 1 = [memRadius plot 1 tspan 10(t span 10,11)\*2,memRadius plot 1 tspan 25(t sp an 25,11) \*2, memRadius plot 1 tspan 50(t span 50,11) \*2, memRadius plot 1 ts pan 100(t span 100,11)\*2,memRadius plot 1 tspan 200(t span 200,11)\*2]\*10^ 6; radius end t span 10 = [memRadius plot 0 05 tspan 10(t span 10,11)\*2,memRadius plot 0 1 tspan 10 (t span 10,11)\*2, memRadius plot 0 5 tspan 10(t span 10,11)\*2, memRadius pl ot 1 tspan 10(t span 10,11)\*2]\*10^6; radius end t span 25 = [memRadius plot 0 05 tspan 25(t span 25,11)\*2,memRadius plot 0 1 tspan 25 (t span 25,11)\*2,memRadius plot 0 5 tspan 25(t span 25,11)\*2,memRadius pl ot 1 tspan 25(t span 25,11)\*2]\*10^6; radius end t span 50 =[memRadius plot 0 05 tspan 50(t span 50,11)\*2,memRadius plot 0 1 tspan 50 (t span 50,11)\*2,memRadius plot 0 5 tspan 50(t span 50,11)\*2,memRadius pl ot 1 tspan 50(t span 50,11)\*2]\*10^6; radius end t span  $10\overline{0}$  = [memRadius plot 0 05 tspan 100(t span 100,11)\*2, memRadius plot 0 1 tspan 100(t span 100,11)\*2,memRadius plot 0 5 tspan 100(t span 100,11)\*2,memRad ius\_plot\_1\_tspan\_100(t\_span\_100,11)\*2]\*10^6; radius end t span 200 = [memRadius plot 0 05 tspan 200(t span 200,11)\*2,memRadius plot 0 1 tspan 200(t span 200,11)\*2, memRadius plot 0 5 tspan 200(t span 200,11)\*2, memRad ius plot 1 tspan 200(t span 200,11)\*2]\*10^6; radius\_10s\_t\_span\_10 =

[memRadius plot 0 05 tspan 10(t span 10,2)\*2,memRadius plot 0 1 tspan 10(

```
t span 10,2)*2,memRadius plot 0 5 tspan 10(t span 10,2)*2,memRadius plot
1 tspan 10(t span 10,2)*2]*10^6;
radius 10s t span 25 =
[memRadius plot 0 05 tspan 25(t span 25,2)*2,memRadius plot 0 1 tspan 25(
t span 25,2)*2,memRadius plot 0 5 tspan 25(t span 25,2)*2,memRadius plot
1 tspan 25(t span 25,2)*2]*10^6;
radius 10s t span 50 =
[memRadius plot 0 05 tspan 50(t span 50,2)*2,memRadius plot 0 1 tspan 50(
t span 50,2)*2,memRadius plot 0 5 tspan 50(t span 50,2)*2,memRadius plot
1 tspan 50(t span 50,2)*2]*10^6;
radius 10s t span 100 =
[memRadius_plot_0_05_tspan_100(t_span_100,2)*2,memRadius_plot_0_1_tspan_1
00(t span 100,2)*2,memRadius plot 0 5 tspan 100(t span 100,2)*2,memRadius
_plot_1_tspan_100(t_span_100,2)*2]*10^6;
radius_10s_t_span_200 =
[memRadius plot 0 05 tspan 200(t span 200,2)*2,memRadius plot 0 1 tspan 2
00(t span 200,2)*2,memRadius plot 0 5 tspan 200(t span 200,2)*2,memRadius
plot 1 tspan 200(t span 200,2)*2]*10<sup>6</sup>;
% Define r intervall and delta t
r intervall = [t span 10,t span 25,t span 50,t span 100,t span 200]*2;
delta t = [0.05, \overline{0.1}, \overline{0.5}, 1];
×_____
% Plot the particle radius over the number of radial sections for the
% different delta t
figure(90)
plot(r_intervall, radius end dt 0 05, '-
ks', 'LineWidth',1, 'MarkerSize',17, 'MarkerFaceColor', 'k')
hold on
plot(r intervall, radius end dt 0 1, '-
gs', 'LineWidth', 1, 'MarkerSize', 12, 'MarkerFaceColor', 'g')
hold on
plot(r intervall, radius end dt 0 5, '-
rs', 'LineWidth',1, 'MarkerSize',7, 'MarkerFaceColor', 'r')
hold on
plot(r intervall, radius end dt 1, '-
bs', 'LineWidth',1, 'MarkerSize',2, 'MarkerFaceColor', 'b')
% Label and Title of the plot
title('', 'FontSize',35)
xlabel('Number of radial Sections', 'FontSize',20)
ylabel('SMD {t = 50 sec} [\mum]', 'FontSize',20)
set(gca, 'FontSize', 20)
%set(qca,'YTickLabel',{'0','0.10','0.20','0.30','0.40','0.50','0.60','0.7
0', })
% Legend
legend('\Delta t = 0.05 [sec]','\Delta t = 0.1 [sec]','\Delta t = 0.5
[sec]', '\Delta t = 1.0 [sec]', 'Location', 'NorthEast')
% Define the intervall of the axis
axis([0 410 130 150])
% Resize the plot to fullscreen
set(gcf, 'position', get(0, 'screensize'))
% Save Figure as r int radius.tiff
saveas(gcf, 'radius trend.tiff', 'tiffn');
```

```
۶_____
<u>۶</u>_____
\% Plot the particle radius over the delta t for the different numbers of
% radial sections
figure(100)
plot(delta t, radius end t span 10, '-
ks','LineWidth',1,'MarkerSize',17,'MarkerFaceColor','k')
hold on
plot(delta t, radius end t span 25, '-
gs', 'LineWidth',1, 'MarkerSize',17, 'MarkerFaceColor', 'g')
hold on
plot(delta t, radius end t span 50, '-
rs', 'LineWidth', 1, 'MarkerSize', 17, 'MarkerFaceColor', 'r')
hold on
plot(delta t, radius end t span 100, '-
bs','LineWidth',1,'MarkerSize',17,'MarkerFaceColor','b')
hold on
plot(delta t, radius end t span 200, '-
ys', 'LineWidth',1, 'MarkerSize',17, 'MarkerFaceColor', 'y')
% Label and Title of the plot
title('', 'FontSize',35)
xlabel('\Delta t', 'FontSize',20)
ylabel('SMD {t = 50 sec} [\mum]', 'FontSize',20)
set(gca, 'FontSize', 20)
% Legend
legend('Radial Sections = 20', 'Radial Sections = 50', 'Radial Sections =
100', 'Radial Sections = 200', 'Radial Sections =
400', 'Location', 'NorthEast')
% Define the intervall of the axis
axis([0.0 1.1 130 160])
% Resize the plot to fullscreen
set(gcf, 'position', get(0, 'screensize'))
% Save Figure as dt radius.tiff
saveas(gcf,'dt radius.tiff', 'tiffn');
§_____
%_____
\% Plot the particle radius after 10 seconds over the delta t for the
% different numbers of radial sections
figure(110)
plot(delta_t,radius_10s_t_span_10,'-
ks','LineWidth',1,'MarkerSize',17,'MarkerFaceColor','k')
hold on
plot(delta t, radius 10s t span 25, '-
gs','LineWidth',1,'MarkerSize',17,'MarkerFaceColor','g')
hold on
plot(delta t, radius 10s t span 50, '-
rs','LineWidth',1,'MarkerSize',17,'MarkerFaceColor','r')
hold on
plot(delta_t,radius_10s_t_span_100,'-
bs','LineWidth',1,'MarkerSize',17,'MarkerFaceColor','b')
hold on
plot(delta t, radius 10s t span 200, '-
ys', 'LineWidth',1, 'MarkerSize',17, 'MarkerFaceColor', 'y')
```

### CFL\_Analysis.m

% CFL-Analysis % (c) by Hannes Pucher 8-----% Clear, Close and delete all clc clear all close all 8-----% Load files in the workspace load('memTime\_plot.mat') % Load files for the different CFL Numbers and 260 rpm load('memRadius CFL 3 24.mat') memRadius plot  $\overline{CFL}$   $\overline{3}$   $\overline{24}$  = memRadius plot\*10^6; load('memRadius CFL 6 48.mat') memRadius\_plot\_CFL\_6\_48 = memRadius\_plot\*10^6; load('memRadius CFL 647 7.mat') memRadius plot  $\overline{CFL}$  647  $\overline{7}$  = memRadius plot\*10^6; load('memRadius CFL 6477.mat') memRadius plot  $\overline{CFL}$   $\overline{6477}$  = memRadius plot\*10^6; load('memvolumefraction \_CFL\_3\_24.mat')
Volumefraction\_Poly\_CFL\_3\_24 = volume\_fraction\_rest; load('memvolumefraction \_CFL\_6\_48.mat') Volumefraction\_Poly\_CFL\_6\_48 = volume\_fraction\_rest; load('memvolumefraction \_CFL\_647\_7.mat') Volumefraction\_Poly\_CFL\_647\_7 = volume\_fraction\_rest; load('memvolumefraction \_CFL\_6477.mat') Volumefraction\_Poly\_CFL\_6477 = volume\_fraction rest; ------§\_\_\_\_\_ % Define t span, CFL vector and SMD beginning t span 100 = 100;SMD beginning = 163.49\*10^-6; % [m] SMD of the micro-particle at the beginning t=0  $CFL_vector = [3.24; 6.48; 347.7; 6477];$ Time vector = [33.37;15.73;0.66;0.07]; <u>۶</u>\_\_\_\_\_ §\_\_\_\_\_ % Define the SMD after 1 second for different CFL numbers memRadius CFL 3 24 = memRadius plot CFL 3 24(t span 100,11)\*2; memRadius\_plot\_CFL\_3\_24\_end = memRadius\_plot\_CFL\_3\_24(t\_span\_100,11)\*2/memRadius\_CFL\_3\_24; memRadius\_plot\_CFL\_6\_48\_end = memRadius\_plot\_CFL\_6\_48(t\_span\_100,11)\*2/memRadius\_CFL\_3\_24; memRadius\_plot\_CFL\_647\_7\_end = memRadius plot CFL 647 7(t span 100,11)\*2/memRadius CFL 3 24;

```
memRadius plot CFL 6477 end =
memRadius plot CFL 6477(t span 100,2)*2/memRadius CFL 3 24;
memDeviation vector =
[memRadius_plot_CFL_3_24_end;memRadius_plot_CFL_6_48_end;memRadius_plot_C
FL 647 7 end; memRadius plot CFL 6477 end]-1;
memDeviation vector = memDeviation vector*100;
§_____
§_____
% Plot the different SMD for the different CFL numbers over time
figure(90)
plot (memTime plot, memRadius plot CFL 3 24 (t span 100,:)*2, 'q', memTime plo
t, memRadius plot CFL 6 48(t span 100,:)*2, 'b:', memTime plot, memRadius plo
t CFL 647 7(t span 100,:)*2,'r--','LineWidth',3)
% Label and Title of the plot
%title('w=0', 'FontSize',25)
xlabel('Time [s]', 'FontSize',20)
ylabel('SMD [\mum]', 'FontSize',20)
set(gca, 'FontSize', 20)
% Legend
legend('CFL = 3.24', 'CFL = 6.48', 'CFL = 647.7', 'Location', 'East')
% Define the intervall of the axis
axis([0 1 155 165])
% Resize the plot to fullscreen
set(gcf, 'position', get(0, 'screensize'))
% Save Figure as w=0.tiff
saveas(gcf,'w=260.tiff', 'tiffn');
§_____
§_____
% Compare the final micro-particle radius after 1 second for different
CFL
% numbers
figure(100)
semilogx(CFL_vector,memDeviation vector,'-
rs','LineWidth',1,'MarkerSize',17,'MarkerFaceColor','r')
% Label and Title of the plot
%title('w=0', 'FontSize',25)
xlabel('CFL Number', 'FontSize',20)
ylabel('Deviation [%]', 'FontSize',20)
set(gca, 'FontSize', 20)
% Legend
%legend('CFL = 6.48','CFL = 3.24','CFL = 647.7','w = 50','w = 100','w =
250', 'w = 500', 'Location', 'East')
% Define the intervall of the axis
%axis([0 50 0 200*10^-3])
% Resize the plot to fullscreen
set(gcf, 'position', get(0, 'screensize'))
```

```
% Save Figure as w=0.tiff
saveas(gcf,'CFL compare SMD Deviation 1sec.tiff', 'tiffn');
§_____
<u>ي</u>
% Compare the simulation time between the different cases
figure(110)
semilogx(CFL vector,Time vector,'-
bs','LineWidth',1,'MarkerSize',17,'MarkerFaceColor','b')
% Label and Title of the plot
%title('w=0', 'FontSize',25)
xlabel('CFL Number', 'FontSize',20)
ylabel('Calculation Period [min]', 'FontSize',20)
set(gca, 'FontSize', 20)
% Legend
%legend('CFL = 6.48','CFL = 3.24','CFL = 647.7','w = 50','w = 100','w =
250', 'w = 500', 'Location', 'East')
% Define the intervall of the axis
%axis([0 50 0 200*10^-3])
% Resize the plot to fullscreen
set(gcf, 'position', get(0, 'screensize'))
% Save Figure as w=0.tiff
saveas(gcf,'calculationperiod .tiff', 'tiffn');
§_____
```

### Sensivity\_Analysis

```
% Sensivity Analysis
% (c) by Hannes Pucher
        8-----
% Clear, Close and delete all
clc
clear all
close all
8-----
% Load files in the workspace
load('memTime')
% Load memRadius plot files
load('memRadius plot r3 0.mat')
memRadius plot r3 0 = memRadius_plot*10^6;
load('memRadius plot r3 2.mat')
memRadius plot r3 2 = memRadius plot*10^6;
load('memRadius plot_r3_4.mat')
memRadius plot r3 4 = memRadius plot*10^6;
load('memRadius_plot_r3_6.mat')
memRadius plot r3 6 = memRadius plot*10^6;
load('memRadius plot r3 8.mat')
memRadius plot r3 8 = memRadius plot*10^6;
load('memRadius plot r3 10.mat')
memRadius_plot_r3_10 = memRadius_plot*10^6;
load('memRadius_plot_r3_12.mat')
memRadius_plot_r3_12 = memRadius_plot*10^6;
% Load volumefraction Poly files
load('Volumefraction Poly r3 0.mat')
Volumefraction Poly r3 0 = volume fraction rest;
load('Volumefraction_Poly_r3_2.mat')
Volumefraction_Poly_r3_2 = volume_fraction rest;
load('Volumefraction_Poly_r3_4.mat')
Volumefraction_Poly_r3_4 = volume_fraction rest;
load('Volumefraction Poly r3 6.mat')
Volumefraction Poly r3 6 = volume fraction rest;
load('Volumefraction Poly r3 8.mat')
Volumefraction Poly r3 8 = volume fraction rest;
load('Volumefraction Poly r3 10.mat')
Volumefraction Poly r3 10 = volume fraction rest;
load('Volumefraction Poly r3 12.mat')
Volumefraction Poly r3 12 = volume fraction rest;
§_____
              _____
\% Define the t span and the different vectors and matrixes for the plot
t span 100 = 100;
memRadius plot r3 0 end = memRadius plot r3 0(t span 100,:);
memRadius plot r3 2 end = memRadius plot r3 2(t span 100,:);
memRadius plot r3 4 end = memRadius plot r3 4(t span 100,:);
memRadius plot r3 6 end = memRadius plot r3 6(t span 100,:);
```

```
memRadius plot r3 8 end = memRadius plot r3 8(t span 100,:);
memRadius plot r3 10 end = memRadius plot r3 10(t span 100,:);
memRadius plot r3 12 end = memRadius plot r3 12(t span 100,:);
Volumefraction Poly r3 0 second = Volumefraction Poly r3 0(:,2);
Volumefraction_Poly_r3_2_second = Volumefraction_Poly_r3_2(:,2);
Volumefraction_Poly_r3_4_second = Volumefraction_Poly_r3_4(:,2);
Volumefraction_Poly_r3_6_second = Volumefraction_Poly_r3_6(:,2);
Volumefraction_Poly_r3_8_second = Volumefraction_Poly_r3_8(:,2);
Volumefraction_Poly_r3_10_second = Volumefraction_Poly_r3_10(:,2);
Volumefraction_Poly_r3_12_second = Volumefraction_Poly_r3_12(:,2);
memRadius plot r3 0 second =
memRadius plot r3 0(:,2)/memRadius plot r3 0(t span 100,1);
memRadius plot r3 2 second =
memRadius plot r3 2(:,2)/memRadius plot r3 0(t span 100,1);
memRadius plot r3 4 second =
memRadius plot r3 4(:,2)/memRadius plot r3 0(t span 100,1);
memRadius plot r3 6 second =
memRadius plot r3 6(:,2)/memRadius plot r3 0(t span 100,1);
memRadius plot r3 8 second =
memRadius plot r3 8(:,2)/memRadius plot r3 0(t span 100,1);
memRadius plot r3 10 second =
memRadius_plot_r3_10(:,2)/memRadius_plot_r3_0(t_span_100,1);
memRadius plot r3 12 second =
memRadius plot r3 12(:,2)/memRadius plot r3 0(t span 100,1);
§_____
% Plot the particle radius over time for the different r 3 values
figure(90)
plot(memTime,memRadius plot r3 0 end*2,'k','LineWidth',3)
hold on
plot(memTime,memRadius plot r3 2 end*2,'g--','LineWidth',3)
hold on
plot(memTime,memRadius plot r3 4 end*2,'r','LineWidth',3)
hold on
plot(memTime,memRadius plot r3 6 end*2,'y--','LineWidth',3)
hold on
plot(memTime,memRadius plot r3 8 end*2,'b','LineWidth',3)
hold on
plot(memTime,memRadius plot r3 10 end*2,'c--','LineWidth',3)
hold on
plot(memTime,memRadius plot r3 12 end*2,'m','LineWidth',3)
% Label and Title of the plot
title('', 'FontSize',35)
xlabel('Time [s]', 'FontSize',20)
ylabel('SMD [\mum]', 'FontSize',20)
set(gca, 'FontSize', 20)
% Legend
legend('r {3}=0', 'r {3}=2', 'r {3}=4', 'r {3}=6', 'r {3}=8', 'r {3}=10', 'r {
}=12', 'Location', 'EastOutside')
% Define the intervall of the axis
axis([0 10 80 180])
% Resize the plot to fullscreen
set(gcf,'position',get(0,'screensize'))
```

```
% Save Figure as r 3 radius compare.tiff
saveas(gcf,'r 3 radius compare.tiff', 'tiffn');
§_____
                                   _____
                                                       _ _ _ _ _ _ _ _ _ _ _ _ _ _ _ _ _ _
§_____
% Plot the volumen fraction for 1 sec over the radius for the different
r 3 values
figure(100)
plot (memRadius plot r3 0 second, Volumefraction Poly r3 0 second, 'k', 'Line
Width',3)
hold on
plot (memRadius plot r3 2 second, Volumefraction Poly r3 2 second, 'q--
', 'LineWidth', 3)
hold on
plot (memRadius plot r3 4 second, Volumefraction Poly r3 4 second, 'r', 'Line
Width',3)
hold on
plot (memRadius plot r3 6 second, Volumefraction Poly r3 6 second, 'y--
', 'LineWidth', 3)
hold on
plot (memRadius plot r3 8 second, Volumefraction Poly r3 8 second, 'b', 'Line
Width',3)
hold on
plot (memRadius plot r3 10 second, Volumefraction Poly r3 10 second, 'c--
', 'LineWidth', 3)
hold on
plot(memRadius plot r3 12 second, Volumefraction Poly r3 12 second, 'm', 'Li
neWidth',3)
% Label and Title of the plot
title('', 'FontSize',35)
xlabel('Normalized Radius', 'FontSize',20)
ylabel('\phi {Remaining Components}', 'FontSize',20)
set(gca, 'FontSize', 20)
% Legend
legend('r_{3}=0', 'r_{3}=2', 'r_{3}=4', 'r_{3}=6', 'r_{3}=8', 'r_{3}=10', 'r_{
}=12', 'Location', 'EastOutside')
% Define the intervall of the axis
%axis([0 1 0.8000000*10^-4 1.80000000*10^-4])
% Resize the plot to fullscreen
set(gcf, 'position', get(0, 'screensize'))
% Save Figure as r_3_volume_compare.tiff
saveas(gcf,'r_3_volume_compare.tiff', 'tiffn');
```

```
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```

# **IV. Experimental Validation**

Experimental\_Validation\_1h.m

```
% Experimental Validation 1 hour
% (c) by Hannes Pucher
§_____
8-----
% Clear, Close and delete all
clc
clear all
close all
§_____
§_____
% Load files in the workspace
% Load memRadius plot files
load('memRadius plot r3 7 end.mat')
memRadius plot r3 7 = memRadius end*10^6;
load('memRadius plot r3 9 end.mat')
memRadius plot r3 9 = memRadius end*10^6;
load('memRadius plot r3 11 end.mat')
memRadius plot r3 11 = memRadius end*10^6;
8_____
              _____
% Define the memTime plot vector for the plot
memTime plot = linspace(0,3601,3601);
      _____
§____
8-----
% Data from 12/16.08.2010
QICPIC data 1 = [163.49 115 111.675 105.03 99.5 105 96.25 99.985
92.596 100.165]; % [?m] SMD measured with QICPIC
              = [0 12 50 85 145 205 265 270 315 1170]; % [min]
QICPIC time 1
QICPIC time
QICPIC time 1 plot = QICPIC time 1 * 60; % [sec] QICPIC time
            = [163.49 116 96 110 96.66 104 106.01 107]; % [?m] SMD
HELOS data 1
measured with HELOS
HELOS_time_1 = [0 50 85 225 265 270 315 1170]; % [sec] HELOS time
HELOS_time_1_plot = HELOS_time_1 * 60; % [sec] HELOS time
§_____
% Save all variables
save Experimental Parameters.mat
§_____
8-----
% Plot Radius vs Time
figure(1)
plot(QICPIC time 1 plot/3600,QICPIC data 1, 'bd', 'MarkerSize', 17, 'MarkerFa
ceColor', 'b')
hold on
```

```
plot(HELOS time 1 plot/3600, HELOS data 1, 'gs', 'MarkerSize', 17, 'MarkerFace
Color', 'g')
hold on
plot(memTime plot/3600,memRadius plot r3 7*2,'k','LineWidth',2)
hold on
plot(memTime plot/3600,memRadius plot r3 9*2,'r--','LineWidth',2)
hold on
plot(memTime plot/3600,memRadius plot r3 11*2,'b:','LineWidth',2)
%hold on
%plot(memTime plot/3600,memRadius plot r3 13*2,'b:','LineWidth',2)
% Label and Title of the plot
title('', 'FontSize',35)
xlabel('Time [h]', 'FontSize',20)
ylabel('SMD [\mum]', 'FontSize',20)
set(gca, 'FontSize', 20)
% Legend
legend('QICPIC', 'HELOS', 'r {2} = 6.25, r {3} = 6.75', 'r {2} = 6.00, r {3}
= 9.00', 'r {2} = 5.75, r {3} = 11.25', 'Location', 'NorthEast')
% Define the intervall of the axis
axis([0 1 80 180])
% Resize the plot to fullscreen
set(gcf, 'position', get(0, 'screensize'))
% Save Figure as SMD.tiff
saveas(gcf,'SMD_new.tiff', 'tiffn');
8____
```

# Experimental\_Validation\_5h.m

```
% Experimental Validation 5 hour
% (c) by Hannes Pucher
§_____
8-----
% Clear, Close and delete all
clc
clear all
close all
8-----
۶_____
% Load files in the workspace
% Load memRadius plot files
load('memRadius plot r3 7 end.mat')
memRadius plot r3 7 = memRadius end*10^6;
load('memRadius plot r3 9 end.mat')
memRadius_plot_r3 9 = memRadius end*10^6;
load('memRadius plot r3 11 end.mat')
memRadius plot r3 11 = memRadius end*10^6;
8-----
% Define the memTime plot vector for the plot
memTime plot = linspace(0,18001,18001);
2----
       8-----
% Data from 12/16.08.2010
QICPIC data 1 = [163.49 115 111.675 105.03 99.5 105 96.25 99.985
92.596 100.165]; % [m] SMD measured with QICPIC
QICPIC time 1 = [0 12 50 85 145 205 265 270 315 1170]; % [min]
QICPIC time
QICPIC time 1 plot = QICPIC time 1 * 60; % [sec] QICPIC time
           = [163.49 116 96 110 96.66 104 106.01 107]; % [m] SMD
HELOS data 1
measured with HELOS
HELOS_time_1 = [0 50 85 225 265 270 315 1170]; % [sec] HELOS time
HELOS time 1 plot = HELOS time 1 * 60; % [sec] HELOS time
§_____
§_____
% Save all variables
save Experimental_Parameters.mat
§_____
8-----
% Plot Radius vs Time
figure(1)
plot(QICPIC time 1 plot/3600,QICPIC data 1, 'bd', 'MarkerSize', 17, 'MarkerFa
ceColor', 'b')
hold on
plot(HELOS time 1 plot/3600, HELOS data 1, 'gs', 'MarkerSize', 17, 'MarkerFace
Color', 'g')
hold on
plot (memTime plot/3600, memRadius plot r3 7*2, 'k', 'LineWidth', 2)
```

```
hold on
plot(memTime plot/3600,memRadius plot r3 9*2,'r--','LineWidth',2)
hold on
plot(memTime_plot/3600,memRadius_plot_r3_11*2,'b:','LineWidth',2)
% Label and Title of the plot
title('', 'FontSize',35)
xlabel('Time [h]', 'FontSize',20)
ylabel('SMD [\mum]', 'FontSize',20)
set(gca, 'FontSize', 20)
% Legend
legend('QICPIC', 'HELOS', 'r {2} = 6.25, r {3} = 6.75', 'r {2} = 6.00, r {3}
= 9.00', 'r {2} = 5.75, r {3} = 11.25', 'Location', 'NorthEast')
% Define the intervall of the axis
axis([0 5 80 180])
% Resize the plot to fullscreen
set(gcf, 'position',get(0, 'screensize'))
% Save Figure as SMD.tiff
saveas(gcf,'SMD_new.tiff', 'tiffn');
§_____
```

### Experimental\_Validaiton\_20h.m

```
% Experimental Validation 20 hour
% (c) by Hannes Pucher
§_____
8-----
% Clear, Close and delete all
clc
clear all
close all
8-----
۶_____
% Load files in the workspace
% Load memRadius plot files
load('memRadius plot r3 7 end.mat')
memRadius plot r3 7 = memRadius end*10^6;
load('memRadius plot r3 9 end.mat')
memRadius_plot_r3 9 = memRadius end*10^6;
load('memRadius plot r3 11 end.mat')
memRadius plot r3 11 = memRadius end*10^6;
8-----
% Define the memTime plot vector for the plot
memTime plot = linspace(0,72001,72001);
2----
       8-----
% Data from 12/16.08.2010
QICPIC data 1 = [163.49 115 111.675 105.03 99.5 105 96.25 99.985
92.596 100.165]; % [m] SMD measured with QICPIC
QICPIC time 1 = [0 12 50 85 145 205 265 270 315 1170]; % [min]
QICPIC time
QICPIC time 1 plot = QICPIC time 1 * 60; % [sec] QICPIC time
           = [163.49 116 96 110 96.66 104 106.01 107]; % [m] SMD
HELOS data 1
measured with HELOS
HELOS time 1 = [0 50 85 225 265 270 315 1170]; % [sec] HELOS time
HELOS time 1 plot = HELOS time 1 * 60; % [sec] HELOS time
§_____
§_____
% Save all variables
save Experimental_Parameters.mat
§_____
8-----
% Plot Radius vs Time
figure(1)
plot(QICPIC time 1 plot/3600,QICPIC data 1, 'bd', 'MarkerSize', 17, 'MarkerFa
ceColor', 'b')
hold on
plot(HELOS time 1 plot/3600, HELOS data 1, 'gs', 'MarkerSize', 17, 'MarkerFace
Color', 'g')
hold on
plot (memTime plot/3600, memRadius plot r3 7*2, 'k', 'LineWidth', 2)
```

```
hold on
plot(memTime plot/3600,memRadius plot r3 9*2,'r--','LineWidth',2)
hold on
plot(memTime_plot/3600,memRadius_plot_r3_11*2,'b:','LineWidth',2)
% Label and Title of the plot
title('', 'FontSize',35)
xlabel('Time [h]', 'FontSize',20)
ylabel('SMD [\mum]', 'FontSize',20)
set(gca, 'FontSize', 20)
% Legend
legend('QICPIC', 'HELOS', 'r {2} = 6.25, r {3} = 6.75', 'r {2} = 6.00, r {3}
= 9.00', 'r {2} = 5.75, r {3} = 11.25', 'Location', 'NorthEast')
% Define the intervall of the axis
axis([0 20 80 180])
% Resize the plot to fullscreen
set(gcf, 'position',get(0, 'screensize'))
% Save Figure as SMD.tiff
saveas(gcf,'SMD_new.tiff', 'tiffn');
§_____
```

### Volume\_fraction\_EA\_Comparison.m

```
% Volume fraction EA Comparison
% (c) by Hannes Pucher
        _____
                        _____
8-----
% Clear, Close and delete all
clc
clear all
close all
१_____
% Load files in the workspace
% r3=6.75
% Load memVolumefraction EA plot files
load('memVolumefraction EA plot 1h 6 75.mat')
memVolumefraction EA 0h 6 75 = memVolumefraction_EA_plot(:,1);
load('memVolumefraction EA plot 1h 6 75.mat')
memVolumefraction EA 1h 6 75 = memVolumefraction EA plot(:,11);
load('memVolumefraction EA plot 5h 6 75.mat')
memVolumefraction EA 5h 6 75 = memVolumefraction EA plot(:,11);
load('memVolumefraction EA plot 20h 6 75.mat')
memVolumefraction EA 20h 6 75 = memVolumefraction EA plot(:,11);
% Load memRadius_plot_normalized files
load('memRadius_plot_normalized_1h_6_75.mat')
memRadius_plot_normalized_0h_6_75 = memRadius_plot_normalized(:,1);
load('memRadius_plot_normalized_1h_6_75.mat')
memRadius_plot_normalized_1h_6_75 = memRadius_plot_normalized(:,11);
load('memRadius plot normalized 5h 6 75.mat')
memRadius_plot_normalized_5h_6_75 = memRadius_plot_normalized(:,11);
load('memRadius_plot_normalized_20h_6_75.mat')
memRadius_plot_normalized_20h_6_75 = memRadius_plot_normalized(:,11);
<u>_____</u>
§_____
% r3=9.00
% Load memVolumefraction EA plot files
load('memVolumefraction EA plot 1h 9 00.mat')
memVolumefraction EA 0h 9 00 = memVolumefraction EA plot(:,1);
load('memVolumefraction EA plot 1h 9 00.mat')
memVolumefraction EA 1h 9 00 = memVolumefraction EA plot(:,11);
load('memVolumefraction EA plot 5h 9 00.mat')
memVolumefraction_EA_5h_9_00 = memVolumefraction_EA_plot(:,11);
load('memVolumefraction_EA_plot_20h_9_00.mat')
memVolumefraction EA 20h 9 00 = memVolumefraction EA plot(:,11);
% Load memRadius plot normalized files
load('memRadius plot normalized 1h 9 00.mat')
memRadius plot normalized 0h 9 00 = memRadius plot normalized(:,1);
load('memRadius plot normalized 1h 9 00.mat')
memRadius plot normalized 1h 9 00 = memRadius_plot_normalized(:,11);
load('memRadius plot normalized 5h 9 00.mat')
memRadius plot normalized 5h 9 00 = memRadius plot normalized(:,11);
load('memRadius plot normalized 20h 9 00.mat')
```

```
memRadius plot normalized 20h 9 00 = memRadius plot normalized(:,11);
<u>۶_____</u>
% r3=11.25
% Load memVolumefraction EA plot files
load('memVolumefraction_EA_plot_1h_11_25.mat')
memVolumefraction EA 0h 11 25 = memVolumefraction EA plot(:,1);
load('memVolumefraction_EA_plot_1h_11_25.mat')
memVolumefraction EA 1h 11 25 = memVolumefraction EA plot(:,11);
load('memVolumefraction_EA_plot_5h_11_25.mat')
memVolumefraction_EA_5h_11_25 = memVolumefraction_EA_plot(:,11);
load('memVolumefraction_EA_plot_20h_11_25.mat')
memVolumefraction EA 20h 11 25 = memVolumefraction EA plot(:,11);
% Load memRadius plot normalized files
load('memRadius plot normalized 1h 11 25.mat')
memRadius plot normalized 0h 11 25 = memRadius plot normalized(:,1);
load('memRadius plot normalized 1h 11 25.mat')
memRadius plot normalized 1h 11 25 = memRadius plot normalized(:,11);
load('memRadius plot normalized 5h 11 25.mat')
memRadius plot normalized 5h 11 25 = memRadius plot normalized(:,11);
load('memRadius_plot normalized_20h 11 25.mat')
memRadius_plot_normalized_20h_11_25 = memRadius_plot_normalized(:,11);
§_____
% Save all variables
save Experimental Parameters.mat
§_____
% Plot Radius vs Volume fraction
figure(32)
plot(memRadius plot normalized 0h 6 75, memVolumefraction EA 0h 6 75', 'k-
o', 'LineWidth', 1)
hold on
plot(memRadius_plot_normalized_1h_6_75,memVolumefraction_EA_1h_6_75','b-
o', 'LineWidth',1)
hold on
plot(memRadius plot normalized 5h 6 75, memVolumefraction EA 5h 6 75', 'r-
o', 'LineWidth', 1)
hold on
plot(memRadius plot normalized 20h 6 75, memVolumefraction EA 20h 6 75', 'm
-o', 'LineWidth',1)
hold on
plot(memRadius plot normalized 0h 9 00, memVolumefraction EA 0h 9 00', 'k-
s','LineWidth',1)
hold on
plot (memRadius plot normalized 1h 9 00, memVolumefraction EA 1h 9 00', 'b-
s','LineWidth',1)
hold on
plot(memRadius plot normalized 5h 9 00, memVolumefraction EA 5h 9 00', 'r-
s','LineWidth',1)
hold on
plot(memRadius plot normalized 20h 9 00,memVolumefraction EA 20h 9 00','m
-s','LineWidth',1)
hold on
```
```
plot(memRadius plot normalized 0h 11 25, memVolumefraction EA 0h 11 25', 'k
 -^', 'LineWidth', 1)
hold on
plot(memRadius plot normalized 1h 11 25, memVolumefraction EA 1h 11 25', 'b
 -^', 'LineWidth', 1)
hold on
plot (memRadius plot normalized 5h 11 25, memVolumefraction EA 5h 11 25', 'r
 -^', 'LineWidth',1)
hold on
plot(memRadius plot normalized 20h 11 25, memVolumefraction EA 20h 11 25',
 'm-^', 'LineWidth',1)
 % Label and Title of the plot
 title('', 'FontSize',35)
 % Normalized Radial Positions
xlabel('Normalized Radius', 'FontSize',20)
ylabel('\phi_{Ethyl acetate}', 'FontSize',20)
 set(gca, 'FontSize', 20)
 set(gca,'YTickLabel',{'0','0.10','0.20','0.30','0.40','0.50','0.60','0.70
 ',})
 % Legend
legend('t = 0 h, r_{3} = 6,75', t = 1 h, r_{3} = 6,75', t = 5 h,

r_{3} = 6,75', t = 20 h, r_{3} = 6,75', t = 0 h, r_{3} = 9,00', t = 1 h, r_{3} = 9,00', t = 5 h, r_{3} = 9,00', t = 20 h, r_{3} = 9,00', t = 5 h, r_{3} = 9,00', t = 20 h, r_{3} = 9,00', t = 1 h, r_{3} = 11,25', t = 1 h, r_{3} = 11,25', t = 5 h, r_{3} = 11,25', t = 1 h, r_{3} = 11,25', t = 5 h, r_{3} = 11,25', t = 1 h, r_{3} = 
11,25','t = 20 h, r_{3} = 11,25','Location','EastOutside')
 % Define the intervall of the axis
axis([0 1 0.0 0.7])
 % Resize the plot to fullscreen
 set(gcf, 'position', get(0, 'screensize'))
 % Save Figure as Volumefraction EA.tiff
 %saveas(gcf, 'Volumefraction EA.tiff', 'tiffn');
 2____
```

## Volume\_fraction\_BA\_Comparison.m

```
% Volume fraction BA Comparison
% (c) by Hannes Pucher
        _____
                        _____
8-----
% Clear, Close and delete all
clc
clear all
close all
१_____
% Load files in the workspace
% r3=6.75
% Load memVolumefraction BA plot files
load('memVolumefraction BA plot 1h 6 75.mat')
memVolumefraction BA 0h 6 75 = memVolumefraction_BA_plot(:,1);
load('memVolumefraction BA plot 1h 6 75.mat')
memVolumefraction BA 1h 6 75 = memVolumefraction BA plot(:,11);
load('memVolumefraction BA plot 5h 6 75.mat')
memVolumefraction BA 5h 6 75 = memVolumefraction BA plot(:,11);
load('memVolumefraction BA plot 20h 6 75.mat')
memVolumefraction BA 20h 6 75 = memVolumefraction BA plot(:,11);
% Load memRadius_plot_normalized files
load('memRadius_plot_normalized_1h_6_75.mat')
memRadius_plot_normalized_0h_6_75 = memRadius_plot_normalized(:,1);
load('memRadius_plot_normalized_1h_6_75.mat')
memRadius_plot_normalized_1h_6_75 = memRadius_plot_normalized(:,11);
load('memRadius plot normalized 5h 6 75.mat')
memRadius_plot_normalized_5h_6_75 = memRadius_plot_normalized(:,11);
load('memRadius_plot_normalized_20h_6_75.mat')
memRadius_plot_normalized_20h_6_75 = memRadius_plot_normalized(:,11);
<u>&_____</u>
§_____
% r3=9.00
% Load memVolumefraction BA plot files
load('memVolumefraction BA plot 1h 9 00.mat')
memVolumefraction BA 0h 9 00 = memVolumefraction BA plot(:,1);
load('memVolumefraction BA plot 1h 9 00.mat')
memVolumefraction BA 1h 9 00 = memVolumefraction BA plot(:,11);
load('memVolumefraction BA plot 5h 9 00.mat')
memVolumefraction_BA_5h_9_00 = memVolumefraction_BA_plot(:,11);
load('memVolumefraction_BA_plot_20h_9_00.mat')
memVolumefraction BA 20h 9 00 = memVolumefraction BA plot(:,11);
% Load memRadius plot normalized files
load('memRadius plot normalized 1h 9 00.mat')
memRadius plot normalized 0h 9 00 = memRadius plot normalized(:,1);
load('memRadius plot normalized 1h 9 00.mat')
memRadius plot normalized 1h 9 00 = memRadius_plot_normalized(:,11);
load('memRadius plot normalized 5h 9 00.mat')
memRadius plot normalized 5h 9 00 = memRadius plot normalized(:,11);
load('memRadius plot normalized 20h 9 00.mat')
```

```
memRadius plot normalized 20h 9 00 = memRadius plot normalized(:,11);
<u>۶_____</u>
% r3=11.25
% Load memVolumefraction BA plot files
load('memVolumefraction_BA_plot_1h_11_25.mat')
memVolumefraction BA 0h 11 25 = memVolumefraction BA plot(:,1);
load('memVolumefraction_BA_plot_1h_11_25.mat')
memVolumefraction BA 1h 11 25 = memVolumefraction BA plot(:,11);
load('memVolumefraction_BA_plot_5h_11_25.mat')
memVolumefraction_BA_5h_11_25 = memVolumefraction_BA_plot(:,11);
load('memVolumefraction_BA_plot_20h_11_25.mat')
memVolumefraction_BA_20h 11 25 = memVolumefraction BA plot(:,11);
% Load memRadius plot normalized files
load('memRadius plot normalized 1h 11 25.mat')
memRadius plot normalized 0h 11 25 = memRadius plot normalized(:,1);
load('memRadius plot normalized 1h 11 25.mat')
memRadius plot normalized 1h 11 25 = memRadius plot normalized(:,11);
load('memRadius plot normalized 5h 11 25.mat')
memRadius plot normalized 5h 11 25 = memRadius plot normalized(:,11);
load('memRadius_plot normalized_20h 11 25.mat')
memRadius_plot_normalized_20h_11_25 = memRadius_plot_normalized(:,11);
§_____
% Save all variables
save Experimental Parameters.mat
§_____
% Plot Radius vs Volume fraction
figure(33)
plot(memRadius plot normalized 0h 6 75, memVolumefraction BA 0h 6 75', 'k-
o', 'LineWidth', 1)
hold on
plot(memRadius_plot_normalized_1h_6_75,memVolumefraction_BA_1h_6_75','b-
o', 'LineWidth',1)
hold on
plot(memRadius plot normalized 5h 6 75, memVolumefraction BA 5h 6 75', 'r-
o', 'LineWidth', 1)
hold on
plot(memRadius plot normalized 20h 6 75, memVolumefraction BA 20h 6 75', 'm
-o', 'LineWidth',1)
hold on
plot(memRadius plot normalized 0h 9 00, memVolumefraction BA 0h 9 00', 'k-
s','LineWidth',1)
hold on
plot (memRadius plot normalized 1h 9 00, memVolumefraction BA 1h 9 00', 'b-
s','LineWidth',1)
hold on
plot(memRadius plot normalized 5h 9 00, memVolumefraction BA 5h 9 00', 'r-
s','LineWidth',1)
hold on
plot(memRadius plot normalized 20h 9 00,memVolumefraction BA 20h 9 00','m
-s','LineWidth',1)
hold on
```

```
plot(memRadius plot normalized 0h 11 25, memVolumefraction BA 0h 11 25', 'k
 -^', 'LineWidth', 1)
hold on
plot(memRadius plot normalized 1h 11 25, memVolumefraction BA 1h 11 25', 'b
 -^', 'LineWidth', 1)
hold on
plot (memRadius plot normalized 5h 11 25, memVolumefraction BA 5h 11 25', 'r
 -^', 'LineWidth',1)
hold on
plot(memRadius plot normalized 20h 11 25, memVolumefraction BA 20h 11 25',
 'm-^', 'LineWidth',1)
 % Label and Title of the plot
 title('', 'FontSize',35)
 % Normalized Radial Positions
xlabel('Normalized Radius', 'FontSize',20)
ylabel('\phi {Benzyl alcohol}', 'FontSize',20)
 set(gca, 'FontSize', 20)
 set(gca, 'YTickLabel', {'0', '0.05', '0.10', '0.15', '0.20', '0.25'})
 % Legend
legend ('t = 0 h, r_{3} = 6,75', t = 1 h, r_{3} = 6,75', t = 5 h,

r_{3} = 6,75', t = 20 h, r_{3} = 6,75', t = 0 h, r_{3} = 9,00', t = 1 h, r_{3} = 9,00', t = 5 h, r_{3} = 9,00', t = 20 h, r_{3} = 9,00', t = 20 h, r_{3} = 9,00', t = 20 h, r_{3} = 9,00', t = 1 h, r_{3} = 11,25', t = 1 h, r_{3} = 11,25', t = 5 h, r_{3} = 11,25', t = 1 h, r_{3} = 11,25', t = 5 h, r_{3} = 11,25', t = 1 h, r_{3} = 11,25', t = 5 h, r_{3} = 11,25', t = 1 h, r_{3} 
11,25','t = 20 h, r {3} = 11,25', 'Location', 'EastOutside')
 % Define the intervall of the axis
axis([0 1 0 0.25])
 % Resize the plot to fullscreen
 set(gcf, 'position', get(0, 'screensize'))
 % Save Figure as Volumefraction BA.tiff
 %saveas(gcf,'Volumefraction BA.tiff', 'tiffn');
 e_____
```

## Volume\_fraction\_RC\_Comparison.m

```
% Volume fraction RC Comparison
% (c) by Hannes Pucher
         _____
                         _____
8-----
% Clear, Close and delete all
clc
clear all
close all
१_____
% Load files in the workspace
% r3=6.75
% Load memVolumefraction RC plot files
load('memVolumefraction RC plot 1h 6 75.mat')
memVolumefraction RC 0h 6 75 = volume fraction rest(:,1);
load('memVolumefraction RC plot 1h 6 75.mat')
memVolumefraction RC 1h 6 75 = volume fraction rest(:,11);
load('memVolumefraction RC plot 5h 6 75.mat')
memVolumefraction RC 5h_6_75 = volume_fraction_rest(:,11);
load('memVolumefraction RC plot 20h 6 75.mat')
memVolumefraction RC 20h 6 75 = volume fraction rest(:,11);
% Load memRadius_plot_normalized files
load('memRadius_plot_normalized_1h_6_75.mat')
memRadius_plot_normalized_0h_6_75 = memRadius_plot_normalized(:,1);
load('memRadius_plot_normalized_1h_6_75.mat')
memRadius_plot_normalized_1h_6_75 = memRadius_plot_normalized(:,11);
load('memRadius plot normalized 5h 6 75.mat')
memRadius plot normalized 5h 6 75 = memRadius plot normalized(:,11);
load('memRadius_plot_normalized_20h_6_75.mat')
memRadius plot normalized_20h_6_75 = memRadius_plot_normalized(:,11);
§_____
§_____
% r3=9.00
% Load volume fraction RC files
load('memVolumefraction RC plot 1h 9 00.mat')
memVolumefraction RC 0h 9 00 = volume fraction rest(:,1);
load('memVolumefraction_RC_plot_1h_9_00.mat')
memVolumefraction RC 1h 9 00 = volume fraction rest(:,11);
load('memVolumefraction RC plot 5h 9 00.mat')
memVolumefraction_RC_5h_9_00 = volume_fraction_rest(:,11);
load('memVolumefraction_RC_plot_20h_9_00.mat')
memVolumefraction_RC_20h_9_00 = volume_fraction_rest(:,11);
% Load memRadius plot normalized files
load('memRadius plot normalized 1h 9 00.mat')
memRadius plot normalized 0h 9 00 = memRadius plot normalized(:,1);
load('memRadius plot normalized 1h 9 00.mat')
memRadius plot normalized 1h 9 00 = memRadius_plot_normalized(:,11);
load('memRadius plot normalized 5h 9 00.mat')
memRadius plot normalized 5h 9 00 = memRadius plot normalized(:,11);
load('memRadius plot normalized 20h 9 00.mat')
```

```
memRadius plot normalized 20h 9 00 = memRadius plot normalized(:,11);
<u>۶_____</u>
% r3=11.25
% Load volume fraction RC files
load('memVolumefraction_RC_plot_1h_11_25.mat')
memVolumefraction_RC_0h_11_25 = volume_fraction_Rest(:,1);
load('memVolumefraction_RC_plot_1h_11_25.mat')
memVolumefraction_RC_1h_11_25 = volume_fraction_Rest(:,11);
load('memVolumefraction_RC_plot_5h_11_25.mat')
memVolumefraction_RC_5h_11_25 = volume_fraction_rest(:,11);
load('memVolumefraction_RC_plot_20h_11_25.mat')
memVolumefraction RC 20h 11 25 = volume fraction rest(:,11);
% Load memRadius plot normalized files
load('memRadius plot normalized 1h 11 25.mat')
memRadius plot normalized 0h 11 25 = memRadius plot normalized(:,1);
load('memRadius plot normalized 1h 11 25.mat')
memRadius plot normalized 1h 11 25 = memRadius plot normalized(:,11);
load('memRadius plot normalized 5h 11 25.mat')
memRadius plot normalized 5h 11 25 = memRadius plot normalized(:,11);
load('memRadius_plot normalized_20h 11 25.mat')
memRadius_plot_normalized_20h_11_25 = memRadius_plot_normalized(:,11);
8-----
% Save all variables
%save Experimental Parameters.mat
8-----
% Plot Radius vs Volume fraction
figure(33)
plot(memRadius plot normalized 0h 6 75, memVolumefraction RC 0h 6 75', 'k-
o', 'LineWidth', 1)
hold on
plot(memRadius_plot_normalized_1h_6_75,memVolumefraction_RC_1h_6_75','b-
o', 'LineWidth',1)
hold on
plot(memRadius plot normalized 5h 6 75, memVolumefraction RC 5h 6 75', 'r-
o', 'LineWidth', 1)
hold on
plot(memRadius plot normalized 20h 6 75, memVolumefraction RC 20h 6 75', 'm
-o', 'LineWidth', 1)
hold on
plot(memRadius plot normalized 0h 9 00, memVolumefraction RC 0h 9 00', 'k-
s','LineWidth',1)
hold on
plot (memRadius plot normalized 1h 9 00, memVolumefraction RC 1h 9 00', 'b-
s','LineWidth',1)
hold on
plot(memRadius plot normalized 5h 9 00, memVolumefraction RC 5h 9 00', 'r-
s','LineWidth',1)
hold on
plot(memRadius plot normalized 20h 9 00,memVolumefraction RC 20h 9 00','m
-s','LineWidth',1)
hold on
```

```
plot(memRadius plot normalized 0h 11 25, memVolumefraction RC 0h 11 25', 'k
-^', 'LineWidth', 1)
hold on
plot(memRadius plot normalized 1h 11 25, memVolumefraction RC 1h 11 25', 'b
-^','LineWidth',1)
hold on
plot (memRadius plot normalized 5h 11 25, memVolumefraction RC 5h 11 25', 'r
-^', 'LineWidth',1)
hold on
plot(memRadius plot normalized 20h 11 25, memVolumefraction RC 20h 11 25',
'm-^', 'LineWidth',1)
% Label and Title of the plot
title('', 'FontSize',35)
% Normalized Radial Positions
xlabel('Normalized Radius', 'FontSize',20)
ylabel('\phi {Remaining Components}', 'FontSize',20)
set(gca, 'FontSize', 20)
set(gca,'YTickLabel',{'0','0.10','0.20','0.30','0.40','0.50','0.60','0.70
','0.80','0.90','1.00'})
% Legend
legend('t = 0 h, r_{3} = 6,75','t = 1 h, r_{3} = 6,75','t = 5 h,
r_{3} = 6,75', t = 20 h, r_{3} = 6,75', t = 0 h, r_{3} = 9,00', t = 1 h, r_{3} = 9,00', t = 1 h, r_{3} = 9,00', t = 5 h, r_{3} = 9,00', t = 20 h, r_{3} = 9,00', t = 20 h, r_{3} = 9,00', t = 1 h, r_{3} = 11,25', t = 1 h, r_{3} = 11,25', t = 5 h,
11,25','t = 20 h, r {3} = 11,25', 'Location', 'EastOutside')
% Define the intervall of the axis
axis([0 1 0 1])
% Resize the plot to fullscreen
%set(gcf, 'position', get(0, 'screensize'))
% Save Figure as Volumefraction RC.tiff
% saveas(gcf,'Volumefraction RC.tiff', 'tiffn');
§_____
<u>۶</u>_____
% Diffusion Coefficient
volume f initial API = 0.0412;
% System depending Components
r BA 1 = 1.6916;
r EA 1 = 1.7496;
% r3 = 6.75
r_BA_2_6 = 6.2479;
r_{BA_3_6} = 6.7521;
Diffusion_{BA_6_0h} = r_{BA_1*10.^(-r_{BA_2_6} - r_{BA_2_6})
(memVolumefraction_RC_0h_11_25-volume_f_initial_API).*r_BA_3_6);
Diffusion_{BA_6_1h} = r_{BA_1*10.^(-r_{BA_2_6} - r_{BA_2})
(memVolumefraction RC 1h 11 25-volume f initial API).*r BA 3 6);
```

Diffusion BA 6 5h = r BA 1\*10.^ (-r BA 2 6 -(memVolumefraction RC 5h 11 25-volume f initial API).\*r BA 3 6); Diffusion BA 6 20h = r BA 1\*10.^ (-r BA 2 6 -(memVolumefraction RC 20h 11 25-volume f initial API).\*r BA 3 6); r EA 2 6 = 6.2479;r EA 3 6 = 6.7521;Diffusion EA 6 0h = r EA  $1*10.^{-1}$  (-r EA 2 6 -(memVolumefraction RC 0h 11 25-volume f initial API).\*r EA 3 6); Diffusion EA 6 1h = r EA 1\*10.^ (-r EA 2 6 -(memVolumefraction RC 1h 11 25-volume f initial API).\*r EA 3 6); Diffusion EA 6 5h = r EA  $1*10.^{-1}$  (-r EA 2 6 -(memVolumefraction\_RC\_5h\_11\_25-volume\_f\_initial\_API).\*r\_EA\_3\_6); Diffusion\_EA\_6\_20h =  $r_EA_1 \times 10.^{(-r_EA_2 - 6)}$ (memVolumefraction\_RC\_20h\_11\_25-volume\_f\_initial\_API).\*r\_EA\_3\_6); % r3 = 9.00  $r_BA_2_9 = 5.9972;$ r BA 3 9 = 9.0028; Diffusion BA 9 Oh = r BA  $1*10.^{-1}$  (-r BA 2 9 -(memVolumefraction\_RC\_0h\_11\_25-volume\_f\_initial\_API).\*r\_BA\_3\_9); Diffusion\_BA\_9\_1h = r\_BA\_1\*10.^(-r\_BA\_2\_9 -(memVolumefraction\_RC\_1h\_11\_25-volume\_f\_initial\_API).\*r\_BA\_3\_9); Diffusion\_BA\_9\_5h = r\_BA\_1\*10.^(-r\_BA\_2\_9 -(memVolumefraction\_RC\_5h\_11\_25-volume\_f\_initial\_API).\*r\_BA\_3\_9); Diffusion BA 9 20h = r BA 1\*10.^(-r BA 2 9 -(memVolumefraction RC 20h 11 25-volume f initial API).\*r BA 3 9); r EA 2 9 = 5.9972;r EA 3 9 = 9.0028;Diffusion EA 9 Oh = r EA  $1*10.^{-1}$  (-r EA 2 9 -(memVolumefraction RC 0h 11 25-volume f initial API).\*r EA 3 9); Diffusion EA 9 1h = r EA  $1*10.^{(-r)}$  EA 2 9 -(memVolumefraction RC 1h 11 25-volume f initial API).\*r EA 3 9); Diffusion EA 9 5h = r EA 1\*10.^ (-r EA 2 9 -(memVolumefraction RC 5h 11 25-volume f initial API).\*r EA 3 9); Diffusion EA 9 20h = r EA 1\*10.^(-r EA 2 9 -(memVolumefraction RC 20h 11 25-volume f initial API).\*r EA 3 9); % r3 = 11.25  $r_{BA_2_{11}} = 5.7465;$ r BA 3 11 = 11.2535; Diffusion BA 11 Oh = r BA 1\*10.^ (-r BA 2 11 -(memVolumefraction\_RC\_Oh\_I1\_25-volume\_f\_initial\_API).\*r\_BA\_3\_11); Diffusion\_BA\_11\_1h = r\_BA\_1\*10.^(-r\_BA\_2\_11 -(memVolumefraction\_RC\_1h\_11\_25-volume\_f\_initial\_API).\*r\_BA\_3\_11); Diffusion\_BA\_11\_5h = r\_BA\_1\*10.^(-r\_BA\_2\_11 -(memVolumefraction\_RC\_5h\_11\_25-volume\_f\_initial\_API).\*r\_BA\_3\_11); Diffusion\_BA\_11\_20h = r\_BA\_1\*10.^(-r\_BA\_2\_11 -(memVolumefraction RC 20h 11 25-volume f initial API).\*r BA 3 11); r EA 2 11 = 5.7465;r EA 3 11 = 11.2535;Diffusion EA 11 Oh = r EA 1\*10.^ (-r EA 2 11 -(memVolumefraction RC Oh 11 25-volume f initial API).\*r EA 3 11); Diffusion EA 11 1h = r EA 1\*10.^(-r EA 2 11 -(memVolumefraction RC 1h 11 25-volume f initial API).\*r EA 3 11); Diffusion\_EA\_11\_5h =  $r_EA_1 \times 10.^{(-r_EA_2)}$  11 -(memVolumefraction RC 5h 11 25-volume f initial API).\*r EA 3 11); Diffusion EA 11 20h = r EA 1\*10.^ (-r EA 2 11 -(memVolumefraction RC 20h 11 25-volume f initial API).\*r EA 3 11); \_\_\_\_\_

```
&_____
% Plot Radius vs Diffusion Coefficient for EA and BA r3=6.75
figure(40)
semilogy(memRadius_plot_normalized_0h_6_75,Diffusion_EA_6_0h','k-
^','LineWidth',1)
hold on
semilogy (memRadius plot normalized 1h 6 75, Diffusion EA 6 1h', 'b-
^','LineWidth',1)
hold on
semilogy (memRadius plot normalized 5h 6 75, Diffusion EA 6 5h', 'r-
^','LineWidth',1)
hold on
semilogy (memRadius plot normalized 20h 6 75, Diffusion EA 6 20h', 'm-
^','LineWidth',1)
hold on
semilogy (memRadius plot normalized 0h 6 75, Diffusion BA 6 0h', 'k-
o', 'LineWidth', 1)
hold on
semilogy (memRadius plot normalized 1h 6 75, Diffusion BA 6 1h', 'b-
o', 'LineWidth', 1)
hold on
semilogy(memRadius plot normalized 5h 6 75, Diffusion BA 6 5h', 'r-
o', 'LineWidth', 1)
hold on
semilogy (memRadius plot normalized 20h 6 75, Diffusion BA 6 20h', 'm-
o','LineWidth',1)
hold on
% Label and Title of the plot
title('', 'FontSize',35)
% Normalized Radial Positions
xlabel('Normalized Radius', 'FontSize',20)
ylabel('Diffusion Coefficient', 'FontSize',20)
set(gca, 'FontSize', 20)
%set(gca,'YTickLabel',{'0','0.10','0.20','0.30','0.40','0.50','0.60','0.7
0','0.80','0.90','1.00'})
% Legend
legend('D {EA,t=0h}','D {EA,t=1h}','D {EA,t=5h}','D {EA,t=20h}','D {BA,t=
0h}','D {BA,t=1h}','D {BA,t=5h}','D {BA,t=20h}','Location','East')
% Define the intervall of the axis
%axis([0 1 0 1])
% Resize the plot to fullscreen
set(gcf, 'position', get(0, 'screensize'))
% Save Figure as Diffusion 6.75.tiff
% saveas(gcf, 'Diffusion 6.75.tiff', 'tiffn');
۶_____
٥<u>,</u>
% Plot Radius vs Diffusion Coefficient for EA and BA r3=9.00
```

```
figure(41)
semilogy(memRadius plot normalized 0h 9 00,Diffusion EA 9 0h', 'k-
^','LineWidth',1)
hold on
semilogy(memRadius plot normalized 1h 9 00, Diffusion EA 9 1h', 'b-
^', 'LineWidth', 1)
hold on
semilogy (memRadius plot normalized 5h 9 00, Diffusion EA 9 5h', 'r-
^','LineWidth',1)
hold on
semilogy(memRadius plot normalized 20h 9 00, Diffusion EA 9 20h', 'm-
^','LineWidth',1)
hold on
semilogy(memRadius plot normalized 0h 9 00, Diffusion BA 9 0h', 'k-
^','LineWidth',1)
hold on
semilogy(memRadius plot normalized 1h 9 00, Diffusion BA 9 1h', 'b-
o', 'LineWidth', 1)
hold on
semilogy (memRadius plot normalized 5h 9 00, Diffusion BA 9 5h', 'r-
o', 'LineWidth', 1)
hold on
semilogy (memRadius plot normalized 20h 9 00, Diffusion BA 9 20h', 'm-
o', 'LineWidth', 1)
hold on
% Label and Title of the plot
title('', 'FontSize',35)
% Normalized Radial Positions
xlabel('Normalized Radius', 'FontSize',20)
ylabel('Diffusion Coefficient', 'FontSize',20)
set(gca, 'FontSize', 20)
%set(gca,'YTickLabel',{'0','0.10','0.20','0.30','0.40','0.50','0.60','0.7
0','0.80','0.90','1.00'})
% Legend
legend('D {EA,t=0h}','D {EA,t=1h}','D {EA,t=5h}','D {EA,t=20h}','D {BA,t=
0h}','D {BA,t=1h}','D {BA,t=5h}','D {BA,t=20h}','Location','East')
% Define the intervall of the axis
%axis([0 1 0 1])
% Resize the plot to fullscreen
set(gcf, 'position', get(0, 'screensize'))
% Save Figure as Diffusion 9.00.tiff
% saveas(gcf, 'Diffusion 9.00.tiff', 'tiffn');
§_____
<u>_____</u>
8-----
% Plot Radius vs Diffusion Coefficient for EA and BA r3=11.25
figure(42)
```

```
semilogy (memRadius plot normalized 0h 11 25, Diffusion EA 11 0h', 'k-
^', 'LineWidth', 1)
hold on
semilogy (memRadius plot normalized 1h 11 25, Diffusion EA 11 1h', 'b-
^', 'LineWidth', 1)
hold on
semilogy (memRadius plot normalized 5h 11 25, Diffusion EA 11 5h', 'r-
^','LineWidth',1)
hold on
semilogy (memRadius plot normalized 20h 11 25, Diffusion EA 11 20h', 'm-
^','LineWidth',1)
hold on
semilogy (memRadius plot normalized 0h 11 25, Diffusion BA 11 0h', 'k-
o', 'LineWidth', 1)
hold on
semilogy (memRadius plot normalized 1h 11 25, Diffusion BA 11 1h', 'b-
o', 'LineWidth', 1)
hold on
semilogy (memRadius plot normalized 5h 11 25, Diffusion BA 11 5h', 'r-
o','LineWidth',1)
hold on
semilogy (memRadius plot normalized 20h 11 25, Diffusion BA 11 20h', 'm-
o', 'LineWidth', 1)
hold on
% Label and Title of the plot
title('', 'FontSize',35)
% Normalized Radial Positions
xlabel('Normalized Radius', 'FontSize',20)
ylabel('Diffusion Coefficient', 'FontSize',20)
set(gca, 'FontSize', 20)
%set(gca,'YTickLabel',{'0','0.10','0.20','0.30','0.40','0.50','0.60','0.7
0','0.80','0.90','1.00'})
% Legend
legend('D_{EA,t=0h}','D_{EA,t=1h}','D_{EA,t=5h}','D_{EA,t=20h}','D_{BA,t=
0h}','D {BA,t=1h}','D {BA,t=5h}','D {BA,t=20h}','Location','East')
% Define the intervall of the axis
%axis([0 1 0 1])
% Resize the plot to fullscreen
set(gcf, 'position', get(0, 'screensize'))
% Save Figure as Diffusion 11.25.tiff
% saveas(gcf,'Diffusion 11.25.tiff', 'tiffn');
```

## **D\_Variations.m**

```
% D Variations
% (c) by Hannes Pucher
       ------
8-----
% Clear, Close and delete all
clc
clear all
close all
8-----
۶_____
% Load files in the workspace
% Load memRadius plot files
load('memRadius end d50.mat')
memRadius d50 = memRadius end*10^6;
load('memRadius end d100.mat')
memRadius d100 = memRadius end*10^6;
load('memRadius end d163.mat')
memRadius d163 = memRadius end*10^6;
load('memRadius end d200.mat')
memRadius d200 = memRadius end*10^6;
8-----
§_____
% Calculate the Percentage of Shrinkage
Percent_d50 = 100-(memRadius_d50*2)/(memRadius_d50(1,1)*2)*100;
Percent_d100 = 100-(memRadius_d100*2)/(memRadius_d100(1,1)*2)*100;
Percent_d163 = 100-(memRadius_d163*2)/(memRadius_d163(1,1)*2)*100;
Percent d200 = 100-(memRadius d200*2)/(memRadius d200(1,1)*2)*100;
      _____
8_____
% Define the memTime plot vector for the plot
memTime plot = linspace(0,3601,3601);
٥<u>,</u>
% Save all variables
save Experimental Parameters.mat
§_____
% Plot Radius vs Time
figure(1)
plot(memTime_plot/3600,memRadius_d50*2,'k','LineWidth',2)
hold on
plot(memTime plot/3600,memRadius d100*2,'m-.','LineWidth',2)
hold on
plot(memTime plot/3600,memRadius d163*2,'r--','LineWidth',2)
hold on
plot(memTime_plot/3600,memRadius_d200*2,'b:','LineWidth',2)
% Label and Title of the plot
title('', 'FontSize',35)
```

```
xlabel('Time [h]', 'FontSize',20)
ylabel('SMD [\mum]', 'FontSize',20)
set(gca, 'FontSize', 20)
% Legend
legend('d {t=0} = 50','d {t=0} = 100','d {t=0} = 163','d {t=0} =
200', 'Location', 'NorthEast')
% Define the intervall of the axis
axis([0 1 0 250])
% Resize the plot to fullscreen
set(gcf, 'position', get(0, 'screensize'))
% Save Figure as SMD.tiff
saveas(gcf,'SMD.tiff', 'tiffn');
%_____
§_____
% Plot Percentage of Shrinkage vs Time
figure(11)
plot(memTime plot/3600, Percent d50, 'k', 'LineWidth', 2)
hold on
plot(memTime plot/3600, Percent d100, 'm-.', 'LineWidth', 2)
hold on
plot(memTime plot/3600, Percent d163, 'r--', 'LineWidth', 2)
hold on
plot(memTime plot/3600, Percent d200, 'b:', 'LineWidth', 2)
% Label and Title of the plot
title('', 'FontSize',35)
xlabel('Time [h]', 'FontSize',20)
ylabel('Shrinkage [%]', 'FontSize',20)
set(gca, 'FontSize', 20)
% Legend
legend('d {t=0} = 50', 'd {t=0} = 100', 'd {t=0} = 163', 'd {t=0} =
200', 'Location', 'SouthEast')
% Define the intervall of the axis
axis([0 1 0 50])
% Resize the plot to fullscreen
set(gcf, 'position',get(0, 'screensize'))
% Save Figure as SMD.tiff
saveas(gcf,'Percentage.tiff', 'tiffn');
§_____
```